

1 **Evaluation of a silver-impregnated coating to inhibit colonization of**
2 **orthopedic implants by biofilm forming Methicillin Resistant *Staphylococcus***
3 ***pseudintermedius***

4 **M.A. Azab^{1,3}; M.J. Allen^{1,2}; J.B. Daniels¹**

5 ¹Department of Veterinary Clinical Sciences, College of Veterinary Medicine, The Ohio State
6 University, Columbus, OH, USA; ²Department of Veterinary Medicine, University of
7 Cambridge, England; ³Department of Surgery, Faculty of Veterinary Medicine, Damanhour
8 University, Egypt

9

10 **Correspondence to**

11 Joshua B. Daniels, DVM, PhD, DACVM

12 The Ohio State University College of Veterinary Medicine

13 601 Vernon Tharp Dr.

14 Columbus, OH, USA 43210

15 Phone: 614-247-1725

16 Fax: 614-292-0895

17 Email: daniels.384@osu.edu

18

19 **Acknowledgements:** The authors thank Bio-Gate AG for providing the Ag/SiOxCy plasma
20 coating on the test discs.

21

22 **Conflict of interest:**

23 Dr. Allen is a paid consultant to BioMedtrix, LLC, who provided the samples for the study.

24 However, no compensation was provided for performing the study.

25 **Introduction**

26 Surgical site infection (SSI) related to orthopedic procedures is a major complication that
27 is associated with increased morbidity, mortality, and financial expenses. Implant-related SSI can
28 be difficult or impossible to resolve with routine antimicrobial therapy alone due to the formation
29 of biofilms on the orthopedic implants (1). Staphylococci are the most frequent causes of
30 biofilm-associated infections as they are common opportunistic bacteria that reside on the skin
31 and mucous surfaces (2). The most clinically relevant Staphylococci are the coagulase positive
32 Staphylococci, and in dogs specifically: *Staphylococcus pseudintermedius*. Recently, methicillin-
33 resistant *Staphylococcus pseudintermedius* (MRSP) has emerged as an important cause of SSI in
34 dogs (3). MRSP isolates are often not only resistant to β -lactam antibiotics, but also to several
35 other classes of antimicrobial drugs (4). The large increase in antimicrobial-resistant
36 microorganisms clearly shows that new control strategies are required. Antimicrobial coatings of
37 implant surfaces have a great potential in this context, such as coatings containing or releasing
38 antimicrobial agents. Coatings containing inorganic antimicrobial agents are very attractive
39 alternatives from the perspective of doping of biomaterials, which have advantages including
40 good antibacterial activity, biocompatibility, and stability (5). Silver coated orthopedic implants
41 have widely been used to prevent the growth of bacterial biofilms (6, 7) due to silver's broad-
42 spectrum of activity against gram-positive and gram-negative bacteria. (8).

43 As the use of silver and silver-based products increases, it is becoming important to
44 clarify the efficacy and efficiency of silver against different microorganisms and biofilms.
45 Accordingly, the objective of this study is to evaluate the *in vitro* antibacterial activity of new
46 ultrathin plasma coating with polysiloxan embedded silver particles against a strong biofilm-
47 forming MRSP strain.

48 **Methods, Results & Discussion**

49 Additional details are furnished in the supplemental materials.

50 An MRSP isolate (OSU 12-2910), originally sourced from an infected canine total knee
51 replacement in a 9 year old male neutered Kuvasz was evaluated for biofilm production using a
52 microtitre plate assay (MPA) described by Stepanovich et al (9). The average OD₅₇₀ of the
53 triplicates of isolate and negative controls and the cut-off value (OD_c) were established where
54 OD_c = average OD₅₇₀ of the negative control + 3×SD of the negative control. According to the
55 scheme of Stepanovich et al., the tested clinical MRSP isolate was classified as a strong biofilm
56 producer where the OD₅₇₀ of the eluted crystal violet was greater than 4 times of the cut off value
57 (4×OD_c), consistent with an earlier study of *S. pseudintermedius*, which showed that the
58 majority of isolates produced biofilm, and 96% were classified as either strong or moderate
59 biofilm producers (10).

60 Silver/Siloxane chemistry (Ag/SiO_xC_y) plasma polymer-coated circular discs (10 mm
61 diameter and 1 mm thickness) were manufactured from commercially pure titanium (ASTM
62 F67), and had previously undergone cytotoxicity testing in L-929 mouse fibroblast cells with a
63 method compliant with ISO 10993-5; 2009, with no cytotoxicity evident by 72 h (unpublished
64 data). Uncoated titanium discs were used as negative controls. All discs were sterilized by
65 gamma irradiation prior to laboratory testing. The *in vitro* antimicrobial activity assay was
66 performed according to the standard test method, ASTM E-2180-07, with the modification of
67 using one log step higher inoculum (11). The antimicrobial efficacies of silver-coated titanium
68 specimens (*n* =12), and controls (*n* =12) were evaluated at two times: 5 minutes after inoculation
69 of the specimens (T₀) and after 24 hours of incubation (T₂₄). The numbers of recovered
70 organisms were averaged as the mean CFU/ml. The averaged means were then transformed and

71 expressed as mean log₁₀ CFU. The statistical significance between the mean log₁₀ CFU counts of
72 silver-coated and control specimens at T₀ and T₂₄ was evaluated using an unpaired *t*-test; a value
73 of *P* <0.05 was considered statistically significant.

74 At T₀, there was no significant difference in MRSP growth between control uncoated
75 (3.83 ± 0.51 log₁₀ CFU/ml, mean ± SD) and silver-coated discs (3.59 ± 0.33 log₁₀ CFU/ml) (*P*
76 =0.36) (Figure 1). This demonstrates that the initial bacterial challenge was similar in test and
77 control specimens. At T₂₄, the silver coated discs had significantly reduced growth (0.64 ± 0.99
78 log₁₀ CFU/ml) which resulted in a difference of more than four log steps as compared to the non-
79 coated discs (4.60 ± 0.91 log₁₀ CFU/ml) (*P* <0.0001). Uncoated discs did not show any reduction
80 in the number of bacteria while the silver coating demonstrated a significant antimicrobial
81 efficacy and showed more than 99.98 % reduction in the number of CFU/ml after 24-hour
82 incubation.

83 Previous studies that have evaluated clinically relevant *Staphylococcus spp.* affecting
84 human beings rather than dogs, have shown excellent *in vitro* antimicrobial activity of different
85 formulations of silver coatings against *Staphylococcus aureus*, *Staphylococcus epidermidis*,
86 methicillin-resistant *Staphylococcus aureus* (MRSA), and methicillin-resistant *Staphylococcus*
87 *epidermidis* (MRSE) (6, 12). Khalilpour et al. (6) reported that Ag/SiO_xC_y coating showed a
88 significant *in vitro* antimicrobial activity against MRSA and *ex vivo* suppression of more than
89 99.9% of bacterial growth by the coating compared to non-coated samples after 28 days. Furkert
90 et al. (7) observed similar results during a study on *Staphylococcus epidermidis* where they
91 demonstrated that fixation pins coated with silver showed a 3-log step reduction in the number of
92 biofilm-forming bacteria compared to a non-coated stainless steel or titanium implant. Similarly,
93 the present study demonstrated that the new silver plasma coating was highly effective against

94 biofilm-forming MRSP and showed more than 99.98 % reduction in the number of CFU
95 compared with the non-coated specimens. This work is the first report of successful application
96 of silver coating technology to a MSRP isolate that is of direct relevance to canine orthopedics.

97 The antimicrobial activity of silver is dependent on the availability of free silver ions
98 (SI). In the presence of moisture, the embedded metallic silver particles (Ag^0) generate silver
99 ions (SI) which diffuse through the siloxane top layer to create an antimicrobial surface. The
100 pure metallic silver particles act as a depot of silver and provides a continuous and long term
101 generation of silver ions. SI strongly bind to cellular components such as enzymes and structural
102 proteins leading to altered function (8, 13, 14). Free SI interfere with bacterial cell metabolism
103 and disturb the integrity of the bacterial cell membrane (13, 15). Furthermore, SI can interact
104 with the DNA of bacteria, preventing bacterial replication (15). Antimicrobial coating of
105 surfaces with silver seems to reveal differences based on the size of the silver particles, which
106 are used. Meyer et al. (16) reported that the use of colloidal silver for coating of fixation pins
107 caused deficient antimicrobial effect. In contrast, nanoparticulate silver provides a larger active
108 surface area and a more homogeneous distribution of silver on biomaterials. The titanium
109 specimens used in this study were coated with a plasma polymer in which silver nanoparticles
110 (5–50 nm) were embedded. Our findings are similar to those demonstrated by Panáček et al. (13)
111 who reported that the smaller particles with a larger surface area available for interaction
112 provided a more efficient means of antibacterial activity than larger particles. It has been
113 reported that impregnation of silver into a coating can be more effective than direct surface
114 coating alone as surface silver can be deactivated by protein anions (14).

115 *In vitro* antibacterial efficiency of the silver coating and biofilm structure was secondarily
116 evaluated by scanning electron microscopy (SEM). Three titanium specimens (one silver-coated

117 and two control uncoated) were incubated separately, each in a petri dish containing 10 ml of
118 MRSP suspension in tryptic soy broth of $OD_{600} = 0.5$ for 24 hours aerobically at 37°C to initiate
119 biofilm formation. Following incubation, each specimen was washed by immersion in 10 ml of
120 PBS and then fixed with 2.5% glutaraldehyde in 0.1 M phosphate buffer; pH 7.4 at 4°C until
121 time of SEM imaging. The results obtained by SEM revealed no bacterial growth or biofilm
122 formation on the silver-coated specimen ($n = 1$) after 24 hours of incubation in strong biofilm
123 forming MRSP suspension, while biofilm formation was observed on the control uncoated
124 specimens ($n = 2$). The biofilm was characterized by micro colonies of bacteria along with large
125 amounts of irregularly extracellular polymeric substances (EPS) (Figure 2). Similar findings
126 were observed by Singh et al. (10). These SEM images correlated with the lower number of CFU
127 recovered on the silver-coated specimens after 24 hours of incubation compared to uncoated
128 specimens.

129 In conclusion, the results from this laboratory confirm the *in vitro* antimicrobial activity
130 of the silver impregnated coating against a strong biofilm-forming MRSP strain that was isolated
131 from a dog with an infected total knee replacement. Our findings suggest that this silver plasma
132 coating may represent a potentially valuable strategy for reducing adhesion of MRSP and
133 preventing implant-associated infections in dogs undergoing orthopedic surgery.

134

135 **References**

- 136 1. **DiCicco M, Neethirajan S, Singh A, et al.** Efficacy of clarithromycin on biofilm formation
137 of methicillin-resistant *Staphylococcus pseudintermedius*. BMC Vet Res 2012; 8:225-232.
- 138 2. **Vuong C, Otto M.** *Staphylococcus epidermidis* infections. Microbes Infect 2002; 4:481–489.

- 139 3. **Eugster S, Schawalder P, Gaschen F, et al.** A prospective study of postoperative surgical
140 site infections in dogs and cats. *Vet Surg* 2004; 33:542-550.
- 141 4. **Wettstein K, Descloux S, Rossano A, et al.** Emergence of methicillin-resistant
142 *Staphylococcus pseudintermedius* in Switzerland: three cases of urinary tract infections in
143 cats. *Schweiz Arch Tierheilkd* 2008; 150: 339-343.
- 144 5. **Zhao L, Chu PK, Zhang Y, et al.** Antibacterial coatings on titanium implants. *J Biomed*
145 *Mat Res B* 2009; 91:470-480.
- 146 6. **Khalilpour P, Lampe K, Wagener M, et al.** Ag/SiOxCy plasma polymer coating for
147 antimicrobial protection of fracture fixation devices. *J Biomed Mater Res B* 2010; 94(1):196-
148 202.
- 149 7. **Furkert FH, Sörensen JH, Arnoldi J, et al.** Antimicrobial Efficacy of Surface-Coated
150 External Fixation Pins. *Curr Microbiol* 2011; 62:1743-1751.
- 151 8. **Melaiye A, Youngs WJ.** Silver and its application as an antimicrobial agent. *Expert Opin*
152 *Ther Pat* 2005; 15:125-130.
- 153 9. **Stepanovich S, Vukovic D, Hola V, et al.** Quantification of biofilm in microtiter plates:
154 overview of testing conditions and practical recommendations for assessment of biofilm
155 production by staphylococci. *APMIS* 2007; 115:891-899.
- 156 10. **Singh A, Walker M, Rousseau J, et al.** Characterization of the biofilm forming ability of
157 *Staphylococcus pseudintermedius* from dogs. *BMC Vet Res* 2013; 9(1): 93-98.
- 158 11. **ASTM Standard E2180-07, 2012,** "Standard test method for determining the activity of
159 incorporated antimicrobial agent(s) in polymeric or hydrophobic materials," ASTM
160 International, West Conshohocken, PA, 2012, DOI: 10.1520/E2180-07R12, www.astm.org.

- 161 12. **Alt V, Bechert T, Steinrücke P, et al.** An in vitro assessment of the antibacterial properties
162 and cytotoxicity of nanoparticulate silver bone cement. *Biomaterials* 2004; 25:4383-4391.
- 163 13. **Panáček A, Kvítek L, Pucek R, et al.** Silver colloid nanoparticles: synthesis,
164 characterization, and their antibacterial activity. *J Phys Chem B* 2006; 110:16248-53.
- 165 14. **Furno F, Morley KS, Wong B, et al.** Silver nanoparticles and polymeric medical devices: a
166 new approach to prevention of infection? *J Antimicrob Chemother* 2004; 54:1019-1024.
- 167 15. **Damm C, Münstedt H, Rösch A.** The antimicrobial efficacy of polyamide 6/silver-nano-
168 and microcomposites. *Mater Chem Phys* 2008; 108:61-66.
- 169 16. **Meyer Ch, Keßler J, Alt V, et al.** Antimicrobial effect of silver-coated external fixator pins.
170 *Osteo Trauma Care* 2004; 12:81-84.

171

172

173 **Figure legends**

174 **Figure 1**

175 Antimicrobial efficiency of control uncoated and silver-coated specimens against biofilm
176 forming MRSP at T₀ and T₂₄ (log₁₀ CFU/ml). (*) significant difference at $p < 0.0001$.

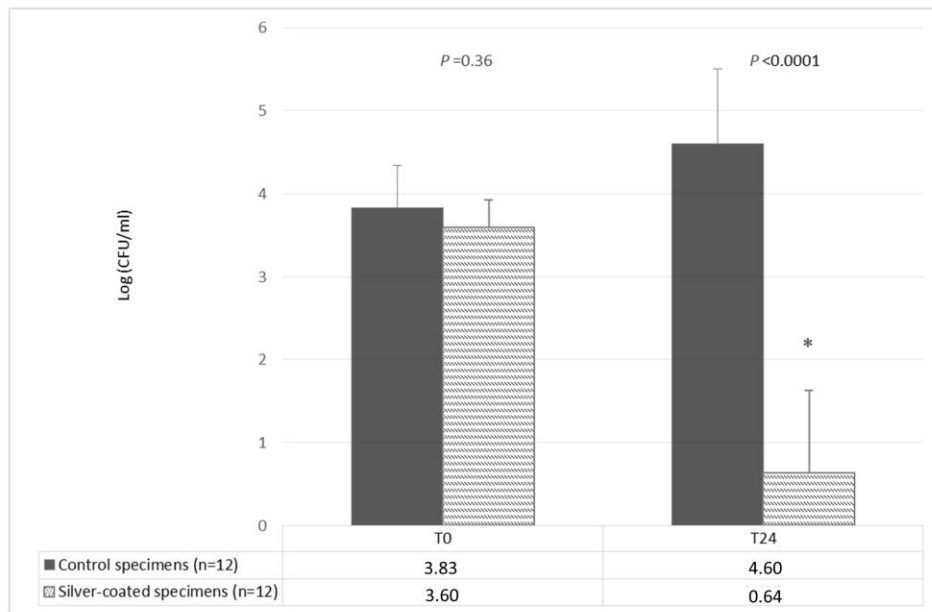
177

178

179 **Figure 2**

180 Scanning electron microscopy (SEM) of non-coated (left) and silver-coated (right) titanium
181 specimens inoculated with MRSP. The SEM images were taken at three different magnifications,
182 1000x, 2500x, 10000x (from top to bottom).

183

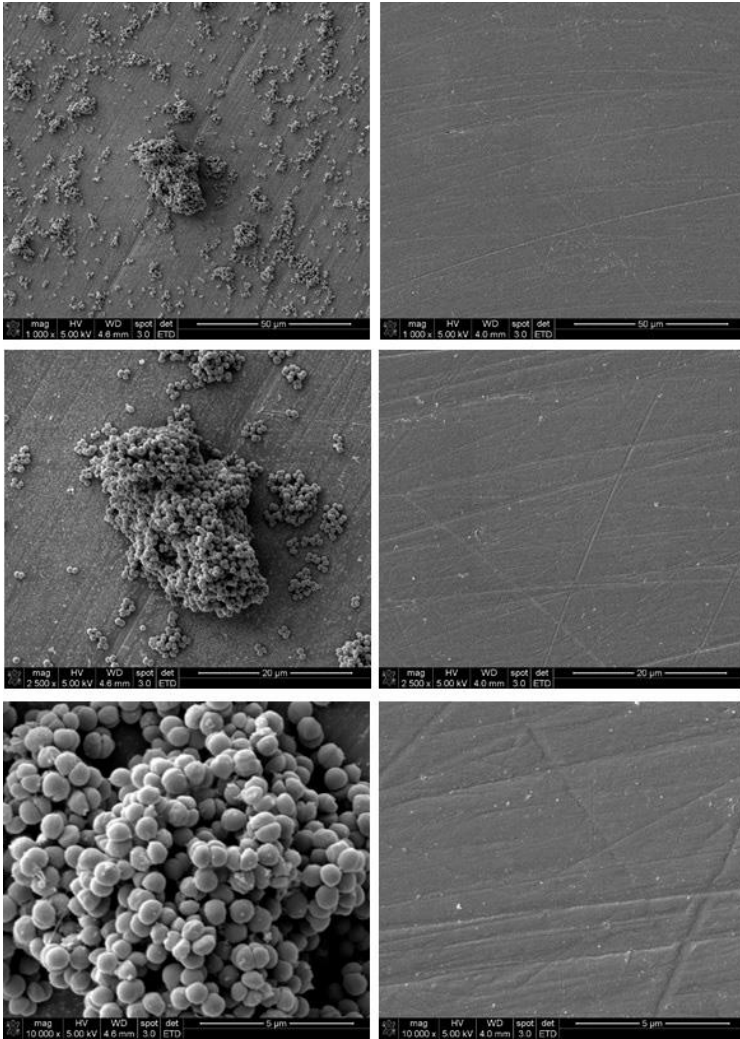


184

185 **Figure 1.** Antimicrobial efficiency of control uncoated and silver-coated specimens against
 186 biofilm forming MRSP at T₀ and T₂₄ (log₁₀ CFU/ml). (*) significant difference at $p < 0.0001$.

187

188



189

190

191 **Figure 2.** Scanning electron microscopy (SEM) of non-coated (left) and silver-coated (right)
192 titanium specimens inoculated with MRSP. The SEM images were taken at three different
193 magnifications, 1000x, 2500x, 10000x (from top to bottom).

194

195