Cortical and subcortical changes in Alzheimer's disease: a longitudinal and quantitative MRI study

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Short title: Longitudinal and quantitative MRI in AD

Abstract

Quantitative MRI provides important information about tissue properties in brain both in normal ageing and in degenerative disorders. Although it is well known that those with Alzheimer's disease (AD) show a specific pattern and faster rate of atrophy than controls, the precise spatial and temporal patterns of quantitative MRI in AD are unknown. We aimed to investigate neuroimaging correlates of AD using serial quantitative MRI. In our study, twenty-one subjects with AD and thirty-two similar-aged healthy controls underwent two serial MRI scans at baseline and 12 months. Tissue characteristics were captured using two quantitative MRI parameters: longitudinal relaxation time (qT1) and transverse relaxation time (qT2). The two groups (AD and controls) were statistically compared using a voxel based quantification (VBQ) method based on Matlab and SPM8. At baseline, subjects with AD showed a significant reduction of qT1 and qT2 compared to controls in bilateral temporal and parietal lobes, hippocampus, and basal ganglia. This pattern was also observed at follow-up. Longitudinally, in AD we found a significant increase rather than further reduction of qT1 and qT2 from the baseline in bilateral hippocampus, thalamus and right caudate nucleus. In addition, the longitudinal change of qT1 in left hippocampus was negatively correlated with cognitive decline in AD over the 1-year period, and the general disease severity significantly predicted the amount of increase of qT1 in bilateral hippocampus over 12 months. The longitudinal change of qT2 in left parahippocampus correlated with change in neuropsychiatric features over time. In summary, quantitative MRI parameters were reduced in AD cross-sectionally, but increased over time, showing distinct spatiotemporal patterns

from the atrophy in AD. We also showed the clinical relevance of quantitative MRI parameters, indicating their potential promise as new imaging markers in AD.

(286 words)

Keywords quantitative MRI, VBQ, Alzheimer's disease, amyloid, relaxometry, early diagnostics

Introduction

One of the main current research focuses on Alzheimer's disease (AD) is early intervention, thus, there is a pressing need for reliable biomarkers for early AD detection. Existing biomarkers include cerebrospinal fluid (CSF), PET/SPECT imaging of neural metabolism and β-amyloid binding, as well as structural and functional MRI [1]. Among these techniques, MRI is noninvasive, so provides a powerful and safe tool for research and clinical diagnosis / screening, both of which are important for investigating the underlying neuropathology and early detection [2].

It has been shown that MRI not only reveals changes in brain volume and macrostructure, but also microstructural alterations in brain tissue integrity and its biochemical environment [3]. An emerging neuroimaging technique is quantitative MRI (qMRI) based on the physical measurement of longitudinal (qT1) and transverse (qT2) relaxation times. (Here we shall refer to these quantitative measurements as qT1 and qT2 to distinguish them from the more common qualitative radiological T1 or T2 weighted scans). In general, qT1 is correlated with water content and the level of myelination, and qT2 is related to chemically determined brain iron concentration [3].

Quantitative MRI provides important information about tissue properties in brain both in normal ageing [4,5], degenerative disorders such as Parkinson's disease [6], AD and dementia with Lewy bodies (DLB) [7], and neuronal loss due to brain and spinal cord injury [8]. In our previous study of DLB using qMRI, we demonstrated that the spatial pattern in the changes of qT1 and

qT2 was different from the pattern of atrophy, thus quantitative MRI may provide incremental benefit over and above that of structural MRI [7]. We also argue that quantitative MRI may indirectly detect neuronal and molecular changes in AD that precede the structural brain damage and clinical impairments decades in time [2]. Although it is well known that those with AD show a specific pattern and faster rate of atrophy than controls, the precise spatial and temporal patterns of quantitative MRI alteration in AD are unknown.

In this study, we aimed to investigate neuroimaging correlates of AD using serial quantitative MRI. In particular, we evaluated maps of qT1 and qT2 in grey matter comparing these parameters between the AD and the similarly aged control groups using the voxel-based quantification (VBQ) approach [4] both cross-sectionally and longitudinally. In addition, we explored the clinical relevance of quantitative MRI changes over a 12-month period.

Materials and Methods

Subjects, assessment and diagnosis

Thirty-six subjects with probable AD [9] over the age of 60 were recruited from a community dwelling population of patients referred to local Old Age Psychiatry, Geriatric Medicine or Neurology Services. Thirty-five similarly aged control subjects were recruited from relatives and friends of subjects with dementia or volunteered via advertisements in local community newsletters. Twenty-one AD subjects and 32 controls underwent MR imaging

at both baseline and follow-up and are included in the analyses reported here. These subjects underwent clinical and neuropsychological evaluations at baseline and follow-up at 1 year. (The rest of subjects were not scanned at follow-up, thus excluded from the analysis.)

The research was approved by Newcastle & North Tyneside 1 Research Ethics Committee (No. 05/Q0905/217). All subjects or, where appropriate, their nearest relative, provided written informed consent. Assessment of global cognitive measures at both baseline and follow-up assessments included the Cambridge Cognitive Examination (CAMCOG) [10], which incorporates the Mini-Mental State Examination (MMSE) [11]. Motor parkinsonism was evaluated with the Unified Parkinson's Disease Rating Scale Part III (UPDRS-III) [12]. For subjects with dementia, neuropsychiatric features were evaluated with the Neuropsychiatric Inventory (NPI) [13].

MRI data acquisition

Participants underwent MRI scanning on a 3T Philips Achieva MRI system with an 8-channel receiver head coil at both baseline and 12-month follow-up. Structural images were acquired using a T1 weighted volumetric sequence (3D MPRAGE, sagittal acquisition aligned with the AC-PC line, 1mm isotropic resolution, matrix 240×240×180, TR=9.6ms, TE=4.6ms, flip angle=8^{o}, SENSE factor 2). In addition, a B0 field-map using a dual echo 3D GRE (2mm isotropic resolution, matrix 128×128×72, TR=27ms, TE=2.6/6.1ms) was acquired.

Quantitative mapping of tissue qT1 and qT2 relaxation times was performed using custom designed MRI sequences developed in-house under a research agreement with Philips Medical Systems.

Fast qT1 mapping was based on the inversion recovery (IR) methods originally published by Ordidge et al [14] and expanded by Clare and Jezzard [15]. The sequence imaged 72 axial slices spanning the brain, which were grouped into 5 consecutive slabs each of thickness 24mm. For each slab a slice selective adiabatic (sech) inversion pulse was applied to invert the magnetisation ensuring that the region of full inversion encompassed the 24 mm thick section of interest. This inversion was followed by slice selective single shot EPI readout of 12 contiguous slices of 2 mm thickness equally spaced across the slab. The first slice was imaged 250ms post inversion and subsequent slices every 205 ms thereafter. During the repetition time (TR) of 15000ms each slab was inverted and imaged with a slab order of 1,3,5,2,4 to minimise interaction between slices. In this way the time between inverting adjacent slabs was 6000ms, sufficient to allow full relaxation of brain tissue. The sequence was repeated 12 times and on each repetition the order of acquired slices within each slab was permuted by one position, for example

1,2,3,4,5,6,7,8,9,10,11,12

2,3,4,5,6,7,8,9,10,11,12,1

3,4,5,6,7,8,9,10,11,12,1,2

etc

such that the at the end of acquisitions every slice had been imaged at each

of the 12 inversion times. Total scan time was therefore 180s for the complete IR series in 72 slices with isotropic 2mm resolution. This sequence is shown schematically in Figure 1.

Insert Figure 1 here

Calculation of qT1 maps used a purpose written algorithm in Matlab, which reordered the data into incremental inversion order for each slice and then performed voxel-wise non-linear least squares fitting to the standard 3 parameter model for the inversion recovery experiment:

$$S(T_{IR}) = S_o(1 - \alpha e^{\frac{-T_{IR}}{qT1}})$$

where T_{IR} is the inversion time, $S(T_{IR})$ is the signal value or the data obtained from the inversion recovery experiment, qT1 is the longitudinal relaxation time, S_o is the proton density and α is the effective inversion efficiency . qT1, S_o and α were computed pixel-wise from the fitting process. Ideally α is expected to be 2 but it was allowed to be a free variable in the fitting in order to increase the accuracy of the computed qT1. The 3D images of proton density S_0, qT1, and the goodness of fit were saved for evaluation.

Fast qT2 mapping used a multi-spin echo sequence with segmented EPI readout based around a Gradient and Spin Echo Imaging sequence. The sequence collected 8 spin echoes with equal spacing of 20ms and 5 gradient recalled echoes per spin echo (EPI factor 5) to accelerate image collection.

185 Repetition time was set to 4700ms and 72 slices were collected in standard
186 interleaved acquisition (2mm isotropic resolution, matrix 128×128). Total
187 scan time was 120s.
188
189 Calculation of qT2 maps again used a purpose written algorithm in Matlab,
190 which performed voxel-wise non-linear least squares fitting to the standard 2
191 parameter model for transverse relaxation.
192

$$S(TE) = S_o e^{\frac{-TE}{qT2}}$$

193
194 where *TE* is the echo time, qT2 is the transverse relaxation time and S_o is the
195 proton density. qT2, and S_o were computed pixel-wise from the fitting
196 process. The 3D images of proton density S_o, qT2, and the goodness of fit
197 were saved for evaluation.
198
199 Scans were collected using both sequences in aqueous and gel based test
200 objects of known qT1 and qT2 and compared to data collection using a single
201 slice inversion recovery sequence for qT1 and a single slice Carr-Purcell
202 Meiboom-Gill (CPMG) sequence for qT2 to validate the method.
203
204 *Statistical Tests of Demographic, clinical, and cognitive measures.*

205 Group characteristics were evaluated with Statistical Toolbox of Matlab
206 (www.mathworks.co.uk/products/statistics). Differences in demographic and
207 clinical data were assessed with use of either t-tests for continuous variables

208 or χ^2 tests for categorical measures. For each test statistic, a probability value
209 of $p<0.05$ was regarded as significant.
210
211 *Voxel-based quantification*

212 MRI data processing was performed in a combined FSL
213 (fsl.fmrib.ox.ac.uk/fsl/fslwiki) and SPM (www.fil.ion.ucl.ac.uk/spm) based on
214 the previously validated voxel-based quantification (VBQ) procedure [4]. At
215 both baseline and follow-up, raw qT1 and qT2 imaging datasets were
216 corrected for field inhomogeneities using B0 maps and the PRELUDE/FUGUE
217 algorithm in FSL [16]. Then, the bias corrected qT1 and qT2 maps were used
218 for subsequent analysis.
219
220 Volumetric structural T1 weighted images were firstly segmented using
221 Gaussian mixture model implemented in the VBM toolbox [17], and brain
222 tissues were classified into grey matter (GM), white matter (WM) and
223 Cerebrospinal fluid (CSF) for both baseline and follow-up. A conjunction GM
224 brain mask was generated for each individual subject (in both AD and control
225 groups) by computing the intersection between the GM probability maps at
226 the baseline and that at the follow-up of the same subject, and then
227 thresholded at $p>0.5$ in each participant's native space. This mask was used
228 to select a common area of GM tissue at both baseline and follow-up in order
229 to ensure there were equal number of voxels tested in both time points, thus
230 avoiding potential bias in the statistical analysis.
231

As in standard longitudinal VBM procedure, only the baseline GM probability maps were non-linearly normalized to standard MNI space (www.mni.mcgill.ca) using the diffeomorphic registration algorithm (DARTEL) [17] in SPM, and the resulting parameters were used to normalize the qT1 and qT2 maps in both baseline and follow-up. The qT1 and qT2 maps at both time points were firstly co-registered with the GM probability maps derived from structural T1 images at baseline, then the thresholded conjunction GM brain masks were applied to qT1 and qT2 data at both time points. Finally, we transformed the GM maps of qT1 and qT2 MRI parameters into standard MNI space using the participant-specific diffeomorphic parameters estimated from the baseline scans based on the previous DARTEL procedure. However, we did not apply modulation to these quantitative MRI parameters in order to avoid confound of age and disease related GM volume changes. Finally, all normalized quantitative qT1 and qT2 maps were smoothed with an isotropic Gaussian kernel of 6 mm full width at half maximum.

For statistical analysis investigating disease induced regional microstructural alterations between the AD and control groups, and between the baseline and follow-up, we used the General Linear Model (GLM) with age and gender as covariates. Then, two-tailed t-tests were performed at each voxel to detect voxel-wise difference between the groups or time points. We also tested the group x time interaction using a mixed model ANOVA. The false positive rate was controlled using family-wise error (FWE) correction for multiple comparisons, and thresholded at $p<0.05$ at the cluster level.

Post-hoc region-of-interest analysis

To explore the clinical relevance of qT1 and qT2, in a post-hoc region-of-interest (ROI) analysis, we extracted the averaged quantitative MRI values from significant clusters found in the longitudinal comparison. Here, we used the unsmoothed maps in order to preserve the original values of the MR parameters. Then, we correlated cognitive and clinical measures with the averaged quantitative MRI values extracted from the significant clusters obtained from the previous group comparisons. These measurements included the CAMCOG, MMSE, UPDRS III and NPI total scores. Multiple comparisons were controlled using Bonferroni correction for the number of ROIs.

Results

Demographic clinical and cognitive measures

As shown in Table 1, there were no significant differences between AD and control groups for age, sex and educational level. However, as expected, the two groups significantly different at both baseline and follow-up for UPDRS III, NPI, MMSE and CAMCOG scores with subjects with AD scoring poorer in all measures compared to the controls.

Insert Table 1 here

Cross-sectional comparison of qT1: AD vs. controls

As shown in Figure 2A and Table 2A, at the baseline, we found a significant decrease in qT1 for the AD group compared to controls (p<0.0001, FWE) in bilateral temporal, parietal and occipital lobes, as well as several subcortical / striatal nuclei. Largest significant clusters were within bilateral hippocampus, parahippocampus, cuneus, precuneus, caudate and putamen. At the follow-up, we found a very similar pattern of qT1 changes comparing between AD and control groups. See Figure 2B and Table 2B. No significant increase in qT1 was found for the AD group compared to controls at either baseline or follow-up.

Insert Table 2 here

Insert Figure 2 here

Cross-sectional comparison of qT2: AD vs. controls

For qT2 at the baseline, we also found a significant decrease for the AD group compared to controls (p<0.0001, FWE) in left superior and right middle temporal lobes, bilateral hippocampus and left parahippocampus as shown in Figure 3A and Table 3A. At the follow-up, we found a very similar pattern of qT2 changes comparing between AD and control groups except for a cluster covering left caudate, putamen and pallidum, and a right cuneus cluster, which were not seen at the baseline. See Figure 3B and Table 3B. No significant increase in qT2 was found for the AD group compared to controls at either baseline or follow-up.

304

305 Insert Table 3 here

306

307 Insert Figure 3 here

308

309 *Longitudinal comparison of qT1: baseline vs. follow-up*

310 When comparing qT1 between baseline and follow-up in the AD group, we
311 found a significant increase over 12 months in bilateral hippocampus and
312 parahippocampus (p<0.0001, FWE), thalamus (p<0.0001 for left and p=0.002
313 for right, FWE) and right caudate (p<0.0001, FWE) as shown in Figure 2C
314 and Table 4A. The significant hippocampus clusters in the longitudinal
315 comparison are more medial to the clusters found in the cross-sectional
316 comparisons; see Figure 2. We found no longitudinal change for qT1 in the
317 control group and no group (AD and controls) x time (baseline and follow-up)
318 interaction.

319

320 Insert Table 4 here

321

322 *Longitudinal comparison of qT2: baseline vs. follow-up*

323 For qT2, we found a significant increase between the baseline and the follow-
324 up in the AD group as shown in Figure 3C and Table 4B. Significant clusters
325 are located in left parahippocampus (p<0.0001, FWE), right caudate, putamen
326 and insula (p<0.0001, FWE), as well as right middle frontal lobe (p=0.002,
327 FWE). We found a significant group x time interaction in right insula

(p<0.0001, FWE) bordering with right putamen and extending to right caudate at lower threshold (p<0.001, uncorrected). We argue that atrophy is unlike the explanation of this effect because if atrophy were a driver of an increase in qT2 over time, we would expect AD subjects at baseline to have a greater qT2 than controls because of their greater atrophy, a result opposite to what we found here.

For the control group, we found a significant longitudinal increase in qT2 (p<0.0001, FWE) in left superior parietal lobe, caudate head, and supplementary motor area extending to superior medial prefrontal cortex. (See Figure 3D.)

Correlation between cognitive / clinical measures and quantitative MRI

Here, the main focus is on the relationship between longitudinal changes in quantitative MRI parameters and cognitive / clinical measures in the AD group at baseline, follow-up and change over the 1-year period. Thus for qT1, we have defined three region-of-interest (ROIs) based on the results of the longitudinal comparison of qT1, i.e. left / right hippocampus and right caudate. We found a significant negative correlation between the longitudinal changes in qT1 in left hippocampus and the cognitive decline (i.e. change in total MMSE score over the 1-year period) in AD (r=-0.58, p=0.006). We found a significant correlation between baseline CAMCOG score and the changes of qT1 in bilateral hippocampus over the 1-year period. In addition, a significant correlation was found between baseline UPDRS III score and the longitudinal

changes of qT1 in bilateral hippocampus. Both effects were stronger in the right hemisphere than in the left and only the right hippocampus survived the correction for multiple comparisons. (See Table 5A.) Nonetheless, this suggests that baseline CAMCOG and UPDRS scores predict changes in qT1 in these regions, that is, the more severe the dementia in general, the more qT1 increases.

We also found a significant correlation between qT1 in right caudate and UPDRS score cross-sectionally at both baseline (r=0.60, *p*=0.004) and follow-up (r=0.51, *p*=0.018) in AD. Moreover, qT1 in right hippocampus was significantly correlated with the CAMCOG score only at the follow-up (r=-0.60, *p*=0.004) but not at the baseline. (See Table 5A.) No other correlation survived the correction for multiple comparisons.

Insert Table 5 here

For qT2, we have extracted qMRI values from four significant clusters found in the longitudinal comparison: right insula extending to putamen, left parahippocampus, right caudate and right superior medial frontal cortex (BA8). We found a significant correlation between the longitudinal changes of qT2 in left parahippocampus and the changes in NPI score over time (r=0.54, *p*=0.012) in AD. (See Table 5B.) No other correlation was found.

Individual analysis in longitudinal comparison

Figure 4 shows the individual variability in longitudinal changes in quantitative MRI within the AD group, and how it relates to disease severity. It can be seen in Figure 4A that subjects with AD showed a general increase in qT1 in right hippocampus, and the rate of increase seems to accelerate in moderate and severe cases of AD, i.e. baseline MMSE score lower than 20. The same pattern was observed in other clusters found in the longitudinal analysis. Figure 4B shows the individual changes in qT2 in left parahippocampus over time. We have found a very similar trend as in qT1 with subjects with AD generally showing an increase in qT2 over 12 months. We have also found similar pattern in other significant clusters derived in the longitudinal analysis in the AD group.

Insert Figure 4 here

Discussion

Using novel longitudinal and quantitative MRI method and voxel-based quantification, we showed that at the cross-sectional level, qT1 and qT2 in AD were significantly decreased in multiple cortical areas in bilateral temporal and parietal lobes with the largest changes in medial temporal structures comparing to similarly aged control subjects at baseline. This pattern is consistent with previous neuroimaging studies with AD showing significant volume reduction in these regions such as hippocampal, enthorinal and parahippocampal cortices [18].

At follow-up, we found a very similar pattern of quantitative MRI changes in both qT1 and qT2 comparing AD and control groups with the main affected brain areas in bilateral hippocampus and associated structures. This demonstrates the robustness of qMRI in reproducing a consistent pattern of quantitative MRI parameter changes at two different time points with 12 months gap.

It is worth noting that both qT1 and qT2 parameters consistently picked up substantial changes in subcortical regions, e.g. bilateral caudate, putamen and thalamus. However, comparing to neocortex, in particular the hippocampus, these basal nuclei and thalamus have received much less attention in previous research, and conventional volumetric MRI showed a mixed picture of atrophy in these subcortical areas. For example, atrophy of putamen was found in DLB but not in AD [19], whereas putamen and thalamic atrophy were both shown in AD in a different study [20] reflecting a relatively high level of noise in volumetric measures in these regions and large inter-study variability. In contrast, quantitative MRI may detect neuronal and macromolecular changes in tissue environment, which does not rely on atrophy shown in structural T1 weighted MRI. Based on this, we argue that qMRI provides incremental benefit over and above that of structural MRI. Quantitative MRI also offers a unique opportunity to detect early brain changes in AD before observable brain volume reduction can be reliably shown and cognitive / clinical impairments can be found [2].

Although we found that AD was characterized by a reduction in qMRI

parameters in cross-sectional comparison, in longitudinal comparison, we found that qT1 was increased rather than decreased in right caudate, bilateral hippocampus and parahippocampus, as well as in thalamus. We also found that qT2 was increased in right caudate, putamen and insula in addition to left parahippocampus in AD. Frontal changes in qT2 over time were also notable in AD. This spatial pattern is consistent with the development of atrophy in AD [21]. Increase in qT2 was found in healthy controls in left superior parietal lobe, left caudate head, and bilateral supplementary motor area extending to superior medial prefrontal cortex. However, none of these brain regions overlap with longitudinal qT1 / qT2 changes found in AD suggesting the increase of qT2 in AD and controls may reflect distinct underlying causes. The only significant group x time interaction was found in right insula extending to putamen and caudate nucleus.

To further understand the increase in qMRI over time in AD, we performed an individual analysis, which showed the changes of qT1 and qT2 over time in hippocampus, caudate and other clusters found in the longitudinal comparison. By sampling individual subjects that were at different stages of the disease indicated by their severity (i.e. baseline MMSE), we have pictured an overall trajectory of qT1 and qT2 in clinically diagnosed AD. It is notable that the rate of qMRI increase was slow at early stages of AD but accelerated at severe stage of AD. Thus, although qT1 and qT2 decreased in AD comparing with controls at the cross-section level, it is possible that qT1 and qT2 may increase over time in AD because plaque burden may stabilize or even fall in established stages of AD as the disease progresses. In addition,

450 we found that general disease severity (measured by different but related
451 scales, i.e. CAMCOG and UPDRS) predicts the rate of change in qT1 in
452 hippocampus showing a faster rate of increase at the severe stage of AD.
453
454 These changes in qMRI followed a trend that mirrors the inverted 'U' shape
455 trajectory of brain β-amyloid over time [22] suggesting that at the severe stage
456 of AD the brain β-amyloid (and/or other factors) may undergo a decrease. A
457 more quantitative treatment of the parallels between the current results and
458 the findings by Jack et al will require a deeper analysis of how the very
459 different properties of the two might reflect how brain β-amyloid burden is
460 captured by each imaging method, and the consequences of this for temporal
461 trajectory of these variations. This analysis is outside the scope of the current
462 paper, and the comparisons we provide here should be regarded as
463 preliminary and illustrative. However, it is clear that such a 'U' shaped
464 temporal pattern has not been found in atrophy in AD.
465
466 In addition, we showed the clinical relevance of quantitative MRI parameters
467 in AD, i.e. the change of qT1 at left hippocampus was correlated with
468 cognitive decline (annual changes in MMSE score) in AD. For qT2, the
469 longitudinal change in right parahippocampus was significantly correlated with
470 the annual changes in neuropsychiatry condition (NPI) in AD over time. In
471 addition, we found a significant correlation between qT2 in right caudate
472 nucleus and parkinsonism (UPDRS score) at the cross-sectional level (at both
473 baseline and follow-up), suggesting the AD pathology may be present in basal
474 ganglia structures, therefore causing motor parkinsonism in AD. Here, it is

interesting to see that qT2 in caudate was sensitive to the changes in UPDRS scores. This finding is also consistent with Wilson et al. [23], which showed that parkinsonian signs are strong predictors for the progression of AD.

In our previous cross-sectional study on dementia with Lewy bodies (DLB), we also found a significant reduction of qMRI parameters in DLB compared to controls [7]. In addition, we showed that the spatial pattern of qMRI alteration only partly overlapped with that of atrophy, making the latter an unlikely explanation for the qMRI decreases. In the current study, we have followed the similar analysis procedure in order to avoid partial volume effect due to atrophy. In seeking the possible underlying biochemical interpretation of these quantitative MRI parameters and their evolution over time, qT1 is predominantly influenced by water content but also relates to the degree of myelination [24,25,26]. Both qT1 and qT2 are also sensitive to the level of iron, which is present in amyloid plaques [27] and in microbleeds.

Although it is not possible to precisely determine the pathological changes associated with alterations in qT1 or qT2 in AD, it has been suggested that decreases in qT1 and qT2 might be associated with increases in amyloid burden and iron load in the brain based on histologically confirmed animal model of AD [28,29]. Consistent with our finding, decreased qT1 was found to be associated with an increase in β-amyloid deposition in 5xFAD transgenic mouse model of Alzheimer's disease compared with wild type mice [30]. In addition, decreased qT2 was found in APP/PS1 transgenic mouse model of

AD [31,32] probably reflecting a complex interaction between β-amyloid and iron concentration as well as other factors.

In a longitudinal study of β-amyloid plaque development in Tg2576 transgenic mice using qT2 relaxation time [33], it has been found that qT2 decreases with age (12 - 18 months) following an increase in plaque area, number and size in the brain. Although it is difficult to match the disease stage of the mouse model to humans with AD and it is not common to find atrophy in the animal model of AD, this finding is nonetheless consistent with our results showing decreased qT2 in medial temporal lobes in AD. It has also been shown in a study based on APP/PS1 transgenic mice model that qT2 is modulated by the level of amyloid in subiculum without histochemically detectable iron in the brain [34], providing promises in detecting the pathological process in AD at the earliest stages.

In addition to our previous findings on qMRI changes in DLB [7], as well as the established literature on animal qMRI correlates, the current data provided convergent evidence for the potential ability of quantitative MRI in detecting early changes of tissue property caused by neurodegenerative disease. Being able to apply this novel technique in human using relatively safe MRI method enables new means for early detection of AD and tracking its progression over time. This approach is also likely to close the gap between animal models of amyloidosis and studies on human AD in the context of drug discovery.

Conclusion

In summary, quantitative MRI parameters were reduced in AD cross-sectionally, but increased over time, showing distinct spatiotemporal patterns from the atrophy in AD. Our findings are consistent with animal model of AD showing quantitative MRI can provide information, which may reflect pathology such as amyloid burden and iron load. We also showed the clinical relevance of quantitative MRI, indicating their potential promise as new early imaging markers in AD. With reduced radiation, MRI is more suited for longitudinal studies than PET. Thus, longitudinal and quantitative MRI will be valuable in developing new treatments by tracking brain changes associated AD in vivo.

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550 **Reference**

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