The leap to ordinal: detailed functional prognosis after traumatic brain injury with a flexible modelling approach

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Abstract

When a patient is admitted to the intensive care unit (ICU) after a traumatic brain injury (TBI), an early prognosis is essential for baseline risk adjustment and shared decision making. TBI outcomes are commonly categorised by the Glasgow Outcome Scale – Extended (GOSE) into eight, ordered levels of functional recovery at 6 months after injury. Existing ICU prognostic models predict binary outcomes at a certain threshold of GOSE (e.g., prediction of survival [GOSE > 1]). We aimed to develop ordinal prediction models that concurrently predict probabilities of each GOSE score. From a prospective cohort (*n* = 1,550, 65 centres) in the ICU stratum of the Collaborative European NeuroTrauma Effectiveness Research in TBI (CENTER-TBI) patient dataset, we extracted all clinical information within 24 hours of ICU admission (1,151 predictors) and 6-month GOSE scores. We analysed the effect of two design elements on ordinal model performance: (1) the baseline predictor set, ranging from a concise set of ten validated predictors to a token-embedded representation of all possible predictors, and (2) the modelling strategy, from ordinal logistic regression to multinomial deep learning. With repeated *k*-fold cross-validation, we found that expanding the baseline predictor set significantly improved ordinal prediction performance while increasing analytical complexity did not. Half of these gains could be achieved with the addition of eight high-impact predictors to the concise set. At best, ordinal models achieved 0.76 (95% CI: 0.74 – 0.77) ordinal discrimination ability (ordinal *c*-index) and 57% (95% CI: 54% – 60%) explanation of ordinal variation in 6-month GOSE (Somers' D_{xy}). Model performance and the effect of expanding the predictor set decreased at higher GOSE thresholds, indicating the difficulty of predicting better functional outcomes shortly after ICU admission. Our results motivate the search for informative predictors that improve confidence in prognosis of higher GOSE and the development of ordinal dynamic prediction models.

Introduction

Globally, traumatic brain injury (TBI) is a major cause of death, disability, and economic burden [1]. The treatment of critically ill TBI patients is largely guided by an initial prognosis made within a day of admission to the intensive care unit (ICU) [2]. Early outcome prediction models set a baseline against which clinicians consider the effect of therapeutic strategies and compare patient trajectories. Therefore, well-calibrated and reliable prognostic models are an essential component of intensive care.

Outcome after TBI is most often evaluated on the ordered, eight-point Glasgow Outcome Scale – Extended (GOSE) [3-6], which stratifies patients by their highest level of functional recovery according to participation in daily activities. Existing baseline prediction models used in the ICU dichotomise the GOSE into binary endpoints for TBI outcome. For example, the Acute Physiologic Assessment and Chronic Health Evaluation (APACHE) II [7] model predicts in-hospital survival (GOSE > 1) while the International Mission for Prognosis and Analysis of Clinical Trials in TBI (IMPACT) [8] models focus on predicting functional independence (GOSE > 4, or 'favourable outcome') and survival at 6 months post-injury.

Dichotomised GOSE prediction employs a fixed threshold of favourability among the eight levels of recovery for all patients. However, there is no empirical justification for an ideal treatment-effect threshold of GOSE [9]. Moreover, dichotomisation removes each patient or caregiver's ability to define a different level of recovery as 'favourable' during prognosis. By concealing the nuanced differences in outcome defined by the GOSE, dichotomisation also limits the prognostic information made available during a shared treatment decision making process. For example, when clinicians, patients, or next of kin must together decide whether to withdraw life-sustaining measures (WLSM) after severe TBI, knowing the probability of different levels of functional recovery in addition to the baseline probability of survival would enable better quality-of-life consideration and confidence in the decision (**Fig 1B**) [10]. These problems of dichotomisation cannot be addressed simply by independently training a combination of binary prediction models at several GOSE thresholds. If model predictions are not constrained across the thresholds (i.e., ensuring probabilities do not increase with higher thresholds) during training, then combining multiple threshold outputs may result in nonsensical values. For example, the purported probability of survival (GOSE > 1) might be lower than that of recovering functional independence (GOSE > 4).

Fig 1. Comparison of ordinal outcome prediction to binary outcome prediction in terms of model architecture and clinical application. GOSE=Glasgow Outcome Scale – Extended at 6 months post-injury. ReLU=rectified linear unit. Pr(●)=Probability operator, i.e., "probability of ●." Pr(●|○)=Conditional probability operator, i.e., "probability of ●, given ○." (**A**) Output layer architectures of binary and ordinal GOSE prediction models. Ordinal prediction models must not only have a more complicated output structure (in terms of learned weights and outcome encoding choices) but also constrain probabilities across the possible levels of functional outcome (indicated by 'Constraint' in the ordinal model representations). The constraint for multinomial outcome encoding is performed with a softmax activation function while the constraint for ordinal outcome encoding is performed with subtractions of output values (implemented with a negative ReLU transformation) from lower thresholds. In the provided legend formula for the softmax activation function, z_i represents the outputted value of the i^{th} node of the multinomial outcome encoding layer (i.e., the node representing the i^{th} possible score of GOSE) preceding the softmax transformation. (**B**) A sample patient case to demonstrate the difference in prognostic information between ordinal and binary GOSE prediction models. Binary models predict outcomes at one GOSE threshold while ordinal models predict outcomes at every GOSE threshold concurrently and provide conditional predictions of higher GOSE threshold outcomes given lower GOSE threshold outcomes. Bespoke conditional probability diagrams can be constructed between any number of GOSE thresholds, as desired by model users, so long as lower thresholds (e.g., GOSE > 1) precede higher thresholds (e.g., GOSE > 3) in directionality. Conditional probabilities are calculated by dividing the model probability at the higher threshold by the model probability at the lower threshold (e.g., $\Pr(GOSE > 3 | GOSE > 1) = \Pr(GOSE > 3) / \Pr(GOSE > 1)$).

A practical solution would be to train ordinal outcome prediction models, which concurrently return probabilities at each GOSE threshold by learning the interdependent relationships between the predictor set and the possible levels of functional recovery (**Fig 1A**). Ordinal GOSE prediction models would allow users to interpret the probability of different levels of functional recovery. Additionally, they can provide insight into the conditional probability of obtaining greater levels of recovery given lower levels (see **Fig**

1B for a practical clinical application of this information). However, moving from binary to ordinal outcome prediction poses three key challenges. First, there is no guarantee that widely accepted TBI outcome predictor sets, validated either by binary or ordinal regression analysis, will be able to capture the nuanced differences between levels of functional recovery well enough for reliable prediction. Second, ordinal prediction models typically need to be more complicated than binary models to encode the possibility of more outcomes and the constrained relationship between them [11]. For GOSE prediction, ordinal models can either encode the outcomes as: (1) multinomial, in which nodes exist for each GOSE score and collectively undergo a softmax transformation (to constrain the sum of values to one) and probabilities are calculated by accumulating values up to each threshold, or (2) ordinal, in which nodes exist for each threshold between consecutive GOSE scores, constrained such that output values must not increase with higher thresholds, and probabilities for each threshold are calculated with a sigmoid transformation (**Fig 1A**). Third, assessment of prediction performance is not as intuitive with an ordinal outcome as with a binary outcome. Widely used dichotomous prediction performance metrics such as the *c*-index (i.e., the area under the receiver operating characteristic curve [AUC]) do not trivially extend to the ordinal case [12], so assessment of ordinal prediction models requires the consideration of multifactorial metrics and visualisations that may complicate interpretations of model performance [13].

As part of the Collaborative European NeuroTrauma Effectiveness Research in TBI (CENTER-TBI) project, we aim to address the challenges of ordinal outcome prediction. Our analyses cover a range of modelling strategies and predictors available within the first 24 hours of admission to the ICU.

Materials and methods

Study population and dataset

The study population was extracted from the ICU stratum of the core CENTER-TBI dataset (v3.0) using Opal database software [14]. The project objectives and experimental design of CENTER-TBI have been described in detail by Maas *et al*. [15] and Steyerberg *et al*. [16] Study patients were prospectively recruited at one of 65 participating ICUs across Europe with the following eligibility criteria: admission to the hospital within 24 hours of injury, indication for CT scanning, and informed consent according to local and national requirements.

Per project protocol, each patient's follow-up schedule included a GOSE assessment at 6 months post-injury, or, more precisely, within a window of 5-8 months post-injury. GOSE assessments were conducted using structured interviews [6] and patient/carer questionnaires [17] by the clinical research team of CENTER-TBI. The eight, ordinal scores of GOSE, representing the highest levels of functional recovery, are decoded in the heading of **Table 1**. Since patient/carer questionnaires do not distinguish vegetative patients (GOSE = 2) into a separate category, GOSE scores 2 and 3 (lower severe disability) were combined to one category (GOSE $\in \{2,3\}$) in our dataset. Of the 2,138 ICU patients in the CENTER-TBI dataset available for analysis, we excluded patients in

the following order: (1) age less than 16 years at ICU admission (n = 82), (2) follow-up GOSE was unavailable (n = 283), and (3) ICU stay was less than 24 hours (n = 223). Our resulting sample size was n = 1,550. For 1,351 patients (87.2%), either the patient died during ICU stay (n = 205) or results from a GOSE evaluation at 5 – 8 months post-injury were available in the dataset (n = 1,146). For the remaining 199 patients (12.8%), GOSE scores were imputed using a Markov multi-state model based on the observed GOSE scores recorded at different timepoints between 2 weeks to one-year post-injury [18]. A flow diagram for study inclusion and follow-up is provided in **S1 Fig**, and summary characteristics of the study population are detailed in **Table 1**.

Table 1. Summary characteristics of the study population at ICU admission stratified by ordinal 6-month outcomes.

Summary characteristics	Overall	Glasgow Outcome Scale – Extended (GOSE) at 6 months post-injury							*p*-value‡
		(1) Death	**(2 or 3)** Vegetative or lower severe disability	**(4)** Upper severe disability	**(5)** Lower moderate disability	**(6)** Upper moderate disability	**(7)** Lower good recovery	**(8)** Upper good recovery	
*n**	1550	318 (20.5%)	262 (16.9%)	120 (7.7%)	227 (14.6%)	200 (12.9%)	206 (13.3%)	217 (14.0%)	
Age [years]	51 (31–66)	66 (50–76)	55 (36–68)	48 (29–61)	44 (31–56)	41 (27–53)	48 (31–65)	41 (24–61)	<0.0001
Sex									0.59
Female	409 (26.4%)	78 (24.5%)	71 (27.1%)	43 (35.8%)	64 (28.2%)	49 (24.5%)	59 (28.6%)	45 (20.7%)	
Race ($n^{\dagger}$ = 1427)									0.13
White	1386 (97.1%)	281 (97.2%)	239 (96.8%)	106 (95.5%)	195 (96.5%)	183 (97.3%)	184 (98.4%)	198 (97.5%)	
Black	21 (1.5%)	2 (0.7%)	4 (1.6%)	3 (2.7%)	5 (2.5%)	3 (1.6%)	2 (1.1%)	2 (1.0%)	
Asian	20 (1.4%)	6 (2.1%)	4 (1.6%)	2 (1.8%)	2 (1.0%)	2 (1.1%)	1 (0.5%)	3 (1.5%)	
Baseline GCS ($n^{\dagger}$ = 1465)	8 (4–14)	5 (3–10)	6 (3–10)	8 (4–13)	8 (5–13)	9 (6–14)	13 (7–15)	13 (8–15)	<0.0001
Mild [13–15]	390 (26.6%)	30 (10.3%)	38 (15.3%)	26 (23.4%)	42 (19.5%)	66 (34.9%)	91 (45.3%)	97 (46.4%)	
Moderate [9–12]	331 (22.6%)	65 (22.3%)	41 (16.5%)	28 (25.2%)	65 (30.2%)	36 (19.0%)	40 (19.9%)	56 (26.8%)	
Severe [3–8]	744 (50.8%)	196 (67.4%)	170 (68.3%)	57 (51.4%)	108 (50.2%)	87 (46.0%)	70 (34.8%)	56 (26.8%)	

Data are median (IQR) for continuous characteristics and *n* (% of column group) for categorical characteristics, unless otherwise indicated. Units or numerical definitions of characteristics are provided in square brackets. Baseline GCS=Glasgow Coma Scale at ICU admission, from 3 to 15. Conventionally, TBI severity is categorically defined by baseline GCS scores as indicated in square brackets.

*Percentages for sample size (*n*) represent proportion of study sample size in each GOSE group.

†Limited sample size of non-missing values for characteristic.

‡*p*-values are determined from proportional odds logistic regression (POLR) coefficient analysis trained on all summary characteristics concurrently [19]. For categorical variables with $k > 2$ categories (e.g., Race), *p*-values were calculated with a likelihood ratio test (with k-1 degrees of freedom) on POLR.

Repeated *k*-fold cross-validation

We implemented the 'scikit-learn' module (v0.23.2) [20] in Python (v3.7.6) to create 100 stratified partitions of our study population for repeated *k*-fold cross-validation (20 repeats, 5 folds). Within each of the partitions, approximately 80% of the population would constitute the training set ($n \approx 1{,}240$ patients) and 20% of the population would constitute the corresponding testing set ($n \approx 310$ patients). For parametric (i.e., deep learning) models, we implemented a stratified shuffle split on each of the 100 training sets to set 15% ($n \approx 46$ patients) aside for validation and hyperparameter optimisation.

Selection and preparation of concise predictor set

In selecting a concise predictor set, our primary aim was to find a small group of well-validated, widely measured clinical variables that are commonly used for TBI outcome prognosis in existing ICU practice. We selected the ten predictors from the extended IMPACT binary prediction model [8] for moderate-to-severe TBI – defined by a baseline Glasgow Coma Scale (GCS) [21,22] score between 3 and 12, inclusive – to represent our concise set. While 26.6% of our study population falls out of this GCS range (**Table 1**), we find that the IMPACT predictor set is the most rigorously validated [23-27] baseline set available for the overall critically ill TBI population. The ten predictors, characterised in **Table 2**, are all measured within 24 hours of ICU admission and include demographic characteristics, clinical severity scores, CT characteristics, and laboratory measurements. The predictors as well as empirical justification for their inclusion in the IMPACT model have been described in detail [28]. In this manuscript, each of the models trained on the IMPACT predictor set is denoted as a concise-predictor-based model (CPM).

Table 2. Concise baseline predictors of the study population stratified by ordinal 6-month outcomes.

Concise predictors	Overall (n = 1550)	Glasgow Outcome Scale – Extended (GOSE) at 6 months post-injury							p-value‡
		1 (n = 318)	2 or 3 (n = 262)	4 (n = 120)	5 (n = 227)	6 (n = 200)	7 (n = 206)	8 (n = 217)	
Age [years]	51 (31–66)	66 (50–76)	55 (36–68)	48 (29–61)	44 (31–56)	41 (27–53)	48 (31–65)	41 (24–61)	<0.0001
GCSm (n† = 1509)	5 (1–6)	2 (1–5)	3 (1–5)	5 (1–6)	5 (1–6)	5 (2–6)	5 (3–6)	6 (5–6)	<0.0001
(1) No response	484 (32.1%)	152 (50.0%)	104 (40.6%)	35 (29.9%)	63 (28.5%)	46 (23.6%)	47 (23.0%)	37 (17.5%)	
(2) Abnormal extension	54 (3.6%)	17 (5.6%)	20 (7.8%)	4 (3.4%)	6 (2.7%)	3 (1.5%)	2 (1.0%)	2 (0.9%)	
(3) Abnormal flexion	63 (4.2%)	14 (4.6%)	12 (4.7%)	8 (6.8%)	11 (5.0%)	8 (4.1%)	4 (2.0%)	6 (2.8%)	
(4) Withdrawal from stimulus	114 (7.6%)	27 (8.9%)	23 (9.0%)	8 (6.8%)	20 (9.0%)	21 (10.8%)	8 (3.9%)	7 (3.3%)	
(5) Movement localised to stimulus	305 (20.2%)	52 (17.1%)	47 (18.4%)	24 (20.5%)	50 (22.6%)	46 (23.6%)	44 (21.6%)	42 (19.8%)	
(6) Obeys commands	489 (32.4%)	42 (13.8%)	50 (19.5%)	38 (32.5%)	71 (32.1%)	71 (36.4%)	99 (48.5%)	118 (55.7%)	
Unreactive pupils (n† = 1465)									<0.0001
One	111 (7.6%)	31 (10.5%)	31 (12.3%)	7 (6.3%)	20 (9.3%)	5 (2.6%)	8 (4.1%)	9 (4.4%)	
Two	168 (11.5%)	84 (28.5%)	33 (13.0%)	8 (7.2%)	14 (6.5%)	8 (4.2%)	16 (8.2%)	5 (2.4%)	
Hypoxia	207 (13.4%)	60 (18.9%)	33 (12.6%)	14 (11.7%)	35 (15.4%)	33 (16.5%)	16 (7.8%)	16 (7.4%)	0.37
Hypotension	210 (13.5%)	56 (17.6%)	51 (19.5%)	21 (17.5%)	32 (14.1%)	22 (11.0%)	15 (7.3%)	13 (6.0%)	0.0038
Marshall CT (n† = 1255)	VI (II–VI)	III (II–VI)	II (II–VI)	II (II–VI)	II (II–II)	II (II–III)	II (II–II)	VI (II–VI)	0.043
No visible pathology (I)	118 (9.4%)	8 (3.3%)	11 (5.3%)	5 (5.2%)	17 (8.7%)	25 (15.2%)	24 (13.6%)	28 (16.5%)	
Diffuse injury II	592 (47.2%)	56 (22.8%)	84 (40.6%)	54 (56.2%)	92 (47.2%)	100 (60.6%)	103 (58.5%)	103 (60.6%)	
Diffuse injury III	108 (8.6%)	42 (17.1%)	17 (8.2%)	10 (10.4%)	14 (7.2%)	9 (5.5%)	6 (3.4%)	10 (5.9%)	
Diffuse injury IV	16 (1.3%)	7 (2.8%)	1 (0.5%)	1 (1.0%)	4 (2.1%)	1 (0.6%)	1 (0.6%)	1 (0.6%)	
Mass lesion (V & VI)	421 (33.5%)	133 (54.0%)	94 (45.4%)	26 (27.1%)	68 (34.9%)	30 (18.2%)	42 (23.9%)	28 (16.5%)	
tSAH (n† = 1254)	957 (76.3%)	221 (90.2%)	176 (84.2%)	73 (76.0%)	150 (76.9%)	106 (63.9%)	125 (71.4%)	106 (63.1%)	0.16
EDH (n† = 1257)	244 (19.4%)	31 (12.7%)	32 (15.3%)	21 (21.9%)	46 (23.6%)	32 (19.3%)	42 (23.9%)	40 (23.5%)	0.016
Glucose [mmol/L] (n† = 1062)	7.7 (6.6–9.4)	8.8 (7.3–11)	8.0 (6.5–9.8)	7.6 (6.5–9.3)	7.8 (6.6–9.6)	7.7 (6.5–8.7)	7.3 (6.3–8.5)	7.1 (6.3–8.1)	0.013
Hb [g/dL] (n† = 1140)	13 (12–14)	13 (11–14)	13 (11–14)	14 (12–14)	13 (12–14)	14 (12–15)	13 (12–15)	14 (13–15)	0.038

Data are median (IQR) for continuous characteristics and n (% of column group) for categorical characteristics. Units of characteristics are provided in square brackets. GCSm=motor component score of the Glasgow Coma Scale. Marshall CT=Marshall computerised tomography classification. tSAH=traumatic subarachnoid haemorrhage. EDH=extradural haematoma. Hb=haemoglobin.

†Limited sample size of non-missing values for characteristic.

‡p-values are determined from proportional odds logistic regression (POLR) analysis trained on all concise predictors concurrently [19] and are combined across 100 missing value imputations via z-transformation [29]. For categorical variables with $k > 2$ categories (e.g., GCSm), p-values were calculated with a likelihood ratio test (with k-1 degrees of freedom) on POLR.

Seven of the concise predictors had missing values for some of the patients in our study population (**S2 Fig**). In each repeated cross-validation partition, we trained an independent, stochastic predictive mean matching imputation function on the training set and imputed all missing values across both sets using the 'mice' package (v3.9.0) [30] in R (v4.0.0) [31]. The result was a multiply imputed (m = 100) dataset with a unique imputation per partition, allowing us to simultaneously account for the variability due to resampling and the variability due to missing value imputation during repeated cross-validation.

Prior to the training of CPMs, each of the multi-categorical variables (i.e., GCSm, Marshall CT, and unreactive pupils in **Table 2**) were one-hot encoded and each of the continuous variables (i.e., age, glucose, and haemoglobin) were standardised based on the mean and standard deviation of each of the training sets with the 'scikit-learn' module in Python.

Selection of concise-predictor-based models (CPMs)

We tested four CPM types, each denoted by a subscript: (1) multinomial logistic regression (CPM_{MNLR}), (2) proportional odds (i.e., ordinal) logistic regression (CPM_{POLR}), (3) class-weighted feedforward neural network with a multinomial (i.e., softmax) output layer (CPM_{DeepMN}), and (4) class-weighted feedforward neural network with an ordinal (i.e., constrained sigmoid at each threshold) output layer (CPM_{DeepOR}). These models were selected because, in the setting of ordinal GOSE prediction, we wished to compare the performance of: (1) nonparametric logistic regression models (CPM_{MNLR} and CPM_{POLR}) to nonlinear, parametric deep learning networks (CPM_{DeepMN} and CPM_{DeepOR}), and (2) multinomial outcome encoding (CPM_{MNLR} and CPM_{DeepMN}) to ordinal outcome encoding (CPM_{POLR} and CPM_{DeepOR}). Each of these model types returns a predicted probability for each of the GOSE thresholds at 6 months post-injury from the concise set of predictors (**Fig 1A**). A detailed explanation of CPM architectures, hyperparameters for the parametric CPMs, loss functions, and optimisation algorithms is provided in **S1 Appendix**.

CPM_{Best} denotes the optimal CPM for a given performance metric in the **Results**. CPM_{MNLR} and CPM_{POLR} were implemented with the 'statsmodels' module (dev. v0.14.0) [32] in Python, and CPM_{DeepMN} and CPM_{DeepOR} were implemented with the 'PyTorch' (v1.10.0) [33] module in Python.

Design of all-predictor-based models (APMs)

In contrast to the CPMs, we designed and trained prediction models on all baseline (i.e., available to ICU clinicians at 24 hours post-admission) clinical information (excluding high-resolution data such as full brain images or physiological waveforms) in the CENTER-TBI database. Each of these models is designated as an all-predictor-based model (APM).

For our study population, there are 1,151 predictors [34], each being in one of the 14 categories listed in **Table 3**, with variable levels of missingness and frequency per patient.

This information also includes 81 predictors denoting treatments or interventions within the first 24 hours of ICU care (e.g., type and dose of medication administered) and 76 predictors denoting the explicit impressions or rationales of ICU physicians (e.g., reason for surgical intervention and expected prognosis with or without surgery).

Table 3. Predictor baseline tokens per patient in the CENTER-TBI dataset.

Predictor category	Types of tokens				
	All	Fixed at ICU admission	Continuous variable	Treatments and interventions	Physician impression or rationale
Emergency care and ICU admission	112 (103–121)	112 (103–121)	13 (10–16)	0 (0–0)	7 (7–8)
Brain imaging	94 (72–114)	74 (68–83)	5 (2–8)	0 (0–0)	9 (8–10)
ICU monitoring and management	63 (52–72)	3 (3–3)	10 (5–13)	40 (34–46)	13 (3–15)
Injury characteristics and severity	55 (49–62)	55 (49–62)	2 (2–2)	0 (0–0)	0 (0–0)
End-of-day assessments	50 (45–54)	0 (0–0)	19 (17–21)	0 (0–0)	0 (0–0)
Laboratory measurements	44 (32–55)	14 (0–20)	42 (31–52)	0 (0–0)	1 (1–1)
Medical and behavioural history	38 (32–51)	38 (32–51)	0 (0–1)	0 (0–0)	0 (0–0)
Medications	30 (21–40)	0 (0–0)	0 (0–0)	22 (15–30)	8 (5–11)
Bihourly assessments	17 (0–32)	0 (0–0)	15 (0–27)	1 (0–2)	0 (0–0)
Demographics and socioeconomic status	15 (14–16)	15 (14–16)	2 (1–2)	0 (0–0)	0 (0–0)
Protein biomarkers	5 (5–5)	0 (0–0)	5 (5–5)	0 (0–0)	0 (0–0)
Surgery	2 (1–6)	1 (1–2)	0 (0–0)	0 (0–1)	1 (0–3)
Haemostatic markers*	0 (0–0)	0 (0–0)	0 (0–0)	0 (0–0)	0 (0–0)
Transitions of care*	0 (0–0)	0 (0–0)	0 (0–0)	0 (0–0)	0 (0–0)
All predictors	532 (486–580)	315 (288–341)	111 (90–132)	64 (50–75)	37 (29–44)

Data represent median (IQR) number of non-missing, unique tokens per patient. Tokens were extracted from the clinical information available up to 24 hours after ICU admission for each study patient in the Collaborative European NeuroTrauma Effectiveness Research in TBI (CENTER-TBI) project dataset. Each token may be of only one predictor category (leftmost column) and of any number of token types (four rightmost columns). ICU=intensive care unit.
*Due to their relative infrequency in the CENTER-TBI dataset, these baseline predictor categories have a 3rd quartile of zero tokens per patient.

To prepare this information into a suitable format for training APMs, we tokenised and embedded heterogenous patient data [35] in a process visualised in **Fig 2**. Predictor tokens were constructed in one of the following ways: (1) for categorical predictors, a token was constructed by concatenating the predictor name and value, e.g., 'GCSTotalScore_04,' (2) for continuous predictors, a token was constructed by learning the distribution of that predictor from the training set and discretising into 20 quantile bins, e.g., 'SystolicBloodPressure_BIN17,' (3) for text-based entries, we removed all special characters, spaces, and capitalisation from the text and appended the unformatted text to the predictor name, e.g., 'InjuryDescription_skullfracture,' and (4) for missing values, a separate token was created to designate missingness, e.g., 'PriorMedications_NA' (**Fig 2A**). The unique tokens from a patient's first 24 hours of ICU stay made up his or her

individual predictor set, and the median number of unique tokens (excluding missing value tokens) per patient per predictor category are provided in **Table 3**. Notably, this process does not require any data cleaning, missing value imputation, outlier removal, or domain-specific knowledge for a large set of variables and imposes no constraints on the number or type of predictors per patients [35]. Additionally, by including missing value tokens, models can discover meaningful patterns of missingness if they exist [36].

Fig 2. Tokenisation and embedding procedure for the development of ordinal all-predictor-based models (APMs). ICU=intensive care unit. ER=emergency room. Hx=history. SES=socioeconomic status. CSF=cerebrospinal fluid. GOSE=Glasgow Outcome Scale – Extended at 6 months post-injury. (**A**) Process of converting all clinical information, from the first 24 hours of each patient, into an indexed dictionary of tokens during model training. The tokenisation process is illustrated with three example predictors and their associated values in step 2. The first entry in the trained token dictionary ('0) <unrecognised>') of step 3 is a placeholder token for any tokens encountered in the testing set that were not seen in the training set. (**B**) Visual representation of token embedding and significance-weighted averaging pipeline during APM prediction runs. After tokenising an individual patient's clinical information, the vector of tokens is converted to a vector of the indices corresponding to each token in the trained token dictionary. The corresponding vectors and significance weights of the indices are extracted to weight-average the patient information into a single vector. The embedding layer and significance weights are learned through stochastic gradient descent during model training, and significance weights are constrained to be positive with an exponential function. While not explicitly shown, the weighted vectors are divided by the number of vectors during weight-averaging. The individual, weight-averaged vector then feeds into an ordinal prediction model to return probabilities at each GOSE threshold. The ordinal prediction model could either have multinomial output encoding (APM_{MN}) or ordinal outcome encoding (APM_{OR}), as represented in **Fig 1A**.

Taking inspiration from artificially intelligent (AI) natural language processing [37,38], all the predictor tokens from the training set (excluding the validation set) are used to construct a token dictionary. APMs learn a lower dimensional vector as well as a positive significance weight for each entry in the dictionary during training. The vectors for each of the tokens of a single patient are significance-weight-averaged into a single vector which is then fed into a class-weighted feedforward neural network (**Fig 2B**). If the neural network has no hidden layers, then the APM is analogous to logistic regression, while if it does have hidden layers, the APM corresponds to deep learning. In this work, we train APMs with one of two kinds of output layers: multinomial, i.e., softmax, (APM_{MN}), or ordinal, i.e., constrained sigmoid at each GOSE threshold, (APM_{OR}). Both model types output a predicted probability for each of the GOSE thresholds at 6 months post-injury. A detailed explanation of APM architectures, hyperparameters, loss functions, and optimisation algorithms is provided in **S2 Appendix**.

APM_{Best} denotes the optimal APM for a given performance metric in the **Results**. APM_{MN} and APM_{OR} were implemented with the 'PyTorch' module in Python.

Predictor importance in all-predictor-based models (APMs)

The relative importance of predictor tokens in the trained APMs was measured with absolute Shapley additive explanation (SHAP) [39] values, which, in our case, can be

interpreted as the magnitude of the relative contribution of a token towards a model output for a single patient. For APM_{MN}, this corresponds to the predictor contributions towards each node (after softmax transformation, **Fig 1A**) corresponding to the probability at a GOSE score. For APM_{OR}, this corresponds to the predictor contributions towards each node (after sigmoid transformation, **Fig 1A**) corresponding to the probability at a GOSE threshold. Absolute SHAP values were measured for each patient in the testing set of every repeated cross-validation partition, and we averaged these values over the partitions to derive our individualised importance scores per token. These scores were averaged, once again, over the entire patient set to calculate the mean absolute SHAP values of each token. Finally, to derive importance scores for each predictor, we calculated the maximum of the mean absolute SHAP values of the possible tokens from the predictor.

Selection and preparation of extended concise predictor set

We selected a small set of the most important APM predictors by mean absolute SHAP values to add to the concise predictor set and observe the change in model performance. Since the concise predictor set does not include any information on intervention decisions or physician impressions from the first day, we did not consider these predictor types. Moreover, for every multi-categorical predictor selected, we examined the mean absolute SHAP values of each of the predictor's possible tokens to determine which of the categories should be explicitly encoded (e.g., including 10 categories for employment status or just one indicator variable for retirement). The extended concise predictor set, including the 10 original concise predictors and the 8 added predictors, in our study population is listed and characterised in **S1 Table**. Each of the models trained on the concise set with these variables added is denoted as an extended concise-predictor-based model (eCPM).

The process of multiple imputation (m = 100), one-hot encoding, and standardisation of the extended concise predictor set was identical to that of the concise predictor set, as described earlier.

Selection of extended concise-predictor-based models (eCPMs)

The four eCPM model types we tested are identical to the four CPM model types, as described earlier and in **S1 Appendix** with, however, the extended concise predictor set: (1) multinomial logistic regression ($eCPM_{MNLR}$), (2) proportional odds (i.e., ordinal) logistic regression ($eCPM_{POLR}$), (3) class-weighted feedforward neural network with a multinomial (i.e., softmax) output layer ($eCPM_{DeepMN}$), and (4) class-weighted feedforward neural network with an ordinal (i.e., constrained sigmoid at each threshold) output layer ($eCPM_{DeepOR}$).

$eCPM_{Best}$ denotes the optimal eCPM for a given performance metric in the **Results**.

Assessment of model discrimination and calibration

All model metrics, curves, and associated confidence intervals (CI) were calculated from testing set predictions using the repeated Bootstrap Bias Corrected Cross-Validation (BBC-CV) method [40] with 1,000 resamples of unique patients for bootstrapping. The collection of metrics from the bootstrapped testing set resamples for each model then formed our unbiased estimation distribution for statistical inference (i.e., CI).

In this work, we assess model discrimination performance (i.e., how well do the models separate patients with different GOSE scores?) and probability calibration (i.e., how reliable are the predicted probabilities at each threshold?). The metrics and visualisations are explained in detail, with mathematical derivation and intuitive examples, in **S3 Appendix**. In this section, we will only list the metrics, their interpretations, and their range of feasible values. Feasible values range from the value corresponding to no model information or random guessing (i.e., the no information value [NIV]) to the value corresponding to ideal model performance (i.e., the full information value [FIV]).

Our primary metric of model discrimination performance is the ordinal *c*-index (ORC) [13]. ORC has two interpretations: (1) the probability that a model correctly separates two patients with two randomly chosen GOSE scores and (2) the average proportional closeness between a model's functional outcome ranking of a set of patients (which includes one randomly chosen patient from each possible GOSE score) to their true functional outcome ranking. In addition, we calculate Somers' D_{xy} [41,42], which is interpreted as the proportion of ordinal variation in GOSE that can be explained by the variation in model output. Our final metrics of model discrimination are dichotomous *c*-indices (i.e., AUC) at each threshold of GOSE. Each is interpreted as the probability of a model correctly discriminating a patient with GOSE above the threshold from one with GOSE below. The range of feasible values for each discrimination metric are: NIV_{ORC} = 0.5 to FIV_{ORC} = 1, $NIV_{Somers'\ Dxy}$ = 0 to $FIV_{Somers'\ Dxy}$ = 1, and $NIV_{Dichotomous\ c\text{-}index}$ = 0.5 to $FIV_{Dichotomous\ c\text{-}index}$ = 1. ORC is the only discrimination metric that is independent of the sample prevalence of each GOSE category [13].

To assess the calibration of predicted probabilities at each GOSE threshold, we use the logistic recalibration framework [43] to measure calibration slope [44]. A calibration slope less than one indicates overfitting (i.e., high predicted probabilities are overestimated while low predicted probabilities are underestimated) while a calibration slope greater than one indicates underfitting [45]. We also examine smoothed probability calibration curves [46] to detect miscalibrations that may be overlooked by the logistic recalibration framework [45]. The ideal calibration curve is a diagonal line with slope one and *y*-intercept 0 while one indicative of random guessing would be a horizontal line with a *y*-intercept at the proportion of the study population above the given threshold. We accompany each calibration curve with the integrated calibration index (ICI) [47], which is the mean absolute error between the smoothed and the ideal calibration curves, to aid comparison of curves across model types. FIV_{ICI} = 0, but NIV_{ICI} varies based on the outcome distribution at each threshold (**S3 Appendix**).

All metrics were calculated using the 'scikit-learn' and 'SciPy' (v1.6.2) [48] modules in Python and figures were plotted using the 'ggplot2' package (v3.3.2) [49] in R.

Computational resources

All computational and statistical components of this work were performed in parallel on the Cambridge Service for Data Driven Discovery (CSD3) high performance computer, operated by the University of Cambridge Research Computing Service (http://www.hpc.cam.ac.uk). The training of each APM was accelerated with graphical processing units and the 'PyTorch Lightning' (v1.5.0) [50] module. The training of all parametric models (CPM_{DeepMN}, CPM_{DeepOR}, APM_{MN}, APM_{OR}, $eCPM_{DeepMN}$, and $eCPM_{DeepOR}$) was made more efficient by dropping out consistently underperforming parametric configurations, on the validation sets, with the Bootstrap Bias Corrected with Dropping Cross-Validation (BBCD-CV) method [40] with 1,000 resamples of unique patients. The results of hyperparameter optimisation are detailed in **S4 Appendix**.

Results

CPM and APM discrimination performance

The discrimination performance metrics for each CPM are listed in **S2 Table**. Deep learning models (CPM_{DeepMN} and CPM_{DeepOR}) made no significant improvement (based on 95% CI) over logistic regression models (CPM_{MNLR} and CPM_{POLR}). The only significant difference in discrimination among the model types was observed in CPM_{DeepOR}, which had a significantly lower ORC and Somers' D_{xy} than the other models. The discrimination performance metrics for each APM are listed in **S3 Table**. APM_{MN} had a significantly higher ORC, Somers' D_{xy}, and dichotomous *c*-indices at lower GOSE thresholds (i.e., GOSE > 1 and GOSE > 3) than did APM_{OR}. Moreover, in **S4 Appendix**, we see that the best-performing parametric configurations of APM_{MN} did not contain additional hidden layers between the token embedding and output layers. Our results of performance within predictor sets consistently demonstrate that increasing analytical complexity, in terms of using deep learning (for CPMs) or adding hidden network layers (for APMs), did not improve discrimination of outcomes. In the case of deep learning models, multinomial outcome encoding significantly outperformed ordinal outcome encoding (**Fig 1A**).

The discrimination performance metrics of the best-performing CPMs (CPM_{Best}), compared with those of the best-performing APMs (APM_{Best}), are listed in **Table 4**. In contrast to the case of analytical complexity, we observe that expanding the predictor set yielded a significant improvement in ORC, Somers' D_{xy}, and each threshold-level dichotomous *c*-index except for those of the highest GOSE thresholds (i.e., GOSE > 6 and GOSE > 7). On average, models trained on the concise predictor set (CPMs) correctly separated two randomly selected patients from two randomly selected GOSE categories 70% (95% CI: 68% – 71%) of the time, while models trained on all baseline predictors (APMs) in the CENTER-TBI dataset did so 76% (95% CI: 74% – 77%) of the time. These percentages also correspond to the average proportional closeness of

predicted rankings to true GOSE rankings of patient sets. CPM_{Best} explained 44% (95% CI: 41% – 48%) of the ordinal variation in GOSE while APM_{Best} explained 57% (95% CI: 54% – 60%) in their respective model outputs. At increasing GOSE thresholds, the dichotomous *c*-indices of CPM_{Best} and APM_{Best}, as well as the gap between them, consistently decreased (**Table 4**). This signifies that predicting higher 6-month functional outcomes is more difficult than predicting lower 6-month functional outcomes. Moreover, the gains in discrimination earned from expanding the predictor set mostly come from improved performance at lower GOSE thresholds (i.e., predicting survival, return of consciousness, or recovery of functional independence).

Table 4. Best ordinal model discrimination and calibration performance per predictor set.

Metric	Threshold	Model		
		CPM_{Best}	**APM_{Best}**	**$eCPM_{Best}$**
Ordinal *c*-index (ORC)		0.70 (0.68–0.71)	0.76 (0.74–0.77)	0.73 (0.71–0.74)
Somers' D_{xy}		0.44 (0.41–0.48)	0.57 (0.54–0.60)	0.50 (0.46–0.54)
Threshold-level dichotomous *c*-index*		0.77 (0.75–0.78)	0.82 (0.80–0.83)	0.79 (0.78–0.80)
	GOSE > 1	0.83 (0.81–0.85)	0.90 (0.88–0.92)	0.86 (0.84–0.87)
	GOSE > 3	0.81 (0.79–0.83)	0.86 (0.84–0.88)	0.84 (0.83–0.86)
	GOSE > 4	0.78 (0.76–0.80)	0.83 (0.80–0.85)	0.82 (0.80–0.83)
	GOSE > 5	0.76 (0.74–0.77)	0.80 (0.78–0.83)	0.77 (0.75–0.79)
	GOSE > 6	0.72 (0.70–0.74)	0.76 (0.73–0.79)	0.75 (0.73–0.77)
	GOSE > 7	0.72 (0.69–0.74)	0.75 (0.72–0.79)	0.72 (0.70–0.75)
Threshold-level calibration slope*		0.98 (0.81–1.12)	0.84 (0.76–0.91)	1.00 (0.78–1.14)
	GOSE > 1	0.95 (0.78–1.10)	0.98 (0.86–1.10)	0.98 (0.78–1.14)
	GOSE > 3	0.97 (0.80–1.12)	0.90 (0.80–1.02)	1.05 (0.81–1.20)
	GOSE > 4	1.06 (0.86–1.23)	0.89 (0.79–1.00)	1.10 (0.85–1.27)
	GOSE > 5	1.01 (0.78–1.21)	0.82 (0.72–0.94)	1.01 (0.76–1.22)
	GOSE > 6	0.98 (0.73–1.20)	0.74 (0.62–0.87)	0.97 (0.70–1.20)
	GOSE > 7	0.92 (0.69–1.18)	0.68 (0.54–0.83)	0.89 (0.61–1.18)

Data represent mean (95% confidence interval) for the best-performing model, per predictor set, based on a given metric. For threshold-level metrics, a single best-performing model, per predictor set, was determined by the overall unweighted average across the thresholds. Interpretations for each metric are provided in **Materials and methods**. Mean and confidence interval values were derived using bias-corrected bootstrapping (1,000 resamples) and represent the variation across repeated *k*-fold cross-validation folds (20 repeats of 5 folds) and, for the concise-predictor-based model (CPM) and the extended concise-predictor-based model (eCPM), 100 missing value imputations. CPM_{Best}=CPM with best value for given metric (**S2 Table**). APM_{Best}=all-predictor-based model (APM) with best value for given metric (**S3 Table**). $eCPM_{Best}$=eCPM with best value for given metric (**S4 Table**). GOSE=Glasgow Outcome Scale – Extended at 6 months post-injury. *Values in these rows correspond to the unweighted average across all GOSE thresholds.

CPM and APM calibration performance

The calibration slopes and calibration curves for each CPM are displayed in **S2 Table** and **S3 Fig**, respectively. Both logistic regression CPMs (CPM_{MNLR} and CPM_{POLR}) are significantly overfitted at the three highest GOSE thresholds (i.e., GOSE > 5, GOSE > 6, and GOSE > 7). The graphical calibration of CPM_{DeepOR} was significantly worse than that of the other CPMs (**S3 Fig**). The calibration slopes and calibration curves for each APM

are displayed in **S3 Table** and **S4 Fig**, respectively. APM_{OR} is poorly calibrated at each threshold of GOSE. APM_{MN} is significantly overfitted at the three highest GOSE thresholds (i.e., GOSE > 5, GOSE > 6, and GOSE > 7).

The calibration slopes and calibration curves for the best-calibrated CPMs (CPM_{Best}), compared against those for the best-calibrated APMs (APM_{Best}), are displayed in **Table 4** and **Fig 3**, respectively. Unlike CPM_{Best}, APM_{Best} could not avoid significant overfitting at the three highest GOSE thresholds (i.e., GOSE > 5, GOSE > 6, and GOSE > 7). At these thresholds, we observe that the calibration curve of APM_{Best} significantly veered off the diagonal line of ideal calibration for higher predicted probabilities. However, due to the relative infrequency of these predictions (comparative histograms in **Fig 3**), the ICI of APM_{Best} is not significantly higher than that of CPM_{Best}. Our results suggest that APM_{Best} requires more patients with higher functional outcomes, in both the training and validation sets, to mitigate overfitting [45].

Fig 3. Ordinal calibration curves of best-performing concise-predictor-based model (CPM_{Best}) and best-performing all-predictor-based model (APM_{Best}). GOSE=Glasgow Outcome Scale – Extended at 6 months post-injury. In each panel, a comparative histogram (200 uniform bins), centred at a horizontal line in the bottom quarter, displays the distribution of predicted probabilities for CPM_{Best} (above the line) and APM_{Best} (below the line) at the given GOSE threshold. CPM_{Best} and APM_{Best} correspond to the CPM (**S2 Table**) and APM (**S3 Table**), respectively, with the lowest unweighted average of integrated calibration indices (ICI) across the thresholds. Shaded areas are 95% confidence intervals derived using bias-corrected bootstrapping (1,000 resamples) to represent the variation across repeated *k*-fold cross-validation folds (20 repeats of 5 folds) and, for CPM_{Best}, 100 missing value imputations. The values in each panel correspond to the mean ICI (95% confidence interval) at the given threshold. The diagonal dashed line represents the line of perfect calibration (ICI = 0).

Predictor importance

Given that APM_{MN} significantly outperforms APM_{OR} in discrimination and calibration, we focus the assessment of predictor importance to APM_{MN}. A bar plot of the mean absolute SHAP values associated with the 15 most important predictors in APM_{MN} is provided in **Fig 4**. We find that the subjective early prognoses of ICU physicians had the greatest contribution towards APM_{MN} predictions, particularly for the prediction of death (GOSE = 1) within 6 months. Initially, this result (along with the high contribution of other physician impressions) seems to suggest that integration of a physician's interpretations of a patient's baseline status may add important prognostic information. These impressions likely summarise information from a variable number of other predictors along with the physician's own experience-based judgement, resulting in high prediction contributions. However, inclusion of these variables may result in problematic self-fulfilling prophecies [51]. For instance, a physician's poor prognosis directly influences WLSM, which was instituted in 144 (70.2%) of the 205 patients who died in the ICU [52]. Including a variable for physician prognosis may then negatively bias the outcome prediction and unduly promote WLSM. Therefore, we do not consider physician impression predictors for our extended concise predictor set. We also observe that 'age at admission' was the only concise predictor among the 15 most important ones. The importance ranks (out of 1,151)

of the concise predictors (**Table 2**) are: age = 5th, glucose = 23rd, Marshall CT = 25th, pupillary reactivity = 29th, GCSm = 42nd, haemoglobin = 50th, hypoxia = 284th, tSAH = 301st, EDH = 414th, and hypotension = 420th. The eight remaining predictors of the top 15 (**Fig 4**) were added to the concise predictor set to form our extended concise predictor set. Within the tokens for "employment status before injury," we found that the single token indicating retirement is much more important than the others. Thus, instead of encoding all 10 options for employment status, we included a single indicator variable for retirement in our extended concise predictor set. The eight added predictors included 2 demographic variables (retirement status and highest level of formal education), 4 protein biomarker concentrations (neurofilament light chain [NFL], glial fibrillary acidic protein [GFAP], total tau protein [T-tau], and S100 calcium-binding protein B [S100B]), and 2 clinical assessment variables (worst abbreviated injury score [AIS] among head, neck, brain, and cervical spine injuries and incidence of post-traumatic amnesia at ICU admission). The extended concise predictor set, including the ten original concise predictors and the eight added predictors, is statistically characterised in **S1 Table**.

Fig 4. Mean absolute Shapley additive explanation (SHAP) values of most important predictors for multinomial-encoding all-predictor-based model (APM_{MN}). ICU=intensive care unit. ER=emergency room. CT=computerised tomography. GOS=Glasgow Outcome Scale (not extended). UO=unfavourable outcome, defined by functional dependence (i.e., GOSE ≤ 4). AIS=Abbreviated Injury Scale. GOSE=Glasgow Outcome Scale – Extended at 6 months post-injury. CPM=predictors that are included in the original concise predictor set. eCPM=predictors that are added to the original concise predictor set to form the extended concise predictor set. The mean absolute SHAP value is interpreted as the average magnitude of the relative additive contribution of a predictor's most important token towards the predicted probability at each GOSE score for a single patient. Predictor types are denoted by the coloured boundary around predictor names. Physician impression predictors denote predictors that encode the explicit impressions or rationales of ICU physicians and are not considered for the extended concise predictor set.

A bar plot of the mean absolute SHAP values of APM_{MN} for each of the five folds of the first repeat is provided in **S5 Fig**. Most of the eight added predictors, along with age at admission, are consistently represented among the most important predictors across the five folds.

eCPM discrimination and calibration

The discrimination and calibration metrics for the best-performing extended-predictor-based model ($eCPM_{Best}$) are listed in **Table 4**. Inclusion of the eight selected predictors accounted for about half of the gains in discrimination performance achieved by APM_{Best} over CPM_{Best} according to ORC, Somers' D_{xy}, and the dichotomous *c*-indices. Based on the difference in Somers' D_{xy}, the eight added predictors allowed models to explain an additional 6% of the ordinal variation in GOSE at 6 months post-injury. Unlike APM_{Best}, $eCPM_{Best}$ is not significantly overfitted at any threshold. The calibration curves of eCPMs (**S6 Fig**) are largely similar to those of the corresponding CPMs (**S3 Fig**), except at the highest threshold (i.e., GOSE > 7). Similar to those of APM_{MN}, the calibration curves of eCPMs veer off the line of ideal calibration at higher predicted probabilities of GOSE > 7. The eCPM results support the finding that discrimination performance can be improved

with the expansion of the predictor set. Furthermore, by limiting the number of added predictors and the analytical complexity of the model, eCPM avoided the significant miscalibration of APM at higher thresholds.

The discrimination and calibration metrics for each eCPM are listed in **S4 Table**.

Discussion

To our knowledge, this is the most comprehensive evaluation of early ordinal outcome prognosis for critically ill TBI patients. Our analysis cross-compares a range of ordinal prediction modelling strategies with a large range of available baseline predictors to determine the relative contribution of each towards model performance. Employing an AI tokenisation and embedding technique, we develop highly flexible ordinal prediction models that can learn from the entire, heterogeneous set of 1,151 predictors, available within the first 24 hours of ICU stay, in the CENTER-TBI dataset. This information includes not only all baseline clinical data currently deemed significant for ICU care of TBI but also advanced sub-study results (e.g., protein biomarkers, central haemostatic markers, genetic markers, and advanced MRI results) that represent the experimental frontier of clinical TBI assessment [1,15,16]. Therefore, our work reveals the interpretable limits of baseline ordinal, 6-month GOSE prediction in the ICU at this time.

Our key finding is that augmenting the baseline predictor set was much more relevant for improving ordinal model prediction performance than was increasing analytical complexity with deep learning. Within a given predictor set, artificial neural networks did not perform better than logistic regression models (**S2 Table**, **S4 Table**), nor did models with additional hidden layers for the APMs (**S4 Appendix**). This result is consistent with findings in the binary prediction case [53]. On the other hand, augmenting the predictor set, from CPM to APM, substantially improved ordinal discrimination (ORC: +8.6%, **Table 4**) and prediction at lower GOSE thresholds (e.g., GOSE > 1 *c*-index: +8.4%, **Table 4**). Just adding eight predictors to the concise predictor set accounted for about half of the gains in discrimination. However, the addition of predictors negatively affected model calibration, particularly at higher GOSE thresholds (**Fig 3**, **Table 4**). This result underlines the need for careful consideration of probability calibration during model development (e.g., recalibrate with isotonic regression to mitigate overfitting).

At the same time, our results also indicate that ordinal early outcome prognosis for critically ill TBI patients is limited in capability. The best-performing model, which learns from all baseline information in the CENTER-TBI dataset, can only correctly discriminate two randomly chosen patients with two randomly chosen GOSE scores 76% (95% CI: 74% – 77%) of the time. Equivalently, if the best performing model was tasked with ranking seven randomly chosen patients – each with a different true GOSE – by predicted GOSE, an average 5.10 (95% CI: 4.74–5.46) of the 21 possible pairwise orderings will be incorrect. Currently, ordinal model outputs explain, at best, 57% (95% CI: 54% – 60%) of the ordinal variation in 6-month GOSE. Ordinal prediction models struggle to reliably predict full recovery (GOSE > 7 *c*-index: 75% [95% CI: 72% – 79%], **Table 4**), and gains from expanding the predictor set diminish with higher GOSE thresholds.

It is important to acknowledge that the predictor importance results of this article should not be interpreted for predictor discovery or validation. SHAP values are visualised (**Fig 4**) solely to globally interpret APM_{MN} predictions and to form the extended concise predictor set. Risk factor validation, which falls out of the scope of this work, would require investigating the robustness and clinical plausibility of the relationship between predictor values and their corresponding SHAP values [54]. Moreover, causal analysis with apt consideration of confounding factors or dataset biases would be necessary before commenting on the potential effects or mechanisms of individual predictors.

We recognise several limitations in our study. While the concise predictor set was originally designed for prognosis after moderate-to-severe TBI [8] (i.e., baseline GCS 3 – 12), 26.6% of our study population had experienced mild (i.e., baseline GCS 13 – 15) TBI (**Table 1**). Predictor sets have been designed for mild TBI patients (e.g., UPFRONT study predictors [55]). However, in line with the aims of the CENTER-TBI project [15], we focus the TBI population not by initial characterisation with GCS but by stratum of care (i.e., admission to the ICU). Therefore, we selected the single concise predictor set that was best validated for the majority of critically ill TBI patients. Our outcome categories (GOSE at 6 months post-injury) were statistically imputed for 13% of our dataset using available GOSE between 2 weeks and one-year post-injury. Although this method was strongly validated on the same (CENTER-TBI) dataset [18], we do recognise that our outcome labels may not be precisely correct. The focus of this work is on the prediction of functional outcomes through GOSE; nonetheless, it is worth considering other outcomes, such as quality-of-life and psychological health, that are important for clinical decision making [56]. Finally, before the AI models developed in this work and in subsequent iterations could be integrated into ICU practice, limitations of generalisability must be addressed [57]. Our models were developed on a multicentre, adult population, prospectively recruited between 2014 and 2017 [25], across Europe, and may encode recruitment, collection, and clinical biases native to our patient set. AI models must continuously be updated, iteratively retrained on incoming information, to help fight the effect these biases may have on returned prognoses for a given patient.

In the setting of TBI prognosis, we encourage the use of AI not to add analytical complexity (i.e., make models “deeper”) but to expand the predictor set (i.e., make models “wider”). Studies have uncovered promising prognostic value in neuro-inflammatory markers [58,59] and high-resolution TBI monitoring and imaging modalities (e.g., intracranial and cerebral perfusion pressure [60-62], accelerometery [63], and MRI [64-66]), and we recommend integrating these features into ordinal prognostic models, especially to improve prediction of higher functional outcomes. We also believe that there is a feasible performance limit to reliable ordinal outcome prognosis if only statically considering the clinical information from the first 24 hours of ICU stay. It would seem far-fetched to expect all relevant information pertaining to an outcome at 6 months to be encapsulated in the first 24 hours of ICU treatment. Heterogeneous pathophysiological processes unfold over time in patients after TBI [67,68], and dynamic prediction models, which return model outputs longitudinally with changing clinical information, are better equipped to consider these temporal effects on prognosis. Dynamic prognosis models

have been developed for TBI patients [69] and the greater ICU population (not exclusive to TBI) [35,70,71], but none of them predict functional outcomes on an ordinal scale. We suggest that the next iteration of this work should be to develop ordinal dynamic prediction models on all clinical information available during the complete ICU stay.

Ethical approval statement

The CENTER-TBI study has been conducted in accordance with all relevant laws of the European Union and all relevant laws of the country where the recruiting sites were located, including (but not limited to) the relevant privacy and data protection laws and regulations, the relevant laws and regulations on the use of human materials, and all relevant guidance relating to clinical studies from time in force including (but not limited to) the ICH Harmonised Tripartite Guideline for Good Clinical Practice (CPMP/ICH/135/95) and the World Medical Association Declaration of Helsinki entitled "Ethical Principles for Medical Research Involving Human Subjects." Written informed consent by the patients and/or the legal representative/next of kin was obtained (according to local legislation) for all patients recruited in the core dataset of CENTER-TBI and documented in the electronic case report form. Ethical approval was obtained for each recruiting site.

The list of sites, ethical committees, approval numbers and approval dates can be found on the website: https://www.center-tbi.eu/project/ethical-approval.

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S.B. co-conceptualised the aims of the study, developed the methodology and design of the study, performed the data analysis and visualisation of results, and wrote the complete manuscript. I.M. aided S.B. in model design and data analysis and reviewed the manuscript. L.W., D.K.M., and R.D.S. reviewed the manuscript. E.W.S. advised S.B. on statistical analysis and reviewed the manuscript. D.W.N. aided S.B. and A.E. in the development of the study methodology and reviewed the manuscript. A.E. served as the principal investigator of this work, co-conceptualized the aims of the study, and reviewed the manuscript.

Competing interests

The authors declare that they have no conflicts of interest.

Code and data availability

All code used in this project can be found at the following online repository: https://github.com/sbhattacharyay/ordinal_GOSE_prediction (doi: 10.5281/zenodo.5933042). The minimal data required to reproduce the study's methods, reported statistics, figures, and results can be found among the commented and structured code of this repository.

Individual participant data, including data dictionary, the study protocol, and analysis scripts are available online, conditional to approved study proposal, with no end date. Interested investigators must provide a methodologically sound study proposal to the management committee. Proposals can be submitted online at https://www.center-tbi.eu/data. Signed confirmation of a data access agreement is required, and all access must comply with regulatory restrictions imposed on the original study.

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Supporting information

S1 Appendix. Explanation of selected ordinal prediction models for CPM and eCPM.

S2 Appendix. Explanation of APM for ordinal GOSE prediction.

S3 Appendix. Detailed explanation of ordinal model performance and calibration metrics.

S4 Appendix. Hyperparameter optimisation results.

S1 Fig. CONSORT-style flow diagram for patient enrolment and follow-up. CENTER-TBI=Collaborative European NeuroTrauma Effectiveness Research in TBI. ICU=intensive care unit. GOSE=Glasgow Outcome Scale – Extended. MSM=Markov multi-state model (see **Materials and methods**). The dashed, olive-green line in the lower-middle of the diagram divides the enrolment flow diagram (above) and the follow-up breakdown (below).

S2 Fig. Characterisation of missingness among concise predictor set. U.P.=unreactive pupils. GCSm=motor component score of the Glasgow Coma Scale. Hb=haemoglobin. Glu.=glucose. HoTN=hypotension. Marshall=Marshall computerised tomography classification. tSAH=traumatic subarachnoid haemorrhage. EDH=extradural haematoma. (**A**) Proportion of total sample size (*n* = 1,550) with missing values for each IMPACT extended model predictor. (**B**) Missingness matrix where each column represents a concise predictor, and each row represents a combination of missing predictors (red) and non-missing predictors (blue) found in the dataset. The prevalence of each combination (i.e., row) in the study population is shown with a horizontal histogram (far right) labelled with the proportion of the study population with the corresponding combination of missing predictors. For example, the bottom row of the matrix shows that 54.77% of the study population had no missing concise predictors while the penultimate row shows that 14.71% of the study population had only glucose and haemoglobin missing among the concise predictors.

S3 Fig. Ordinal calibration curves of each concise-predictor-based model (CPM). GOSE=Glasgow Outcome Scale – Extended at 6 months post-injury. Shaded areas are 95% confidence intervals derived using bias-corrected bootstrapping (1,000 resamples) to represent the variation across repeated *k*-fold cross-validation folds (20 repeats of 5 folds) and 100 missing value imputations. The values in each panel correspond to the mean integrated calibration index (ICI) (95% confidence interval) at the given threshold. The diagonal dashed line represents the line of perfect calibration (ICI = 0). The CPM types (CPM_{MNLR}, CPM_{POLR}, CPM_{DeepMN}, and CPM_{DeepOR}) are decoded in the **Materials and methods** and described in **S1 Appendix**.

S4 Fig. Ordinal calibration curves of each all-predictor-based model (APM). GOSE=Glasgow Outcome Scale – Extended at 6 months post-injury. Shaded areas are 95% confidence intervals derived using bias-corrected bootstrapping (1,000 resamples) to represent the variation across repeated *k*-fold cross-validation folds (20 repeats of 5 folds). The values in each panel correspond to the mean integrated calibration index (ICI) (95% confidence interval) at

the given threshold. The diagonal dashed line represents the line of perfect calibration (ICI = 0). The APM types (APM_{MN} and APM_{OR}) are decoded in the **Materials and methods** and described in **S2 Appendix**.

S5 Fig. Mean absolute SHAP values of the most important predictors for APM_{MN} in each of the five folds of the first repeat. ICU=intensive care unit. CT=computerised tomography. ER=emergency room. GOS=Glasgow Outcome Scale (not extended). AIS=Abbreviated Injury Scale. UO=unfavourable outcome, defined by functional dependence (i.e., GOSE ≤ 4). FIBTEM=fibrin-based extrinsically activated test with tissue factor and cytochalasin D. GOSE=Glasgow Outcome Scale – Extended at 6 months post-injury. The mean absolute SHAP value is interpreted as the average magnitude of the relative additive contribution of a predictor's most important token towards the predicted probability at each GOSE score for a single patient.

S6 Fig. Ordinal calibration curves of each extended concise-predictor-based model (eCPM). GOSE=Glasgow Outcome Scale – Extended at 6 months post-injury. Shaded areas are 95% confidence intervals derived using bias-corrected bootstrapping (1,000 resamples) to represent the variation across repeated *k*-fold cross-validation folds (20 repeats of 5 folds) and 100 missing value imputations. The values in each panel correspond to the mean integrated calibration index (ICI) (95% confidence interval) at the given threshold. The diagonal dashed line represents the line of perfect calibration (ICI = 0). The eCPM types ($eCPM_{MNLR}$, $eCPM_{POLR}$, $eCPM_{DeepMN}$, and $eCPM_{DeepOR}$) are decoded in the **Materials and methods** and described in **S1 Appendix**.

S1 Table. Extended concise baseline predictors of the study population stratified by ordinal 6-month outcomes.

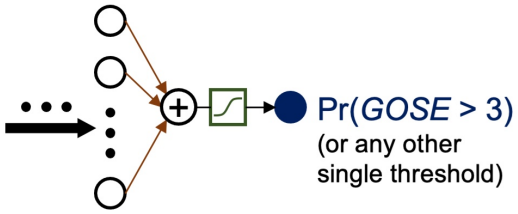
S2 Table. Ordinal concise-predictor-based model (CPM) discrimination and calibration performance.

S3 Table. Ordinal all-predictor-based model (APM) discrimination and calibration performance.

S4 Table. Ordinal extended concise-predictor-based model (eCPM) discrimination and calibration performance.

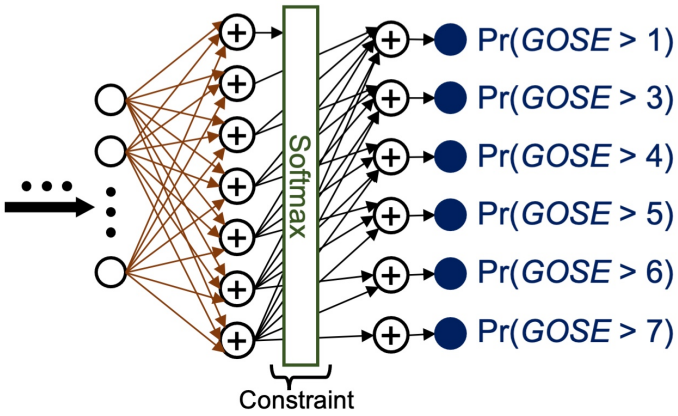
A

Binary prediction models

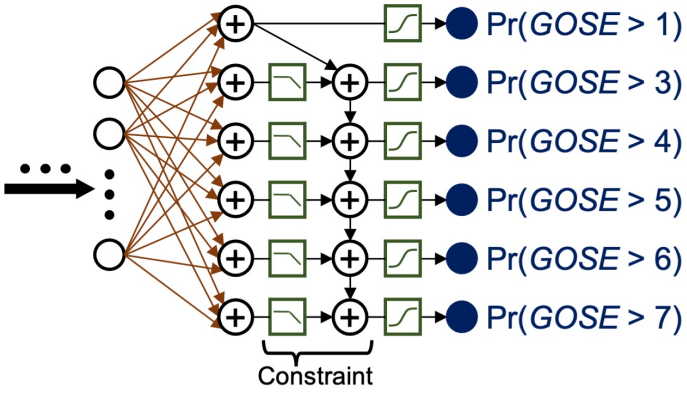


Ordinal prediction models

Multinomial outcome encoding



Ordinal outcome encoding



Legend

Activation functions

- Logistic sigmoid
- Negative ReLU
- Softmax $\left(\frac{e^{z_i}}{\sum_{j=1}^{7} e^{z_j}}\right)$

Architecture

- Learned weight (ω)
- Summation node
- Output node

B

Sample patient case

Presentation:

- Severe traumatic brain injury
- On life-sustaining therapy in the ICU
- Family would strongly prefer to withdraw from life-sustaining therapy if patient is not expected to regain conscious, partial functional independence (*GOSE* > 3) within 6 months

Baseline prognosis with binary prediction model

Model output:

Pr(*GOSE* > 3) = 0.1228617

Interpretation:

"The patient has an 12.3% chance of recovering conscious, partial functional independence within 6 months."

Baseline prognosis with ordinal prediction model

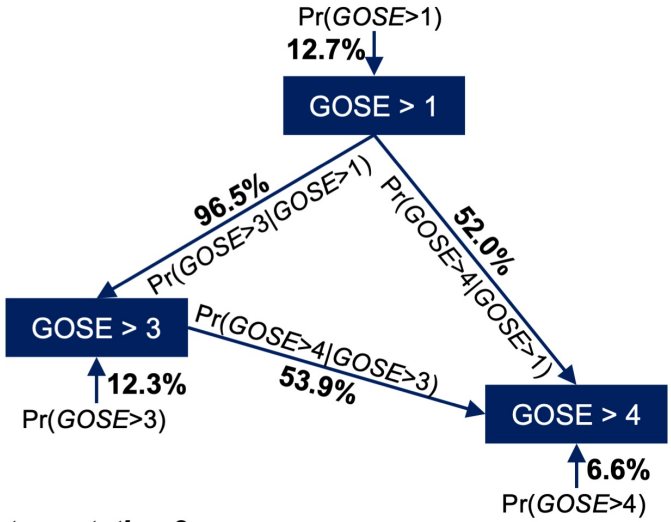
Model output:

Pr(*GOSE* > 1) = 0.1273615
Pr(*GOSE* > 3) = 0.1228617
Pr(*GOSE* > 4) = 0.0661974
Pr(*GOSE* > 5) = 0.0261596
Pr(*GOSE* > 6) = 0.0216245
Pr(*GOSE* > 7) = 0.0038411

Interpretation 1:

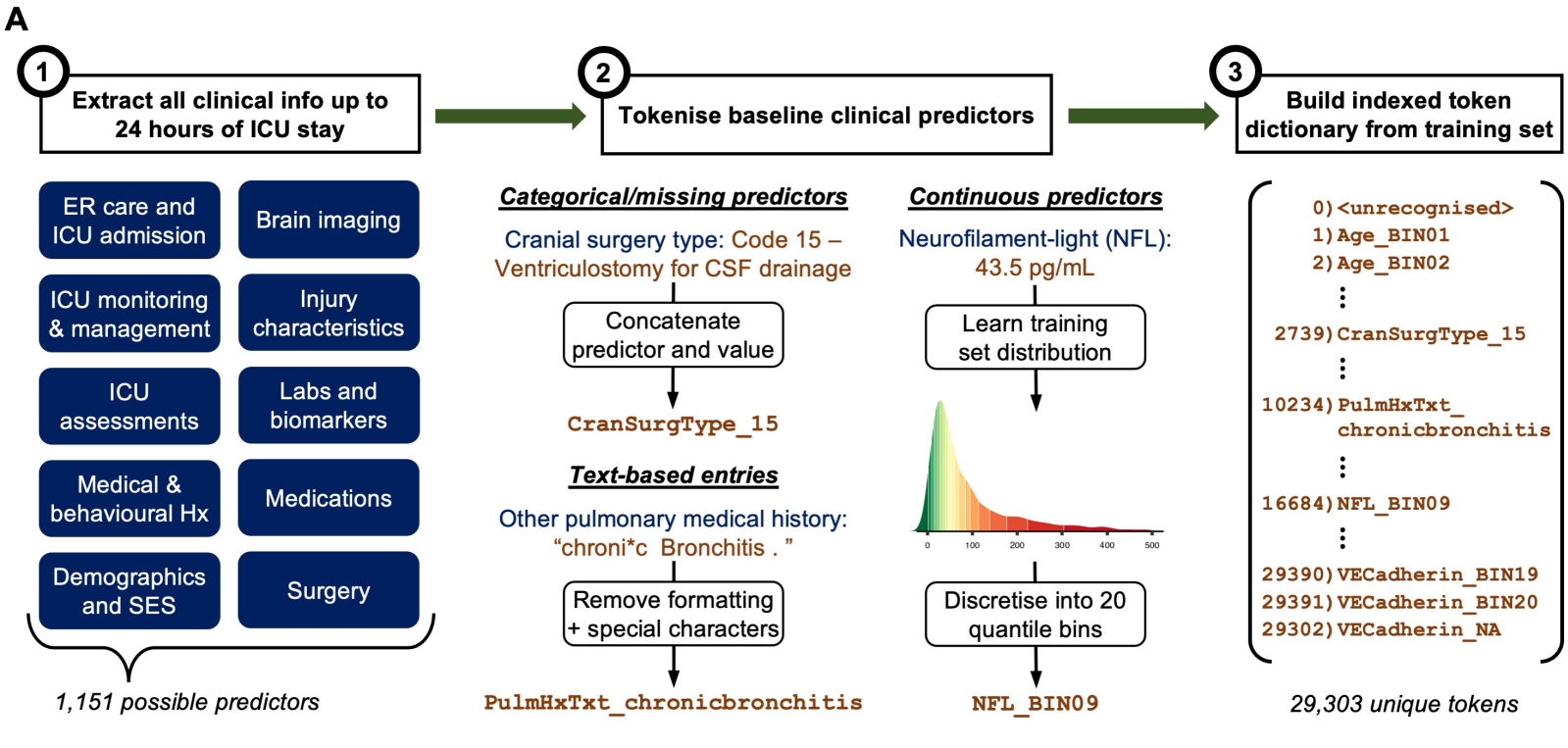
"The patient has a 12.7% chance of survival up to 6 months and a 12.3% chance of recovering conscious, partial functional independence within 6 months."

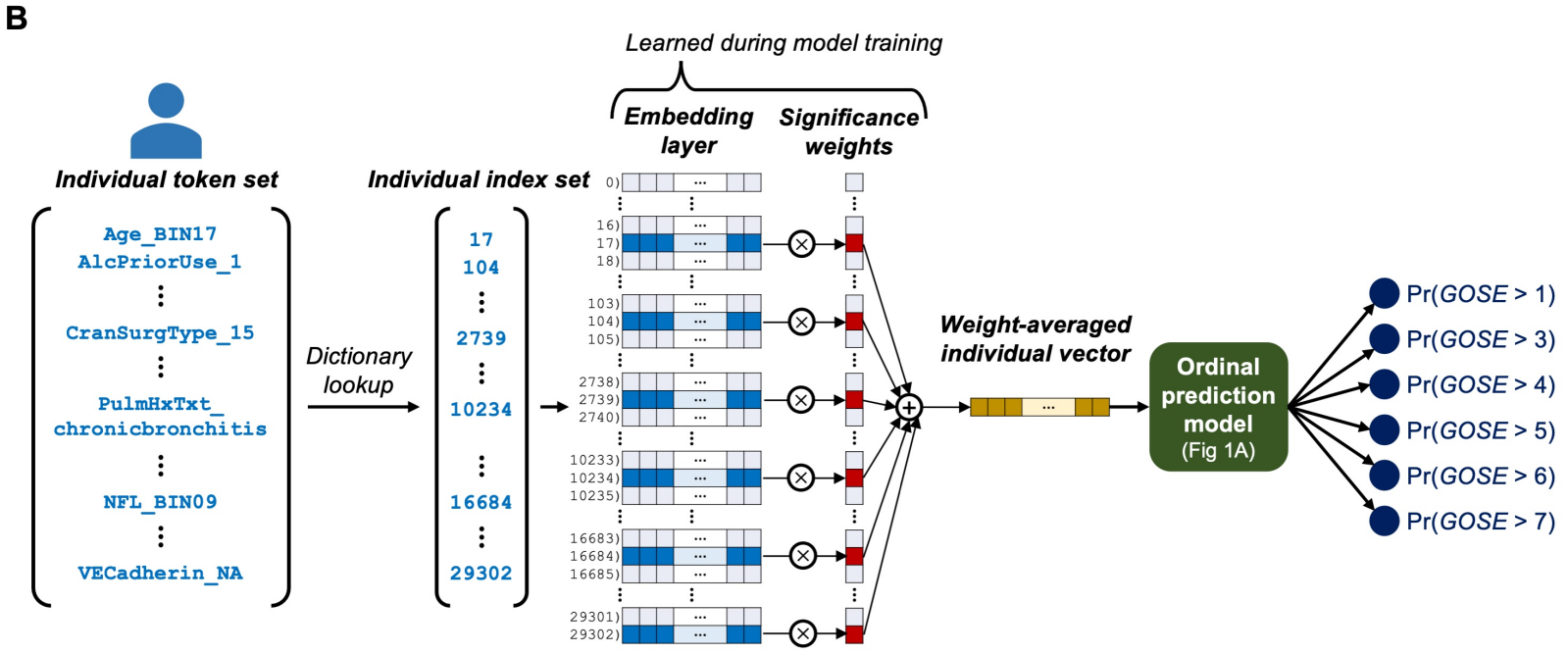
Bespoke conditional probability diagram:

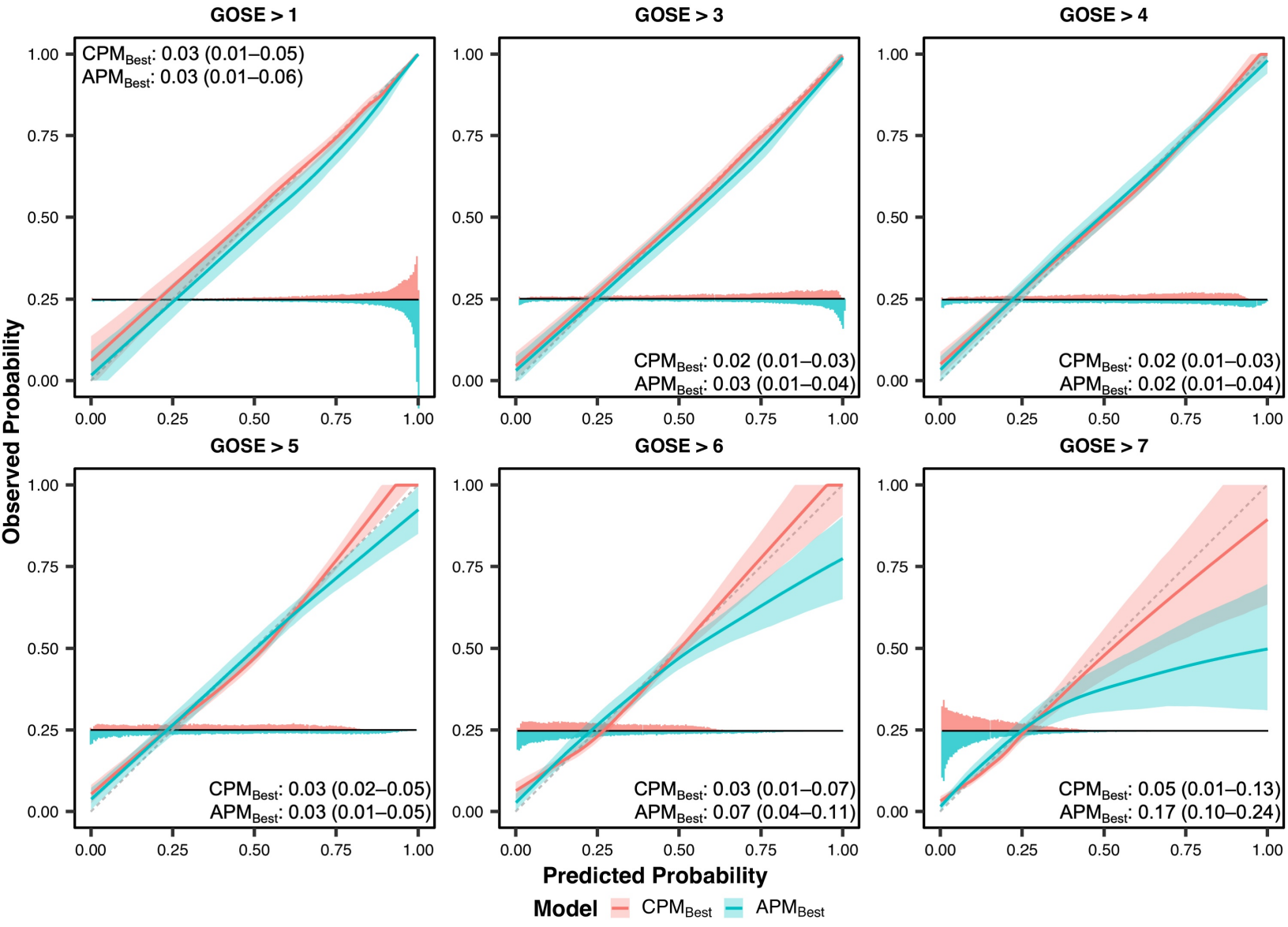


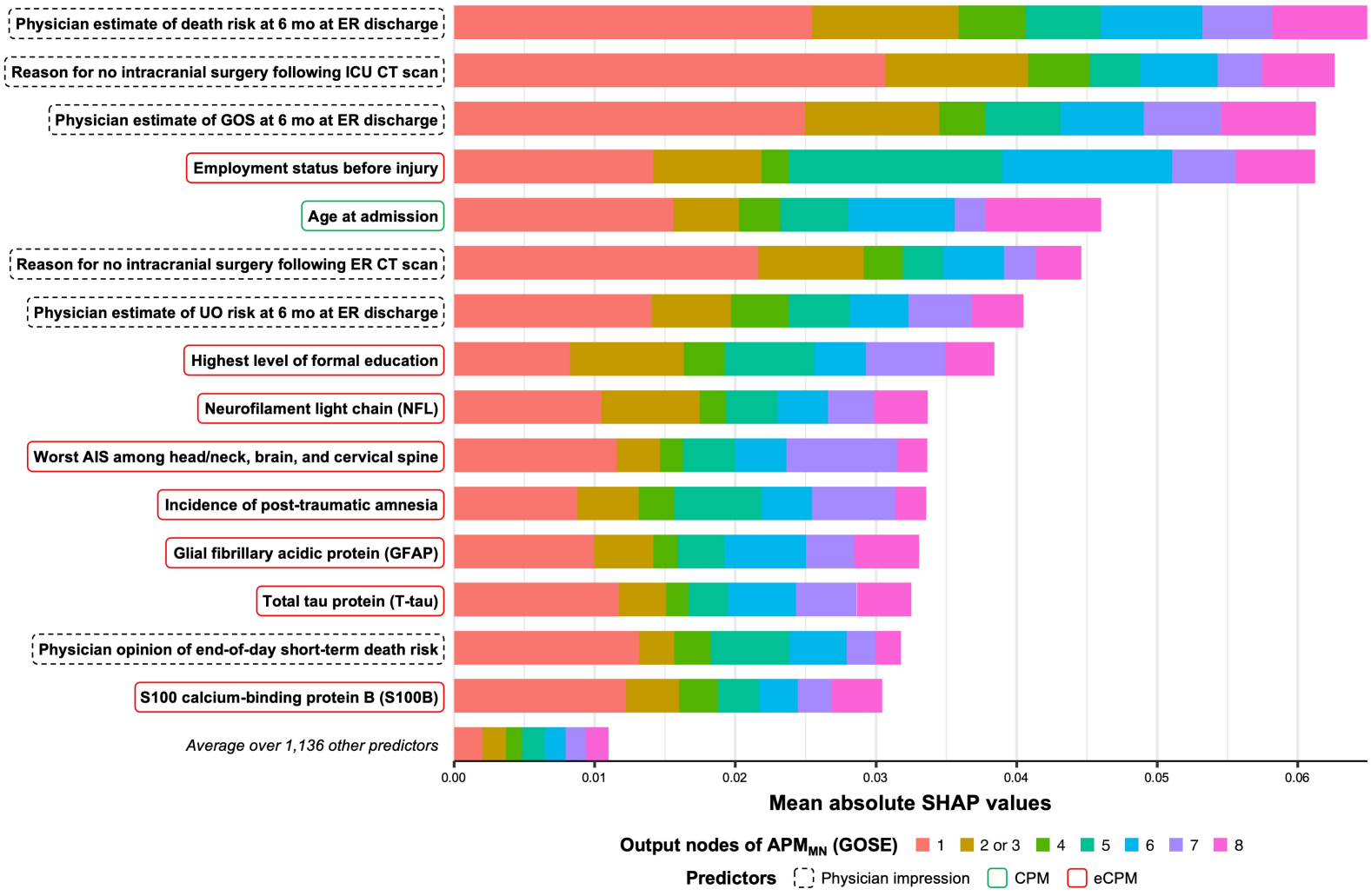
Interpretation 2:

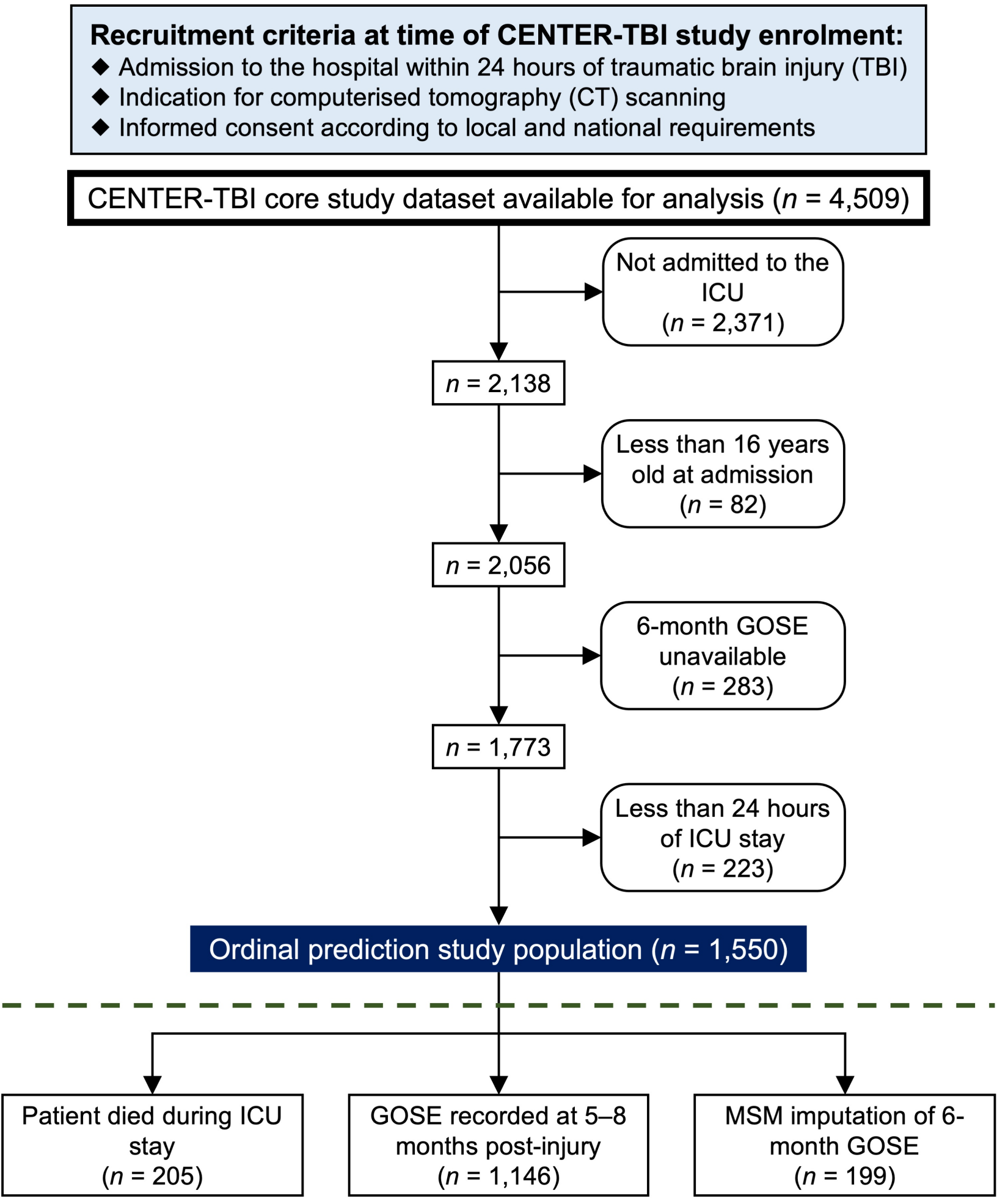
"If the patient does survive up to 6 months, they have a 96.5% chance of recovering conscious, partial functional independence and a 52.0% chance of regaining full functional independence."

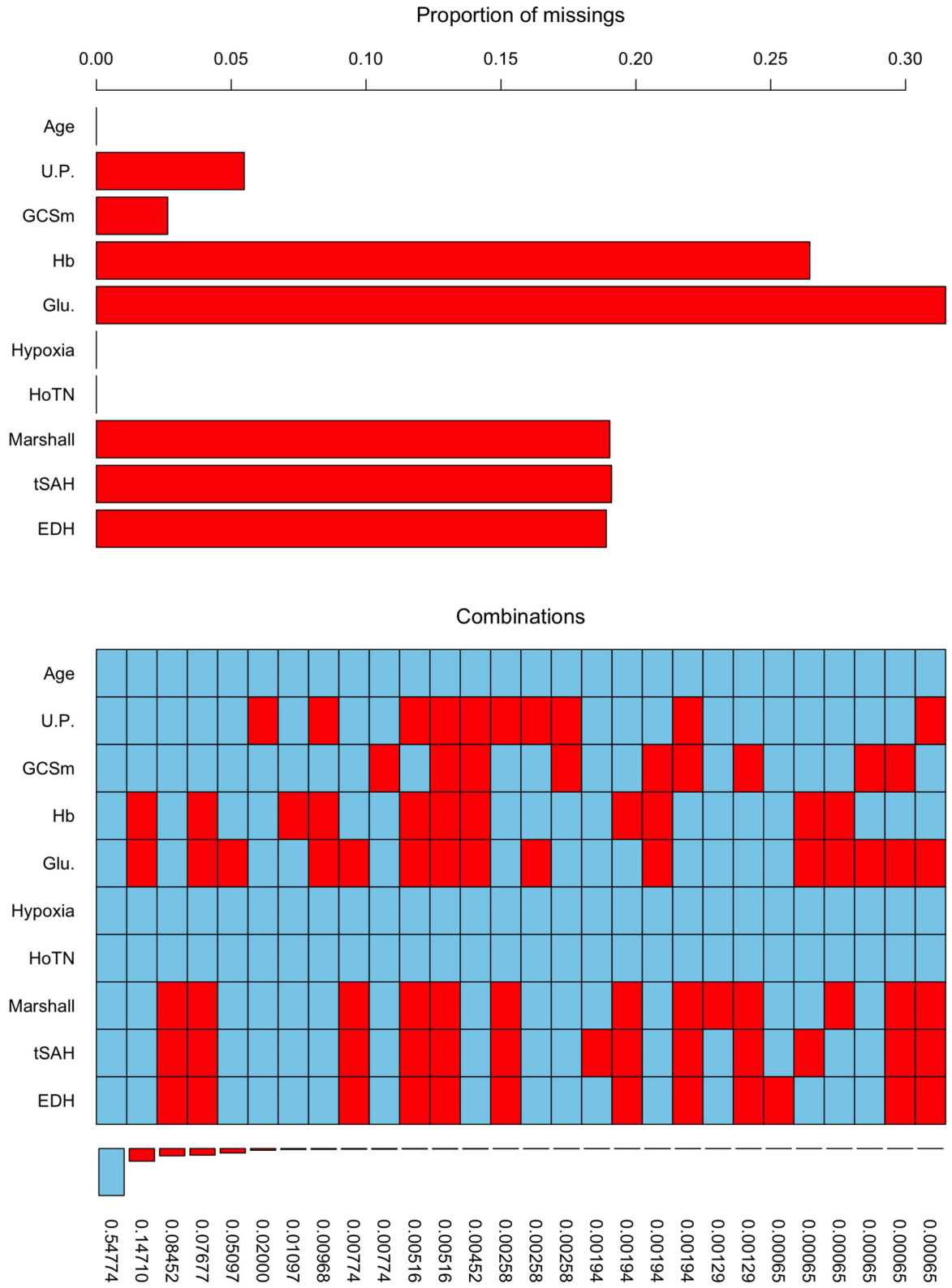

A
1
Extract all clinical info up to 24 hours of ICU stay
ER care and ICU admission
Brain imaging
ICU monitoring & management
Injury characteristics
ICU assessments
Labs and biomarkers
Medical & behavioural Hx
Medications
Demographics and SES
Surgery
1,151 possible predictors
2
Tokenise baseline clinical predictors
Categorical/missing predictors
Cranial surgery type: Code 15 – Ventriculostomy for CSF drainage
Concatenate predictor and value
CranSurgType_15
Text-based entries
Other pulmonary medical history: "chroni*c Bronchitis . "
Remove formatting + special characters
PulmHxTxt_chronicbronchitis
Continuous predictors
Neurofilament-light (NFL): 43.5 pg/mL
Learn training set distribution
0
100
200
300
400
500
Discretise into 20 quantile bins
NFL_BIN09
3
Build indexed token dictionary from training set
0) <unrecognised>
1) Age_BIN01
2) Age_BIN02
2739) CranSurgType_15
10234) PulmHxTxt_chronicbronchitis
16684) NFL_BIN09
29390) VECadherin_BIN19
29391) VECadherin_BIN20
29302) VECadherin_NA
29,303 unique tokens

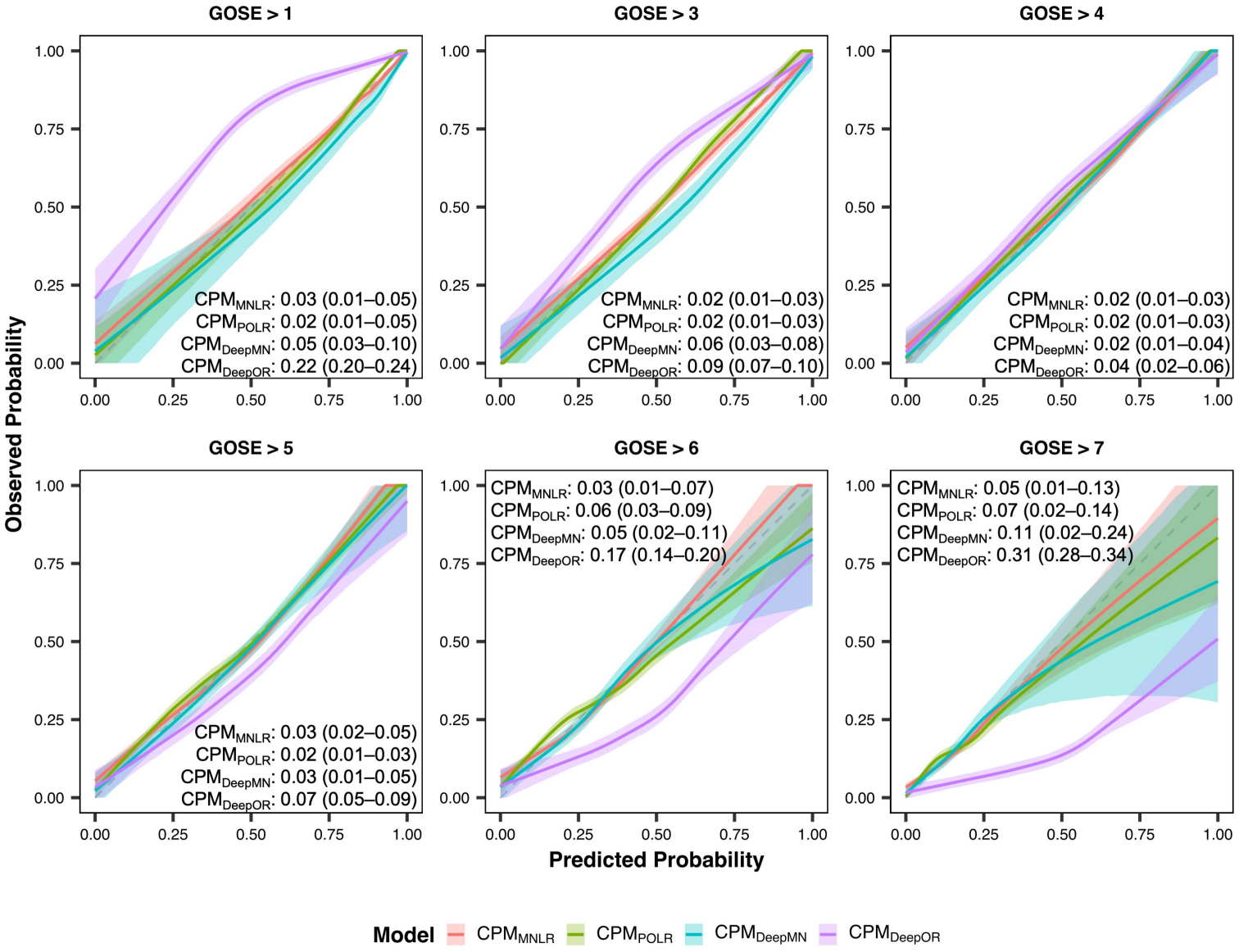

B
Learned during model training
Embedding layer
Significance weights
Individual token set
Age_BIN17
AlcPriorUse_1
CranSurgType_15
PulmHxTxt_chronicbronchitis
NFL_BIN09
VECadherin_NA
Dictionary lookup
Individual index set
17
104
2739
10234
16684
29302
Weight-averaged individual vector
Ordinal prediction model (Fig 1A)
Pr(GOSE > 1)
Pr(GOSE > 3)
Pr(GOSE > 4)
Pr(GOSE > 5)
Pr(GOSE > 6)
Pr(GOSE > 7)

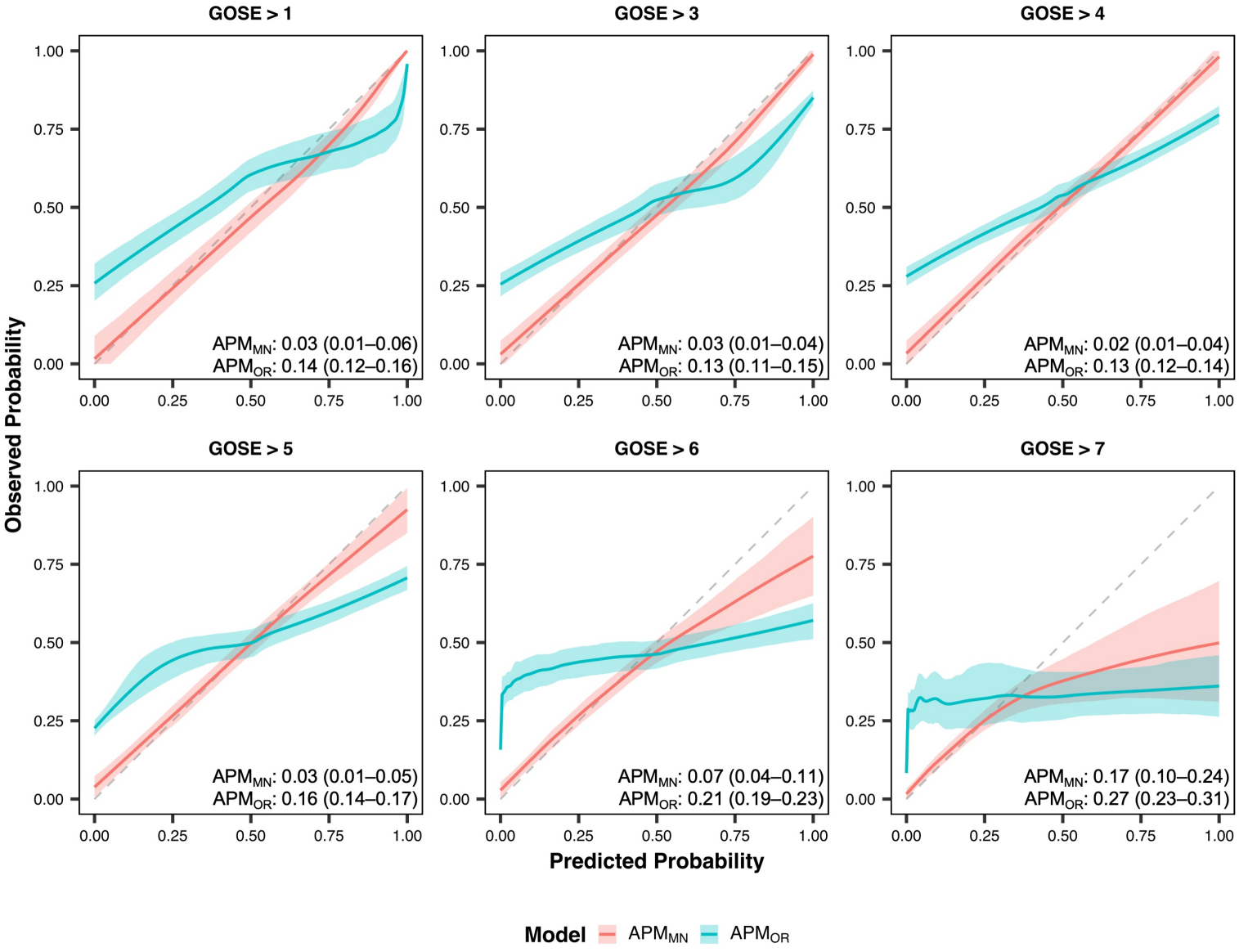

GOSE > 1
CPMBest: 0.03 (0.01–0.05)
APMBest: 0.03 (0.01–0.06)
GOSE > 3
CPMBest: 0.02 (0.01–0.03)
APMBest: 0.03 (0.01–0.04)
GOSE > 4
CPMBest: 0.02 (0.01–0.03)
APMBest: 0.02 (0.01–0.04)
GOSE > 5
CPMBest: 0.03 (0.02–0.05)
APMBest: 0.03 (0.01–0.05)
GOSE > 6
CPMBest: 0.03 (0.01–0.07)
APMBest: 0.07 (0.04–0.11)
GOSE > 7
CPMBest: 0.05 (0.01–0.13)
APMBest: 0.17 (0.10–0.24)
Observed Probability
Predicted Probability
0.00
0.25
0.50
0.75
1.00
Model
CPMBest
APMBest

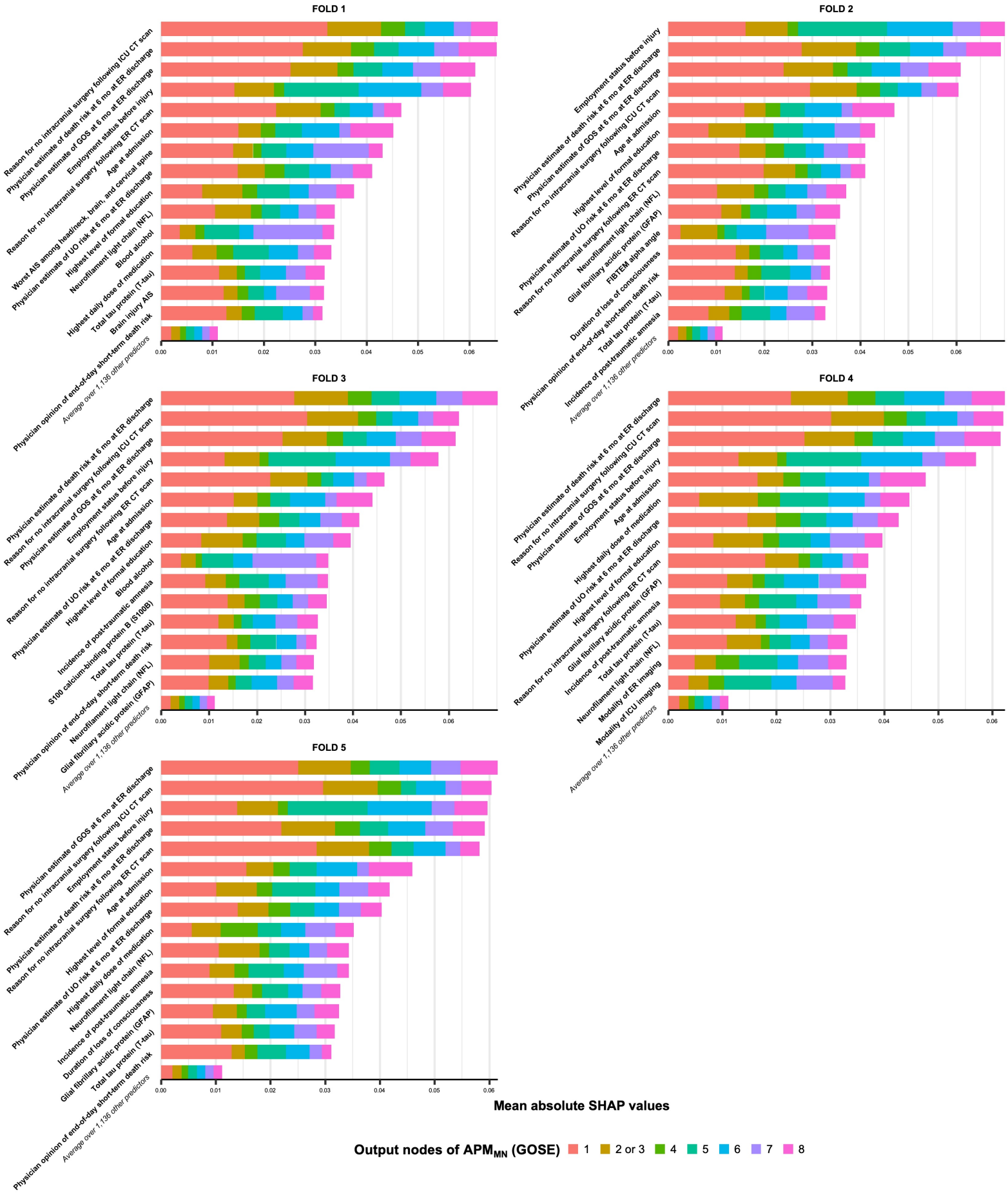

Physician estimate of death risk at 6 mo at ER discharge
Reason for no intracranial surgery following ICU CT scan
Physician estimate of GOS at 6 mo at ER discharge
Employment status before injury
Age at admission
Reason for no intracranial surgery following ER CT scan
Physician estimate of UO risk at 6 mo at ER discharge
Highest level of formal education
Neurofilament light chain (NFL)
Worst AIS among head/neck, brain, and cervical spine
Incidence of post-traumatic amnesia
Glial fibrillary acidic protein (GFAP)
Total tau protein (T-tau)
Physician opinion of end-of-day short-term death risk
S100 calcium-binding protein B (S100B)
Average over 1,136 other predictors
0.00
0.01
0.02
0.03
0.04
0.05
0.06
Mean absolute SHAP values
Output nodes of APM$_{MN}$ (GOSE) 1 2 or 3 4 5 6 7 8
Predictors Physician impression CPM eCPM

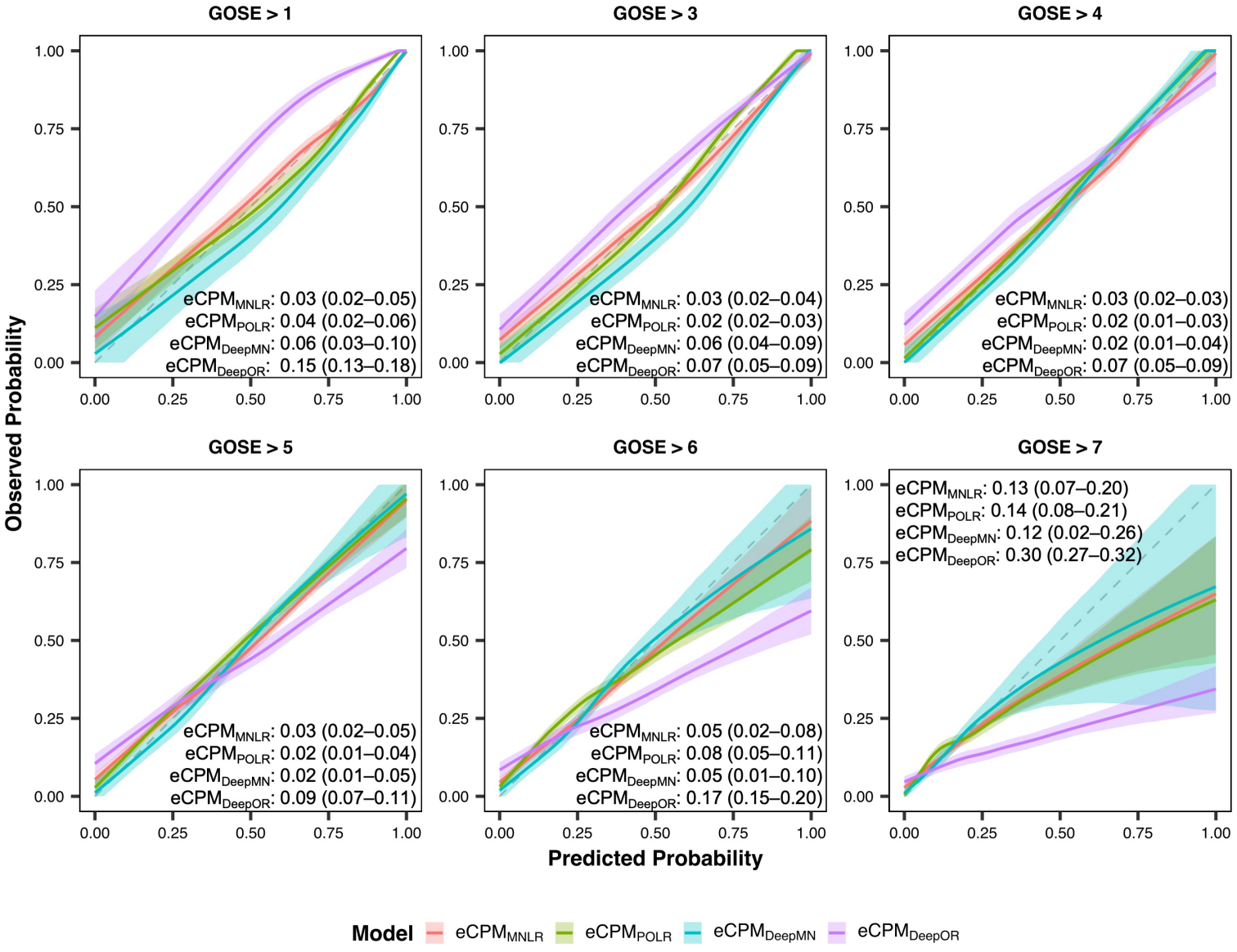

Recruitment criteria at time of CENTER-TBI study enrolment:
◆ Admission to the hospital within 24 hours of traumatic brain injury (TBI)
◆ Indication for computerised tomography (CT) scanning
◆ Informed consent according to local and national requirements
CENTER-TBI core study dataset available for analysis (n = 4,509)
Not admitted to the ICU (n = 2,371)
n = 2,138
Less than 16 years old at admission (n = 82)
n = 2,056
6-month GOSE unavailable (n = 283)
n = 1,773
Less than 24 hours of ICU stay (n = 223)
Ordinal prediction study population (n = 1,550)
Patient died during ICU stay (n = 205)
GOSE recorded at 5–8 months post-injury (n = 1,146)
MSM imputation of 6-month GOSE (n = 199)


Proportion of missings
0.00
0.05
0.10
0.15
0.20
0.25
0.30
Age
U.P.
GCSm
Hb
Glu.
Hypoxia
HoTN
Marshall
tSAH
EDH
Combinations
Age
U.P.
GCSm
Hb
Glu.
Hypoxia
HoTN
Marshall
tSAH
EDH
0.54774
0.14710
0.08452
0.07677
0.05097
0.02000
0.01097
0.00968
0.00774
0.00774
0.00516
0.00516
0.00452
0.00258
0.00258
0.00258
0.00194
0.00194
0.00194
0.00194
0.00129
0.00129
0.00065
0.00065
0.00065
0.00065
0.00065
0.00065


GOSE > 1
CPM_MNLR: 0.03 (0.01–0.05)
CPM_POLR: 0.02 (0.01–0.05)
CPM_DeepMN: 0.05 (0.03–0.10)
CPM_DeepOR: 0.22 (0.20–0.24)
GOSE > 3
CPM_MNLR: 0.02 (0.01–0.03)
CPM_POLR: 0.02 (0.01–0.03)
CPM_DeepMN: 0.06 (0.03–0.08)
CPM_DeepOR: 0.09 (0.07–0.10)
GOSE > 4
CPM_MNLR: 0.02 (0.01–0.03)
CPM_POLR: 0.02 (0.01–0.03)
CPM_DeepMN: 0.02 (0.01–0.04)
CPM_DeepOR: 0.04 (0.02–0.06)
GOSE > 5
CPM_MNLR: 0.03 (0.02–0.05)
CPM_POLR: 0.02 (0.01–0.03)
CPM_DeepMN: 0.03 (0.01–0.05)
CPM_DeepOR: 0.07 (0.05–0.09)
GOSE > 6
CPM_MNLR: 0.03 (0.01–0.07)
CPM_POLR: 0.06 (0.03–0.09)
CPM_DeepMN: 0.05 (0.02–0.11)
CPM_DeepOR: 0.17 (0.14–0.20)
GOSE > 7
CPM_MNLR: 0.05 (0.01–0.13)
CPM_POLR: 0.07 (0.02–0.14)
CPM_DeepMN: 0.11 (0.02–0.24)
CPM_DeepOR: 0.31 (0.28–0.34)
Observed Probability
Predicted Probability
0.00
0.25
0.50
0.75
1.00
Model
CPM_MNLR
CPM_POLR
CPM_DeepMN
CPM_DeepOR


GOSE > 1
APM_MN: 0.03 (0.01–0.06)
APM_OR: 0.14 (0.12–0.16)
GOSE > 3
APM_MN: 0.03 (0.01–0.04)
APM_OR: 0.13 (0.11–0.15)
GOSE > 4
APM_MN: 0.02 (0.01–0.04)
APM_OR: 0.13 (0.12–0.14)
GOSE > 5
APM_MN: 0.03 (0.01–0.05)
APM_OR: 0.16 (0.14–0.17)
GOSE > 6
APM_MN: 0.07 (0.04–0.11)
APM_OR: 0.21 (0.19–0.23)
GOSE > 7
APM_MN: 0.17 (0.10–0.24)
APM_OR: 0.27 (0.23–0.31)
Observed Probability
Predicted Probability
0.00
0.25
0.50
0.75
1.00
Model
APM_MN
APM_OR


FOLD 1
Reason for no intracranial surgery following ICU CT scan
Physician estimate of death risk at 6 mo at ER discharge
Physician estimate of GOS at 6 mo at ER discharge
Employment status before injury
Reason for no intracranial surgery following ER CT scan
Age at admission
Worst AIS among head/neck, brain, and cervical spine
Physician estimate of UO risk at 6 mo at ER discharge
Highest level of formal education
Neurofilament light chain (NFL)
Blood alcohol
Highest daily dose of medication
Total tau protein (T-tau)
Brain injury AIS
Physician opinion of end-of-day short-term death risk
Average over 1,136 other predictors
0.00
0.01
0.02
0.03
0.04
0.05
0.06
FOLD 2
Employment status before injury
Physician estimate of death risk at 6 mo at ER discharge
Physician estimate of GOS at 6 mo at ER discharge
Reason for no intracranial surgery following ICU CT scan
Age at admission
Highest level of formal education
Physician estimate of UO risk at 6 mo at ER discharge
Reason for no intracranial surgery following ER CT scan
Neurofilament light chain (NFL)
Glial fibrillary acidic protein (GFAP)
FIBTEM alpha angle
Duration of loss of consciousness
Total tau protein (T-tau)
Physician opinion of end-of-day short-term death risk
Incidence of post-traumatic amnesia
Average over 1,136 other predictors
0.00
0.01
0.02
0.03
0.04
0.05
0.06
FOLD 3
Physician estimate of death risk at 6 mo at ER discharge
Reason for no intracranial surgery following ICU CT scan
Physician estimate of GOS at 6 mo at ER discharge
Employment status before injury
Reason for no intracranial surgery following ER CT scan
Age at admission
Physician estimate of UO risk at 6 mo at ER discharge
Highest level of formal education
Blood alcohol
Incidence of post-traumatic amnesia
S100 calcium-binding protein B (S100B)
Total tau protein (T-tau)
Physician opinion of end-of-day short-term death risk
Neurofilament light chain (NFL)
Glial fibrillary acidic protein (GFAP)
Average over 1,136 other predictors
0.00
0.01
0.02
0.03
0.04
0.05
0.06
FOLD 4
Physician estimate of death risk at 6 mo at ER discharge
Reason for no intracranial surgery following ICU CT scan
Physician estimate of GOS at 6 mo at ER discharge
Employment status before injury
Age at admission
Highest daily dose of medication
Physician estimate of UO risk at 6 mo at ER discharge
Highest level of formal education
Reason for no intracranial surgery following ER CT scan
Glial fibrillary acidic protein (GFAP)
Incidence of post-traumatic amnesia
Total tau protein (T-tau)
Neurofilament light chain (NFL)
Modality of ER imaging
Modality of ICU imaging
Average over 1,136 other predictors
0.00
0.01
0.02
0.03
0.04
0.05
0.06
FOLD 5
Physician estimate of GOS at 6 mo at ER discharge
Reason for no intracranial surgery following ICU CT scan
Employment status before injury
Physician estimate of death risk at 6 mo at ER discharge
Reason for no intracranial surgery following ER CT scan
Age at admission
Highest level of formal education
Physician estimate of UO risk at 6 mo at ER discharge
Highest daily dose of medication
Neurofilament light chain (NFL)
Incidence of post-traumatic amnesia
Duration of loss of consciousness
Glial fibrillary acidic protein (GFAP)
Total tau protein (T-tau)
Physician opinion of end-of-day short-term death risk
Average over 1,136 other predictors
0.00
0.01
0.02
0.03
0.04
0.05
0.06
Mean absolute SHAP values
Output nodes of APM$_{MN}$ (GOSE)
1
2 or 3
4
5
6
7
8


GOSE > 1
eCPM$_{MNLR}$: 0.03 (0.02–0.05)
eCPM$_{POLR}$: 0.04 (0.02–0.06)
eCPM$_{DeepMN}$: 0.06 (0.03–0.10)
eCPM$_{DeepOR}$: 0.15 (0.13–0.18)
GOSE > 3
eCPM$_{MNLR}$: 0.03 (0.02–0.04)
eCPM$_{POLR}$: 0.02 (0.02–0.03)
eCPM$_{DeepMN}$: 0.06 (0.04–0.09)
eCPM$_{DeepOR}$: 0.07 (0.05–0.09)
GOSE > 4
eCPM$_{MNLR}$: 0.03 (0.02–0.03)
eCPM$_{POLR}$: 0.02 (0.01–0.03)
eCPM$_{DeepMN}$: 0.02 (0.01–0.04)
eCPM$_{DeepOR}$: 0.07 (0.05–0.09)
GOSE > 5
eCPM$_{MNLR}$: 0.03 (0.02–0.05)
eCPM$_{POLR}$: 0.02 (0.01–0.04)
eCPM$_{DeepMN}$: 0.02 (0.01–0.05)
eCPM$_{DeepOR}$: 0.09 (0.07–0.11)
GOSE > 6
eCPM$_{MNLR}$: 0.05 (0.02–0.08)
eCPM$_{POLR}$: 0.08 (0.05–0.11)
eCPM$_{DeepMN}$: 0.05 (0.01–0.10)
eCPM$_{DeepOR}$: 0.17 (0.15–0.20)
GOSE > 7
eCPM$_{MNLR}$: 0.13 (0.07–0.20)
eCPM$_{POLR}$: 0.14 (0.08–0.21)
eCPM$_{DeepMN}$: 0.12 (0.02–0.26)
eCPM$_{DeepOR}$: 0.30 (0.27–0.32)
Observed Probability
Predicted Probability
0.00
0.25
0.50
0.75
1.00
Model
eCPM$_{MNLR}$
eCPM$_{POLR}$
eCPM$_{DeepMN}$
eCPM$_{DeepOR}$

S1 Appendix: Explanation of selected ordinal prediction models for CPM and eCPM

Multinomial logistic regression (MNLR)

CPM_{MNLR} and $eCPM_{MNLR}$ were implemented using the 'MNLogit' class from the 'statsmodels' module (dev. v0.14.0) [1] in Python (v3.7.6). The GOSE score of 1 (death) was designated as the reference label, and, for each other GOSE score, a separate logistic model was trained to regress the logit of the ratio of the probability of that score to the reference score from a linear combination of the predictors. The logit outputs of each model feed into a softmax function, after which cumulative sums would determine the probability at each threshold. Model weights for MNLR were optimised using the Broyden–Fletcher–Goldfarb–Shanno (BFGS) algorithm [2] to maximize conditional likelihood.

Proportional odds (i.e., ordinal) logistic regression (POLR)

CPM_{POLR} and $eCPM_{POLR}$ were implemented using the 'OrderedModel' class from the 'statsmodels' module in Python. The model maps GOSE scores to a latent, logit space where consecutive GOSE scores are separated by thresholds. Thus, the model trains only one set of linear predictor weights, but a separate intercept for each threshold. Model weights for POLR were optimised using the Broyden–Fletcher–Goldfarb–Shanno (BFGS) algorithm [2] to maximize conditional likelihood.

Class-weighted feedforward neural network with a multinomial output layer (DeepMN)

CPM_{DeepMN} and $eCPM_{DeepMN}$ were implemented using the 'PyTorch' (v1.10.0) [3] module in Python. The network architecture of DeepMN included a hyperparametric number of dense hidden layers (either 1, 2, 3, 4, 5, or 6), each containing a hyperparametric number of nodes (either 128, 256, or 512) with a rectified linear unit (ReLU) activation function and a hyperparametric percentage (either 0% or 20%) dropout during training. The output layer of DeepMN was a softmax layer of 7 nodes, from which probabilities at each GOSE are calculated with cumulative sums (**Fig 1A**). DeepMN was optimised using the Adam algorithm (γ [learning rate] = 0.001, β_1 = 0.9, β_2 = 0.999) [4] with categorical cross-entropy loss. In the loss function, classes were weighted inversely proportional to the frequency of each GOSE score in the training set to counter class imbalance.

Class-weighted feedforward neural network with an ordinal output layer (DeepOR)

CPM_{DeepOR} and $eCPM_{DeepOR}$ were implemented using the 'PyTorch' (v1.10.0) [3] module in Python. The network architecture of DeepMN included a hyperparametric number of

dense hidden layers (either 1, 2, 3, 4, 5, or 6), each containing a hyperparametric number of nodes (either 128, 256, or 512) with a rectified linear unit (ReLU) activation function and a hyperparametric percentage (either 0% or 20%) dropout during training. The output layer of DeepOR was a sigmoid layer of 6 nodes, where each node represented the binomial probability of the outcome being greater than a certain threshold, and each node is constrained to be less than or equal to lower-threshold nodes with a negative ReLU transformation (**Fig 1A**). DeepOR was optimised using the Adam algorithm (γ [learning rate] = 0.001, β_1 = 0.9, β_2 = 0.999) with binary cross-entropy loss. In the loss function, classes were weighted inversely proportional to the frequency of each GOSE score in the training set to counter class imbalance.

CPM or eCPM	Description	Hyperparameters			Total number of configurations
		Hidden layers	Neurons per layer*	Dropout	
MNLR	Multinomial logistic regression				1
POLR	Proportional odds (i.e., ordinal) logistic regression				1
DeepMN	Class-weighted feedforward neural network with a multinomial (i.e., softmax) output layer	1, 2, 3, 4, 5, or 6	128, 256, or 512	0% or 20%	2184
DeepOR	Class-weighted feedforward neural network with an ordinal (i.e., sigmoid at each threshold) output layer	1, 2, 3, 4, 5, or 6	128, 256, or 512	0% or 20%	2184

*Different hidden layers may have distinct numbers of neurons.

References

1. Seabold S, Perktold J. Statsmodels: Econometric and Statistical Modeling with Python. In: van der Walt S, Millman J, editors. Proceedings of the 9th Python in Science Conference (SciPy 2010). Austin: SciPy; 2010. pp. 92-96. doi: 10.25080/Majora-92bf1922-011
2. Fletcher R. Practical Methods of Optimization. 2nd ed. New York: John Wiley & Sons; 1987.
3. Paszke A, Gross S, Massa F, Lerer A, Bradbury J, Chanan G, et al. PyTorch: An Imperative Style, High-Performance Deep Learning Library. In: Wallach H, Larochelle H, Beygelzimer A, d'Alché-Buc F, Fox E, Garnett R, editors. Advances in Neural Information Processing Systems 32 (NeurIPS 2019). Vancouver: NeurIPS; 2019.
4. Kingma DP, Ba J. Adam: A Method for Stochastic Optimization. arXiv:1412.6980v9 [Preprint]. 2017 [cited 2021 December 26]. Available from: https://arxiv.org/abs/1412.6980

S2 Appendix: Explanation of APM for ordinal GOSE prediction

APM_{MN} and APM_{OR} were implemented using the 'PyTorch' (v1.10.0) [1] module in Python. Regarding hyperparameters, the embedding and weight-averaging layer (**Fig 2B**) is considered to the be the first hidden layer. Thus, the number of neurons for the first hidden layer can also be considered as the embedding dimension (i.e., the length of each of the embedding vectors trained on the token dictionary). The individual vector returned by the embedding and weight-averaging layer (**Fig 2B**) then undergoes a hyperparametric number of dense hidden layers (either 0, 1, 2, 3, 4, or 5), each containing a hyperparametric number of nodes (either 128, 256, or 512) with a rectified linear unit (ReLU) activation function and a hyperparametric percentage (either 0% or 20%) dropout during training. The output layer of APM_{MN} was a softmax layer of 7 nodes, from which probabilities at each GOSE are calculated with cumulative sums (**Fig 1A**). APM_{MN} was optimised using the Adam algorithm (γ [learning rate] = 0.001, β_1 = 0.9, β_2 = 0.999) [2] with categorical cross-entropy loss. In the loss function, classes were weighted inversely proportional to the frequency of each GOSE score in the training set to counter class imbalance. The output layer of APM_{OR} was a sigmoid layer of 6 nodes, where each node represented the binomial probability of the outcome being greater than a certain threshold, and each node is constrained to be less than or equal to lower-threshold nodes with a negative ReLU transformation (**Fig 1A**). APM_{OR} was optimised using the Adam algorithm (γ [learning rate] = 0.001, β_1 = 0.9, β_2 = 0.999) with binary cross-entropy loss. In the loss function, classes were weighted inversely proportional to the frequency of each GOSE score in the training set to counter class imbalance.

APM	Description	Hyperparameters			Total number of configurations
		Hidden layers*	Neurons per layer†	Dropout	
APM_{MN}	Class-weighted embedding and weight-averaging layer followed by a feedforward neural network with a multinomial (i.e., softmax) output layer	1, 2, 3, 4, 5, or 6	128, 256, or 512	0% or 20%	2184
APM_{OR}	Class-weighted embedding and weight-averaging layer followed by a feedforward neural network with an ordinal (i.e., sigmoid at each threshold) output layer	1, 2, 3, 4, 5, or 6	128, 256, or 512	0% or 20%	2184

*The first hidden layer corresponds to the embedding and weight-averaging layer.
†Different hidden layers may have distinct numbers of neurons.

References

1. Paszke A, Gross S, Massa F, Lerer A, Bradbury J, Chanan G, et al. PyTorch: An Imperative Style, High-Performance Deep Learning Library. In: Wallach H, Larochelle H, Beygelzimer A, d'Alché-Buc F, Fox E, Garnett R, editors. Advances in Neural Information Processing Systems 32 (NeurIPS 2019). Vancouver: NeurIPS; 2019.

2. Kingma DP, Ba J. Adam: A Method for Stochastic Optimization. arXiv:1412.6980v9 [Preprint]. 2017 [cited 2021 December 26]. Available from: https://arxiv.org/abs/1412.6980

S3 Appendix: Detailed explanation of ordinal model performance and calibration metrics

In this appendix, we will describe each of our selected testing set discrimination, classification, and calibration metrics in mathematical and interpretive detail. Much of this information has already been published by Van Calster et al [1] and Austin et al [2], but we summarise and adapt it here for the ease of the reader. For each of the metrics, we derive the no information value (NIV), which corresponds to the metric value a model would theoretically achieve in the absence of predictive information, and the ideal, full information value (FIV).

Discrimination performance metrics

First, as a reference, let us define the dichotomous *c*-index, also known as the area under the receiver operating characteristic curve (AUC). Let us first assume a dichotomous prediction problem, in which there are N_1 patients with outcome 1 and N_2 patients with outcome 2. For a patient of outcome 1, let us denote the predicted probability of outcome 1 as p_{1,n_1}, where $n_1 \in [\![1, N_1]\!]$. Likewise, for a patient of outcome 2, let us denote the predicted probability of outcome 1 as p_{1,n_2}, where $n_2 \in [\![1, N_2]\!]$. The dichotomous *c*-index is then defined as:

$$c = \frac{1}{N_1 N_2} \sum_{n_1=1}^{N_1} \sum_{n_2=1}^{N_2} I_{p_{1,n_1} > p_{1,n_2}}$$

where $I_{p_{1,n_1} > p_{1,n_2}}$ is an indicator variable defined by:

$$I_{p_{1,n_1} > p_{1,n_2}} = \begin{cases} 1 \text{ if } p_{1,n_1} > p_{1,n_2}; \\ 0.5 \text{ if } p_{1,n_1} = p_{1,n_2}; \\ 0 \text{ otherwise.} \end{cases}$$

Thus, the dichotomous *c*-index can be interpreted as the probability that a model correctly separates 2 patients of different outcome. The dichotomous *c*-index is the most widely used discrimination metric for binary outcome prediction; however, there is no trivial extension for ordinal outcome prediction [3]. In this appendix, we explore the extensions used for our study.

Ordinal *c*-index (ORC)

The ordinal *c*-index (ORC), developed by Van Calster et al [1], is the primary metric of model discrimination performance in our study. Consider a set of 7 randomly chosen patients, each of one of the GOSE scores in our study, such that each patient is represented by n_o where $o \in \{1,2 \text{ or } 3, 4,5,6,7,8\}$. Now suppose an ordinal GOSE prediction model, such as one of those presented in **Fig 1A**, receives this set of patients

and is tasked with ranking the patients in order of predicted functional outcome. Let $\Pr^{(n_o)}(GOSE > t)$ represent the predicted probability, returned by our model, at threshold $t \in \{1,3,4,5,6,7\}$ for patient $n_o \in \{n_1, n_{2\text{ or }3}, n_4, n_5, n_6, n_7, n_8\}$ in our set. One way the model could achieve this ranking is to start with the lowest threshold ($GOSE > 1$), select the patient with the lowest probability at this threshold (i.e., $\underset{n_o}{\operatorname{argmin}} \Pr^{(n_o)}(GOSE > 1)$), set that patient aside as the lowest ranked patient, move on to the subsequent threshold ($GOSE > 3$), repeat this process for the remaining patients, and repeat at subsequent thresholds until a single patient remains for the highest rank. The ideal predicted ranking would be $n_1 < n_{2\text{ or }3} < n_4 < n_5 < n_6 < n_7 < n_8$. The primary rationale behind ORC is to calculate the average proportional "closeness" between the model-predicted ranking and this ideal ranking. To achieve a mathematical definition for closeness, the developers of ORC considered a scenario: suppose the model-predicted ranking of the given set is: $n_1 < n_4 < n_5 < n_{2\text{ or }3} < n_6 < n_8 < n_7$. From this predicted ranking, we would require at least 3 pairwise switching steps to achieve the target rank. For example:

- *Step 1*: switch n_4 and $n_{2\text{ or }3}$. *Result*: $n_1 < n_{2\text{ or }3} < n_5 < n_4 < n_6 < n_8 < n_7$
- *Step 2*: switch n_5 and n_4. *Result*: $n_1 < n_{2\text{ or }3} < n_4 < n_5 < n_6 < n_8 < n_7$
- *Step 3*: switch n_8 and n_7. *Result*: $n_1 < n_{2\text{ or }3} < n_4 < n_5 < n_6 < n_7 < n_8$

Let us define *S* as the number of necessary pairwise switching steps (i.e., the number of incorrect pairwise orderings) to reach the ideal ranking. Trivially, the ideal *S* ($S_{\min}$) is 0. In the worst possible scenario, in which the predicted ranking is a complete reversal of the ideal ranking (i.e., $n_8 < n_7 < n_6 < n_5 < n_4 < n_{2\text{ or }3} < n_1$), one would require the maximum number of unique pairwise switching steps possible to achieve the ideal ranking. Since we have 7 possible outcome categories, this is equivalent to $S_{max} = \binom{7}{2} = 21$. In the case of a tie, we add 0.5 to *S*. The definition of the proportion of closeness, denoted as C, between the model-predicted ranking and the ideal ranking for a given set is thus:

$$C = 1 - \frac{S}{S_{max}} = 1 - \frac{S}{21}$$

In the example provided above, where $S = 3$, the proportional closeness between the predicted ranking and the ideal ranking is $C = 1 - \frac{3}{21} \approx 0.86$. Thus, to define ORC as the average proportional closeness in ranking over all possible sets,

$$\boldsymbol{ORC} = \frac{1}{N_1 N_{2\text{ or }3} N_4 N_5 N_6 N_7 N_8} \sum_{n_1=1}^{N_1} \sum_{n_{2\text{ or }3}=1}^{N_{2\text{ or }3}} \sum_{n_4=1}^{N_4} \sum_{n_5=1}^{N_5} \sum_{n_6=1}^{N_6} \sum_{n_7=1}^{N_7} \sum_{n_8=1}^{N_8} C_{n_1, n_{2\text{ or }3}, n_4, n_5, n_6, n_7, n_8}$$

where $N_o \; \forall \; o \in \{1,2 \text{ or } 3, 4,5,6,7,8\}$ denotes the number of patients of GOSE score o, and $C_{n_1 n_{2\text{ or }3} n_4 n_5 n_6 n_7 n_8}$ denotes the proportional closeness of the model ranking to the ideal ranking for patient set $\{n_1, n_{2\text{ or }3}, n_4, n_5, n_6, n_7, n_8\}$. Furthermore, if we simplify this formula:

$$ORC = \frac{1}{N_1 N_{2\text{ or }3} N_4 N_5 N_6 N_7 N_8} \sum_{n_1=1}^{N_1} \sum_{n_{2\text{ or }3}=1}^{N_{2\text{ or }3}} \sum_{n_4=1}^{N_4} \sum_{n_5=1}^{N_5} \sum_{n_6=1}^{N_6} \sum_{n_7=1}^{N_7} \sum_{n_8=1}^{N_8} C_{n_1,n_{2\text{ or }3},n_4,n_5,n_6,n_7,n_8}$$

$$= \frac{1}{N_1 N_{2\text{ or }3} N_4 N_5 N_6 N_7 N_8} \sum_{n_1=1}^{N_1} \sum_{n_{2\text{ or }3}=1}^{N_{2\text{ or }3}} \sum_{n_4=1}^{N_4} \sum_{n_5=1}^{N_5} \sum_{n_6=1}^{N_6} \sum_{n_7=1}^{N_7} \sum_{n_8=1}^{N_8} \left[1 - \frac{S_{n_1,n_{2\text{ or }3},n_4,n_5,n_6,n_7,n_8}}{S_{max}}\right]$$

$$= \frac{1}{N_1 N_{2\text{ or }3} N_4 N_5 N_6 N_7 N_8} \sum_{n_1=1}^{N_1} \sum_{n_{2\text{ or }3}=1}^{N_{2\text{ or }3}} \sum_{n_4=1}^{N_4} \sum_{n_5=1}^{N_5} \sum_{n_6=1}^{N_6} \sum_{n_7=1}^{N_7} \sum_{n_8=1}^{N_8} \left[\frac{S_{max} - S_{n_1,n_{2\text{ or }3},n_4,n_5,n_6,n_7,n_8}}{S_{max}}\right]$$

$$= \frac{1}{N_1 N_{2\text{ or }3} N_4 N_5 N_6 N_7 N_8} \sum_{n_1=1}^{N_1} \sum_{n_{2\text{ or }3}=1}^{N_{2\text{ or }3}} \sum_{n_4=1}^{N_4} \sum_{n_5=1}^{N_5} \sum_{n_6=1}^{N_6} \sum_{n_7=1}^{N_7} \sum_{n_8=1}^{N_8} \left[\frac{1}{\binom{7}{2}} \sum_{i=1}^{6} \sum_{j=i+1}^{7} (S_{max} - S_{n_1,n_{2\text{ or }3},n_4,n_5,n_6,n_7,n_8})\right]$$

$$= \frac{1}{N_1 N_{2\text{ or }3} N_4 N_5 N_6 N_7 N_8} \sum_{n_1=1}^{N_1} \sum_{n_{2\text{ or }3}=1}^{N_{2\text{ or }3}} \sum_{n_4=1}^{N_4} \sum_{n_5=1}^{N_5} \sum_{n_6=1}^{N_6} \sum_{n_7=1}^{N_7} \sum_{n_8=1}^{N_8} \left[\frac{1}{\binom{7}{2}} \sum_{i=1}^{7} \sum_{j=i+1}^{8} I_{o_{n_j} > o_{n_i}}\right]$$

$$= \frac{1}{\binom{7}{2}} \sum_{i=1}^{7} \sum_{j=i+1}^{8} \left[\frac{1}{N_1 N_{2\text{ or }3} N_4 N_5 N_6 N_7 N_8} \sum_{n_1=1}^{N_1} \sum_{n_{2\text{ or }3}=1}^{N_{2\text{ or }3}} \sum_{n_4=1}^{N_4} \sum_{n_5=1}^{N_5} \sum_{n_6=1}^{N_6} \sum_{n_7=1}^{N_7} \sum_{n_8=1}^{N_8} I_{o_{n_j} > o_{n_i}}\right]$$

$$= \frac{1}{\binom{7}{2}} \sum_{i=1}^{7} \sum_{j=i+1}^{8} \left[\frac{1}{N_i N_j} \sum_{n_i=1}^{N_i} \sum_{n_j=1}^{N_j} I_{o_{n_j} > o_{n_i}}\right]$$

$$\boxed{= \frac{1}{\binom{7}{2}} \sum_{i=1}^{7} \sum_{j=i+1}^{8} c_{ij}}$$

which is equivalent to the unweighted average of all pairwise *c*-indices. Therefore, another interpretation of ORC is the probability of a model correctly separating 2 randomly selected patients of 2 randomly selected GOSE scores. Moreover, since the NIV of the *c*-index is 0.5 for random guessing and the FIV is 1, we know that ORC shares the same feasible range of values: $\mathbf{NIV_{ORC}}$ = 0.5 and $\mathbf{FIV_{ORC}}$ = 1. Finally, if there were only 2 possible ordinal outcome categories, we observe that ORC collapses into the dichotomous *c*-index.

The ORC is independent of the prevalence of each GOSE score in the dataset, as each possible set of patients is equally weighted regardless of frequency.

Somers' D_{xy}

The generalised *c*-index, described by Harrell et al [4,5], is defined as the proportion of possible pairs of patients of different functional outcomes in the entire study population which the model correctly discriminates. A pair of patients of different outcomes is defined as a comparable pair and a pair of patients of different outcomes that is correctly discriminated is defined as a concordant pair. Let N^{comp} denote the total number of comparable pairs in the study set and let N^{conc} denote the total number of concordant pairs in the study set. Thus, the generalised *c*-index is defined as:

$$\text{Generalised } c-\text{index} = \frac{N^{conc}}{N^{comp}}$$

Upon simplification,

$$= \frac{N^{conc}}{\sum_{i=1}^{7}\sum_{j=i+1}^{8} N_i N_j}$$

$$= \frac{\sum_{i=1}^{7}\sum_{j=i+1}^{8} N_{ij}^{conc}}{\sum_{i=1}^{7}\sum_{j=i+1}^{8} N_i N_j}$$

$$= \frac{\sum_{i=1}^{7}\sum_{j=i+1}^{8} N_i N_j c_{ij}}{\sum_{i=1}^{7}\sum_{j=i+1}^{8} N_i N_j}$$

we find that the generalised *c*-index is equivalent to a prevalence-weighted average of pairwise *c*-indices. Therefore, the generalised *c*-index shares the same feasible range of values as the dichotomous *c*-index: $NIV_{\text{Generalised } c\text{-index}} = 0.5$ and $FIV_{\text{Generalised } c\text{-index}} = 1$. However, in contrast to ORC, generalised *c*-index is dependent on the prevalence of GOSE scores in the patient set.

Somers' D_{xy} [6,7] is defined as the proportion of the difference between the number of concordant pairs and the number of discordant pairs to the total number of comparable pairs:

$$\boxed{\textbf{Somers' } \boldsymbol{D_{xy}} = \frac{N^{conc} - N^{discord}}{N^{comp}}}$$

Upon simplification,

$$= \frac{N^{conc} - (N^{comp} - N^{conc})}{N^{comp}}$$

$$= \frac{2N^{conc} - N^{comp}}{N^{comp}}$$

$$= 2\frac{N^{conc}}{N^{comp}} - 1$$

$$= 2(\text{Generalised } c - \text{index}) - 1$$

we observe the relationship between Somers' D_{xy} and the generalised *c*-index. Therefore, the feasible range of Somers' D_{xy} is: **NIV$_{\text{Somers' } D_{xy}}$** = 2(0.5) – 1 = 0 and **FIV$_{\text{Somers' } D_{xy}}$** = 2(1) – 1 = 1. Moreover, Somers' D_{xy} is also dependent on the prevalence of GOSE scores in the patient set. Somers' D_{xy} can also be interpreted as the proportion of ordinal variation in the outcome that can be explained by the variation in model output.

Threshold-level dichotomous *c*-index

The threshold-level dichotomous *c*-indices represent the probability of the model correctly discriminating 2 randomly selected patients, one on each side of the threshold of functional recovery. The average of the threshold-level *c*-indices across the 6 possible GOSE thresholds represents the probability of the model correctly discriminating 2 patients, one on each side of a randomly selected GOSE threshold. The average threshold-level dichotomous *c*-index is also a prevalence-weighted form of the pairwise *c*-index, though weighting is not perfectly aligned with prevalence as with the generalised *c*-index [1]. The feasible range of dichotomous *c*-indices are: **NIV$_{\text{Dichotomous } c\text{-index}}$** = 0.5 to **FIV$_{\text{Dichotomous } c\text{-index}}$** = 1.

Probability calibration metrics

Threshold-level calibration slope

Let $Y \in \{0,1\}$ designate the true outcome at a threshold of GOSE and let $p_{pred} \in [0,1]$ designate the predicted probability value returned by a model at this threshold. The logistic recalibration framework [8] fits the following model from the testing set predictions: $\text{logit}(Y) = \beta_0 + \beta_1 \text{logit}(p_{pred})$. β_1 represents the calibration slope [9]. When $\beta_0 = 0$ and $\beta_1 = 1$, the model is calibrated. When $\beta_1 < 1$, the model is overfitted and returns too extreme values: higher p_{pred} are overestimated while lower p_{pred} are underestimated. When $\beta_1 > 1$, the model is underfitted and the converse is true. We do not focus on β_0 in our study because, in the setting of cross-validation, β_0 is not relevant [10].

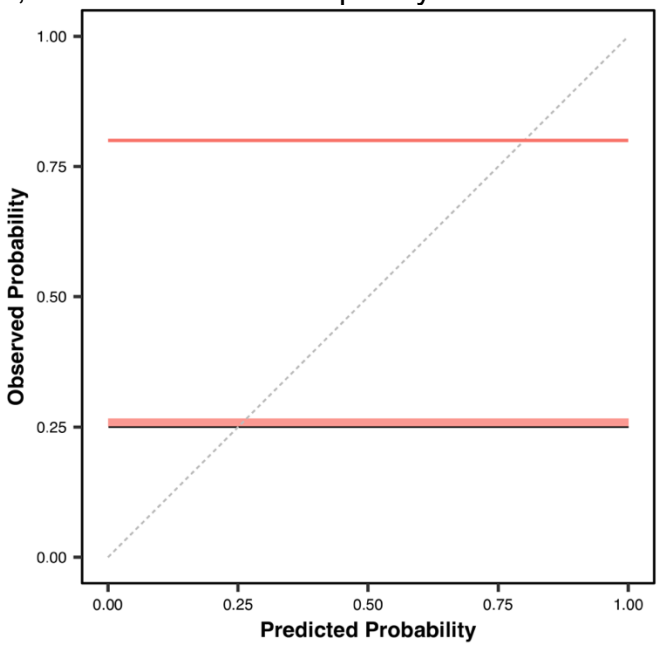
Threshold-level Integrated calibration index (ICI)

On the threshold-level probabilities and threshold-level outcomes of the testing set predictions, we fit a locally weighted scatterplot smoothing (LOWESS) function [11] to return the observed probability at each predicted probability value [12]. The range of corresponding observed probability for each predicted probability is visualised in a

smoothed probability calibration plot (**Fig 3B**). Let $p_{pred} \in [0,1]$ denote a predicted probability value and $p_{obs}(p_{pred}) \in [0,1]$ denote the corresponding observed probability value. Then, the calibration error function, denoted as $E_{calibration}$, is defined as: $\boldsymbol{E_{calibration}(p_{pred})} = \left|p_{obs}(p_{pred}) - p_{pred}\right|$.

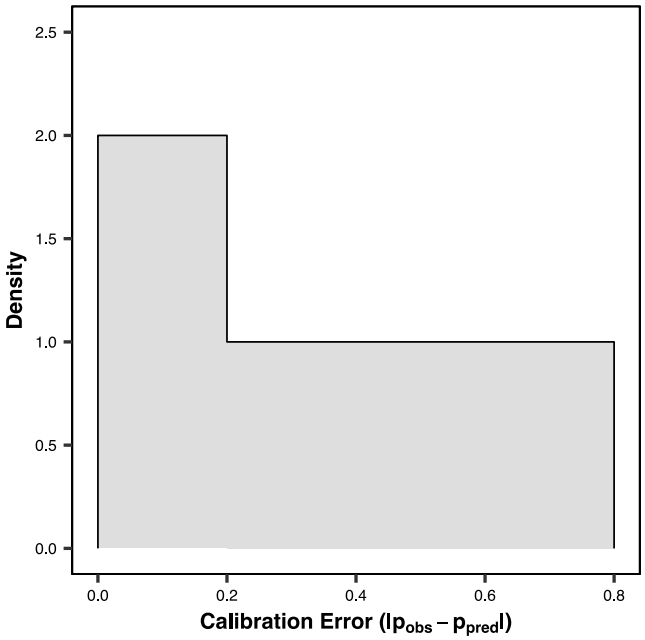
The integrated calibration index (ICI) corresponds to the mean calibration error [2]. Since the ideal calibration error is 0, the $\mathbf{FIV_{ICI}}$ is trivially 0. However, the calculation of the NIV varies based on the outcome distribution at each threshold.

Consider the case of random guessing during prediction at a given threshold. This implies that the model returns predicted probabilities uniformly from 0 to 1, regardless of any patient information (**S3A.1 Fig**). Therefore, the corresponding observed probability at each predicted probability value equals π_{above}, the proportion of patients above the given threshold (**S3A.1 Fig**). In other words, there is no association between predicted and observed probabilities, and the model is completely uncalibrated.



S3A.1 Fig. Example of a probability calibration curve for a random-guessing prediction model at a given threshold of GOSE. The histogram (200 uniform bins), centred at the horizontal line in the bottom quarter, displays the uniform distribution of predicted probabilities for a random guessing model. This plot assumes that the proportion of patients above the threshold (π_{above}) is 0.8.

From the probability calibration curve (**S3A.1 Fig**), we derive a graphical representation of the probability density function of $E_{calibration}$ in **S3A.2 Fig**. This corresponds to an asymmetrical (if $\pi_{above} \neq 0.5$) distribution with density 2 up to $E_{calibration} = \min\{\pi_{above}, 1-\pi_{above}\}$ and then density 1 from $E_{calibration} = \min\{\pi_{above}, 1-\pi_{above}\}$ to $E_{calibration} = \max\{\pi_{above}, 1-\pi_{above}\}$ (**S3A.2 Fig**).



S3A.2 Fig. Example of probability density of calibration error for a random-guessing prediction model at a given threshold of GOSE. This plot assumes that the proportion of patients above the threshold (π_{above}) is 0.8.

ICI is equivalent to the integral of the calibration error function over all returned probability prediction values:

$$\boldsymbol{ICI} = \frac{1}{\max\{p_{pred}\} - \min\{p_{pred}\}} \int_{\min\{p_{pred}\}}^{\max\{p_{pred}\}} f_{P_{pred}}(p_{pred})\, E_{calibration}(p_{pred})\, dp_{pred}$$

where $f_{P_{pred}}(p_{pred})$ represents the probability density function over p_{pred}values. For the random-guessing model, we determined that p_{obs} is constant, i.e., $p_{obs}(p_{pred}) = \pi_{above}\ \forall\ p_{pred} \in [0,1]$ at each threshold. Moreover, p_{pred} is distributed uniformly from 0 to 1. Therefore:

$$\boldsymbol{NIV_{ICI}} = \int_0^1 E_{calibration}(p_{pred})\, dp_{pred}$$

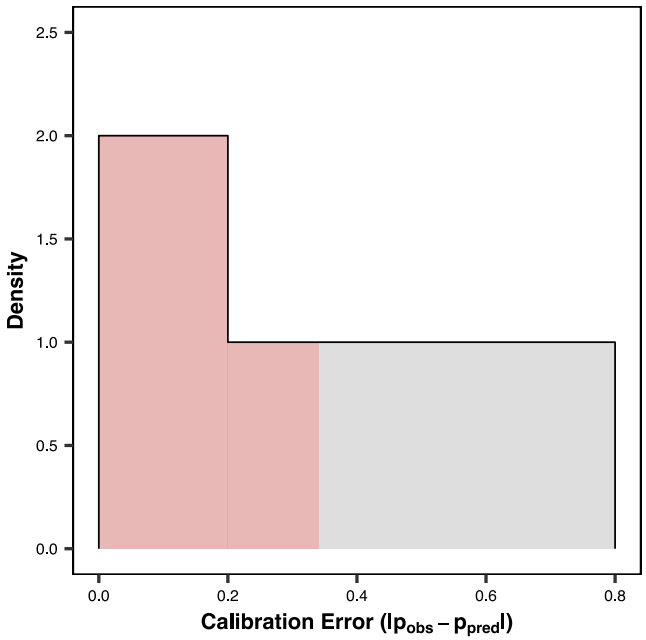
$$= \int_0^1 \left|\pi_{above} - p_{pred}\right| dp_{pred}$$

$$= \int_0^{\pi_{above}} (\pi_{above} - p_{pred})\, dp_{pred} + \int_{\pi_{above}}^1 (p_{pred} - \pi_{above})\, dp_{pred}$$

$$= \frac{1}{2}\pi_{above}^2 + \frac{1}{2}(1 - \pi_{above})^2$$

$$= \pi_{above}^2 - \pi_{above} + \frac{1}{2}$$

A graphical representation of cumulative distribution up to the NIV_{ICI} for our example is provided in **S3A.3 Fig**.



S3A.3 Fig. Example of cumulative probability density up to ICI for a random-guessing prediction model at a given threshold of GOSE. This plot assumes that the proportion of patients above the threshold (π_{above}) is 0.8. The ICI equals 0.34 in calibration error.

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S4 Appendix: Hyperparameter optimisation results

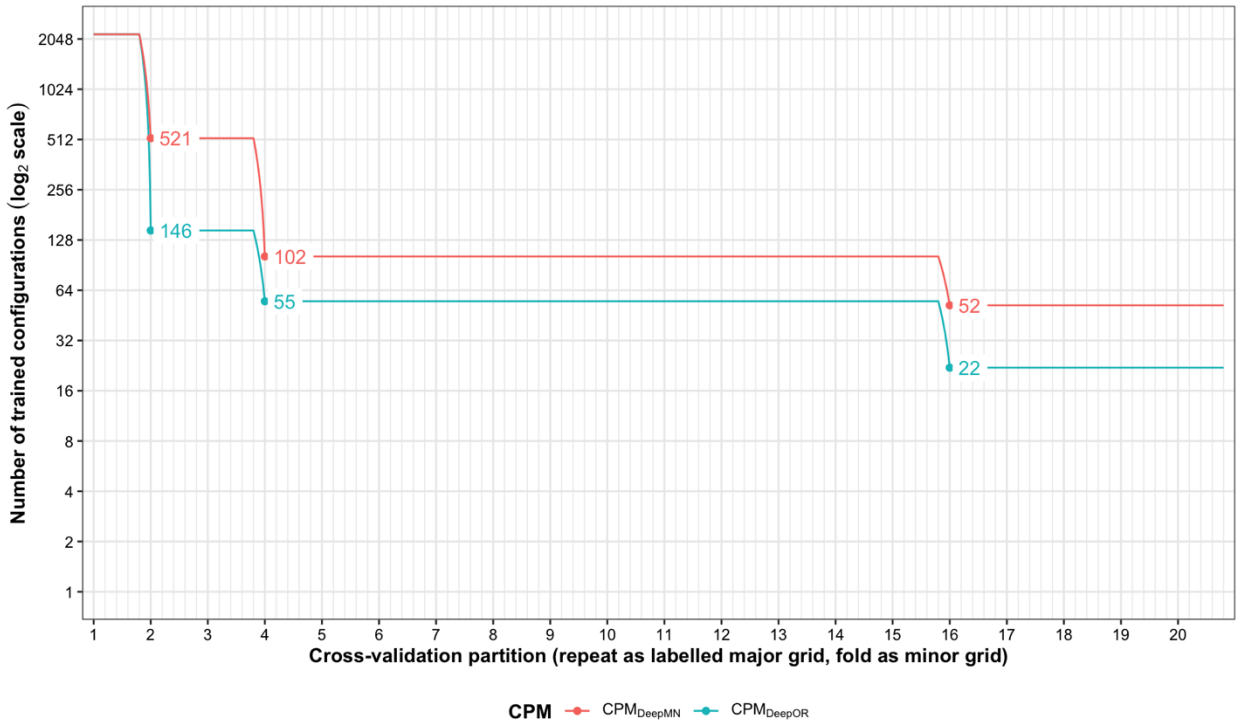
Training for each of the parametric models (CPM_{DeepMN}, CPM_{DeepOR}, APM_{MN}, APM_{OR}, $eCPM_{DeepMN}$, and $eCPM_{DeepOR}$) was made more efficient by dropping out consistently underperforming parametric configurations, on the validation sets, with the Bootstrap Bias Corrected with Dropping Cross-Validation (BBCD-CV) method [1]. During configuration dropout, the optimal configuration for each model was determined over all existing validation set predictions up to that point, and 1,000 resamples of unique patients were drawn to form bootstrapping resamples for the testing of suboptimal configurations versus the optimal configuration in terms of ordinal *c*-index (ORC) [2]. If a given suboptimal configuration was unable to match or outperform the optimal configuration in at least 5% of the resamples, it was dropped out from training in future repeated *k*-fold cross-validation partitions.

Each of the models began repeated *k*-fold cross-validation training with 2,184 parametric configurations (as detailed in **S1 Appendix** and **S2 Appendix**). Under the repeated *k*-fold cross validation scheme of our study, models were trained in the order of repeats (from 1 to 20), and, within each repeat, in the order of folds (from 1 to 5). After training all viable configurations up to a certain partition, BBCD-CV was performed. The decision of which partitions was dependent on the number of remaining viable configurations and the availability of relevant cores (e.g., APM training required GPUs) on the high-performance computer (HPC), and thus varied by model. Since models of the same predictor set were trained together (i.e., CPM_{DeepMN} and CPM_{DeepOR}), BBCD-CV was performed for each of the models of a certain predictor set at after the same partition and a different optimal configuration was determined for each model.

In this appendix, we demonstrate the results of BBCD-CV hyperparameter optimisation by model type. First, we list the partitions after which BBCD-CV was performed, demonstrate the number of configurations dropped at these points, and characterise the variable hyperparameter distribution of the remaining viable configurations.

Concise-predictor-based models (CPMs)

BBCD-CV was performed thrice for CPM_{DeepMN} and CPM_{DeepOR}, after the end of: (1) repeat 1, (2) repeat 3, and (3) repeat 15. The number of remaining viable configurations after these dropouts is visualised, on a binary logarithmic scale, in **S4A.1 Fig**. The distribution of hyperparameters in the viable configurations, after each dropout, are listed in **S4A.1 Table** and **S4A.2 Table** for CPM_{DeepMN} and CPM_{DeepOR}, respectively.



S4A.1 Fig. Number of trained viable configurations for each CPM during repeated *k*-fold cross-validation.

S4A.1 Table. Variable hyperparameter distributions after each dropout for CPM_{DeepMN}.

Hyperparameter	Value	Starting configurations (*n* = 2184)	Remaining configurations after		
			Repeat 1 (*n* = 521)	**Repeat 3** (*n* = 102)	**Repeat 15** (*n* = 52)
Training dropout per layer					
	0	1092 (50.0%)	221 (42.4%)	19 (18.6%)	8 (15.4%)
	0.2	1092 (50.0%)	300 (57.6%)	83 (81.4%)	44 (84.6%)
Number of layers					
	1	6 (0.3%)	0 (0%)	0 (0%)	0 (0%)
	2	18 (0.8%)	3 (0.6%)	2 (2.0%)	1 (1.9%)
	3	54 (2.5%)	10 (1.9%)	4 (3.9%)	4 (7.7%)
	4	162 (7.4%)	32 (6.1%)	12 (11.8%)	8 (15.4%)
	5	486 (22.3%)	143 (27.4%)	57 (55.9%)	38 (73.1%)
	6	1458 (66.8%)	333 (63.9%)	27 (26.5%)	1 (1.9%)
Median number of neurons per layer					
	128	284 (13.0%)	90 (17.3%)	32 (31.4%)	18 (34.6%)
	192	320 (14.7%)	67 (12.9%)	8 (7.8%)	3 (5.8%)
	256	920 (42.1%)	230 (44.1%)	44 (43.1%)	25 (48.1%)
	320	56 (2.6%)	9 (1.7%)	2 (2.0%)	0 (0%)
	384	320 (14.7%)	58 (11.1%)	5 (4.9%)	2 (3.8%)
	512	284 (13.0%)	67 (12.9%)	11 (10.8%)	4 (7.7%)

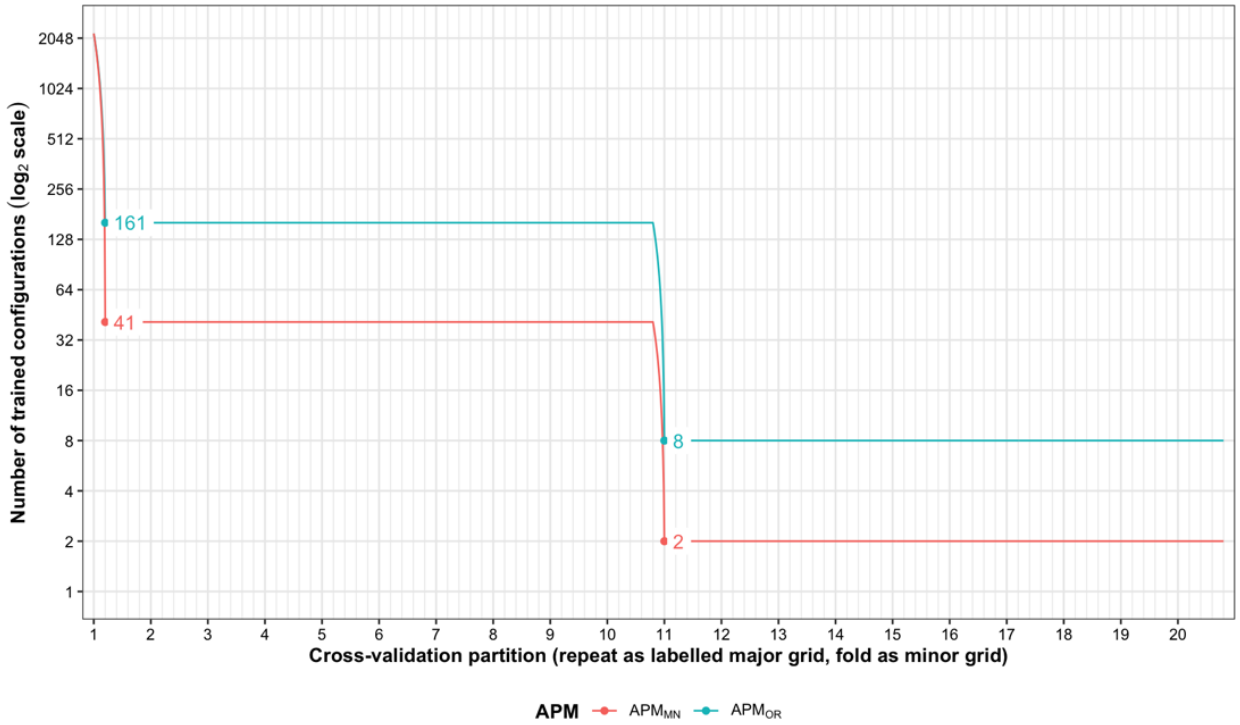
S4A.2 Table. Variable hyperparameter distributions after each dropout for CPM_{DeepOR}.

Hyperparameter	Value	Starting configurations (*n* = 2184)	Remaining configurations after		
			Repeat 1 (*n* = 146)	**Repeat 3** (*n* = 55)	**Repeat 15** (*n* = 22)

Training dropout per layer					
	0	1092 (50.0%)	42 (28.8%)	13 (23.6%)	5 (22.7%)
	0.2	1092 (50.0%)	104 (71.2%)	42 (76.4%)	17 (77.3%)
Number of layers					
	1	6 (0.3%)	0 (0%)	0 (0%)	0 (0%)
	2	18 (0.8%)	0 (0%)	0 (0%)	0 (0%)
	3	54 (2.5%)	2 (1.4%)	1 (1.8%)	1 (4.5%)
	4	162 (7.4%)	0 (0%)	0 (0%)	0 (0%)
	5	486 (22.3%)	56 (38.4%)	23 (41.8%)	12 (54.5%)
	6	1458 (66.8%)	88 (60.3%)	31 (56.4%)	9 (40.9%)
Median number of neurons per layer					
	128	284 (13.0%)	23 (15.8%)	7 (12.7%)	2 (9.1%)
	192	320 (14.7%)	16 (11.0%)	5 (9.1%)	2 (9.1%)
	256	920 (42.1%)	73 (50.0%)	28 (50.9%)	14 (63.6%)
	320	56 (2.6%)	1 (0.7%)	0 (0%)	0 (0%)
	384	320 (14.7%)	17 (11.6%)	6 (10.9%)	1 (4.5%)
	512	284 (13.0%)	16 (11.0%)	9 (16.4%)	3 (13.6%)

All-predictor-based models (APMs)

BBCD-CV was performed twice for APM_{MN} and APM_{OR}, after the end of: (1) the first fold of repeat 1, and (2) repeat 10. The number of remaining viable configurations after these dropouts is visualised, on a binary logarithmic scale, in **S4A.2 Fig**. The distribution of hyperparameters in the viable configurations, after each dropout, are listed in **S4A.3 Table** and **S4A.4 Table** for APM_{MN} and APM_{OR}, respectively.



S4A.2 Fig. Number of trained viable configurations for each APM during repeated *k*-fold cross-validation.

S4A.3 Table. Variable hyperparameter distributions after each dropout for APM_{MN}.

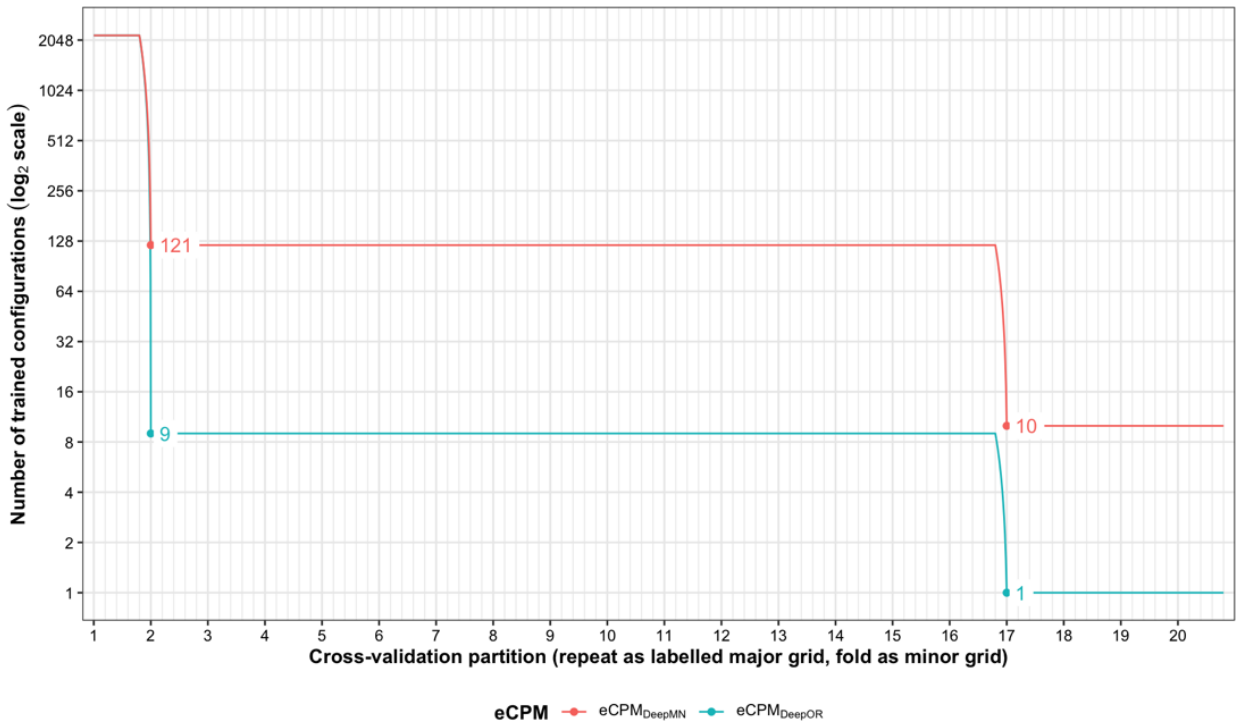
Hyperparameter	Value	Starting configurations (*n* = 2184)	Remaining configurations after	
			Repeat 1, Fold 1 (*n* = 41)	**Repeat 10** (*n* = 2)
Training dropout per layer				
	0	1092 (50.0%)	18 (43.9%)	1 (50.0%)
	0.2	1092 (50.0%)	23 (56.1%)	1 (50.0%)
Number of layers				
	1	6 (0.3%)	3 (7.3%)	2 (100.0%)
	2	18 (0.8%)	2 (4.9%)	0 (0%)
	3	54 (2.5%)	1 (2.4%)	0 (0%)
	4	162 (7.4%)	5 (12.2%)	0 (0%)
	5	486 (22.3%)	5 (12.2%)	0 (0%)
	6	1458 (66.8%)	25 (61.0%)	0 (0%)
Median number of neurons per layer				
	128	284 (13.0%)	3 (7.3%)	0 (0%)
	192	320 (14.7%)	5 (12.2%)	0 (0%)
	256	920 (42.1%)	19 (46.3%)	1 (50.0%)
	320	56 (2.6%)	0 (0%)	0 (0%)
	384	320 (14.7%)	8 (19.5%)	0 (0%)
	512	284 (13.0%)	6 (14.6%)	1 (50.0%)

S4A.4 Table. Variable hyperparameter distributions after each dropout for APM_{OR}.

Hyperparameter	Value	Starting configurations (*n* = 2184)	Remaining configurations after	
			Repeat 1, Fold 1 (*n* = 161)	**Repeat 10** (*n* = 8)
Training dropout per layer				
	0	1092 (50.0%)	22 (13.7%)	0 (0%)
	0.2	1092 (50.0%)	139 (86.3%)	8 (100.0%)
Number of layers				
	1	6 (0.3%)	1 (0.6%)	0 (0%)
	2	18 (0.8%)	1 (0.6%)	0 (0%)
	3	54 (2.5%)	5 (3.1%)	0 (0%)
	4	162 (7.4%)	13 (8.1%)	1 (12.5%)
	5	486 (22.3%)	36 (22.4%)	2 (25.0%)
	6	1458 (66.8%)	105 (65.2%)	5 (62.5%)
Median number of neurons per layer				
	128	284 (13.0%)	31 (19.3%)	2 (25.0%)
	192	320 (14.7%)	29 (18.0%)	4 (50.0%)
	256	920 (42.1%)	73 (45.3%)	1 (12.5%)
	320	56 (2.6%)	6 (3.7%)	0 (0%)
	384	320 (14.7%)	11 (6.8%)	0 (0%)
	512	284 (13.0%)	11 (6.8%)	1 (12.5%)

Extended concise-predictor-based models (eCPMs)

BBCD-CV was performed twice for $eCPM_{DeepMN}$ and $eCPM_{DeepOR}$, after the end of: (1) repeat 1, and (2) repeat 16. The number of remaining viable configurations after these dropouts is visualised, on a binary logarithmic scale, in **S4A.3 Fig**. The distribution of hyperparameters in the viable configurations, after each dropout, are listed in **S4A.5 Table** and **S4A.6 Table** for $eCPM_{DeepMN}$ and $eCPM_{DeepOR}$, respectively.



S4A.3 Fig. Number of trained viable configurations for each eCPM during repeated *k*-fold cross-validation.

S4A.5 Table. Variable hyperparameter distributions after each dropout for $eCPM_{DeepMN}$.

Hyperparameter	Value	Starting configurations (*n* = 2184)	Remaining configurations after	
			Repeat 1 (*n* = 121)	**Repeat 16** (*n* = 10)
Training dropout per layer				
	0	1092 (50.0%)	51 (42.1%)	4 (40.0%)
	0.2	1092 (50.0%)	70 (57.9%)	6 (60.0%)
Number of layers				
	1	6 (0.3%)	3 (2.5%)	2 (20.0%)
	2	18 (0.8%)	8 (6.6%)	3 (30.0%)
	3	54 (2.5%)	15 (12.4%)	3 (30.0%)
	4	162 (7.4%)	45 (37.2%)	2 (20.0%)
	5	486 (22.3%)	48 (39.7%)	0 (0%)
	6	1458 (66.8%)	2 (1.7%)	0 (0%)
Median number of neurons per layer				
	128	284 (13.0%)	21 (17.4%)	3 (30.0%)
	192	320 (14.7%)	14 (11.6%)	2 (20.0%)
	256	920 (42.1%)	55 (45.5%)	4 (40.0%)

320	56 (2.6%)	5 (4.1%)	0 (0%)
384	320 (14.7%)	11 (9.1%)	0 (0%)
512	284 (13.0%)	15 (12.4%)	1 (10.0%)

S4A.6 Table. Variable hyperparameter distributions after each dropout for $eCPM_{DeepOR}$.

Hyperparameter	Value	Starting configurations (*n* = 2184)	Remaining configurations after	
			Repeat 1 (*n* = 9)	**Repeat 16** (*n* = 1)
Training dropout per layer				
	0	1092 (50.0%)	1 (11.1%)	0 (0%)
	0.2	1092 (50.0%)	8 (88.9%)	1 (100.0%)
Number of layers				
	1	6 (0.3%)	1 (11.1%)	1 (100.0%)
	2	18 (0.8%)	4 (44.4%)	0 (0%)
	3	54 (2.5%)	2 (22.2%)	0 (0%)
	4	162 (7.4%)	1 (11.1%)	0 (0%)
	5	486 (22.3%)	0 (0%)	0 (0%)
	6	1458 (66.8%)	1 (11.1%)	0 (0%)
Median number of neurons per layer				
	128	284 (13.0%)	3 (33.3%)	0 (0%)
	192	320 (14.7%)	2 (22.2%)	0 (0%)
	256	920 (42.1%)	3 (33.3%)	1 (100.0%)
	320	56 (2.6%)	1 (11.1%)	0 (0%)
	384	320 (14.7%)	0 (0%)	0 (0%)
	512	284 (13.0%)	0 (0%)	0 (0%)

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S1 Table. Extended concise baseline predictors of the study population stratified by ordinal 6-month outcomes

Extended concise predictors	Overall	Glasgow Outcome Scale–Extended (GOSE) at 6 months post-injury							*p*-value[b]
	(*n* = 1550)	1	2 or 3	4	5	6	7	8	
		(*n* = 318)	(*n* = 262)	(*n* = 120)	(*n* = 227)	(*n* = 200)	(*n* = 206)	(*n* = 217)	
Age [years]	51 (31–66)	66 (50–76)	55 (36–68)	48 (29–61)	44 (31–56)	41 (27–53)	48 (31–65)	41 (24–61)	<0.0001
GCSm (n^a = 1509)	5 (1–6)	2 (1–5)	3 (1–5)	5 (1–6)	5 (1–6)	5 (2–6)	5 (3–6)	6 (5–6)	<0.0001
(1) No response	484 (32.1%)	152 (50.0%)	104 (40.6%)	35 (29.9%)	63 (28.5%)	46 (23.6%)	47 (23.0%)	37 (17.5%)	
(2) Abnormal extension	54 (3.6%)	17 (5.6%)	20 (7.8%)	4 (3.4%)	6 (2.7%)	3 (1.5%)	2 (1.0%)	2 (0.9%)	
(3) Abnormal flexion	63 (4.2%)	14 (4.6%)	12 (4.7%)	8 (6.8%)	11 (5.0%)	8 (4.1%)	4 (2.0%)	6 (2.8%)	
(4) Withdrawal from stimulus	114 (7.6%)	27 (8.9%)	23 (9.0%)	8 (6.8%)	20 (9.0%)	21 (10.8%)	8 (3.9%)	7 (3.3%)	
(5) Movement localised to stimulus	305 (20.2%)	52 (17.1%)	47 (18.4%)	24 (20.5%)	50 (22.6%)	46 (23.6%)	44 (21.6%)	42 (19.8%)	
(6) Obeys commands	489 (32.4%)	42 (13.8%)	50 (19.5%)	38 (32.5%)	71 (32.1%)	71 (36.4%)	99 (48.5%)	118 (55.7%)	
Unreactive pupils (n^a = 1465)									<0.0001
One	111 (7.6%)	31 (10.5%)	31 (12.3%)	7 (6.3%)	20 (9.3%)	5 (2.6%)	8 (4.1%)	9 (4.4%)	
Two	168 (11.5%)	84 (28.5%)	33 (13.0%)	8 (7.2%)	14 (6.5%)	8 (4.2%)	16 (8.2%)	5 (2.4%)	
Hypoxia	207 (13.4%)	60 (18.9%)	33 (12.6%)	14 (11.7%)	35 (15.4%)	33 (16.5%)	16 (7.8%)	16 (7.4%)	0.6272
Hypotension	210 (13.5%)	56 (17.6%)	51 (19.5%)	21 (17.5%)	32 (14.1%)	22 (11.0%)	15 (7.3%)	13 (6.0%)	0.0038
Marshall CT (n^a = 1255)	VI (II–VI)	III (II–VI)	II (II–VI)	II (II–VI)	II (II–II)	II (II–III)	II (II–II)	VI (II–VI)	0.0386
No visible pathology (I)	118 (9.4%)	8 (3.3%)	11 (5.3%)	5 (5.2%)	17 (8.7%)	25 (15.2%)	24 (13.6%)	28 (16.5%)	
Diffuse injury II	592 (47.2%)	56 (22.8%)	84 (40.6%)	54 (56.2%)	92 (47.2%)	100 (60.6%)	103 (58.5%)	103 (60.6%)	
Diffuse injury III	108 (8.6%)	42 (17.1%)	17 (8.2%)	10 (10.4%)	14 (7.2%)	9 (5.5%)	6 (3.4%)	10 (5.9%)	
Diffuse injury IV	16 (1.3%)	7 (2.8%)	1 (0.5%)	1 (1.0%)	4 (2.1%)	1 (0.6%)	1 (0.6%)	1 (0.6%)	
Mass lesion (V & VI)	421 (33.5%)	133 (54.0%)	94 (45.4%)	26 (27.1%)	68 (34.9%)	30 (18.2%)	42 (23.9%)	28 (16.5%)	
tSAH (n^a = 1254)	957 (76.3%)	221 (90.2%)	176 (84.2%)	73 (76.0%)	150 (76.9%)	106 (63.9%)	125 (71.4%)	106 (63.1%)	0.4429
EDH (n^a = 1257)	244 (19.4%)	31 (12.7%)	32 (15.3%)	21 (21.9%)	46 (23.6%)	32 (19.3%)	42 (23.9%)	40 (23.5%)	0.0035
Glucose [mmol/L] (n^a = 1062)	7.7 (6.6–9.4)	8.8 (7.3–11)	8.0 (6.5–9.8)	7.6 (6.5–9.3)	7.8 (6.6–9.6)	7.7 (6.5–8.7)	7.3 (6.3–8.5)	7.1 (6.3–8.1)	0.0123
Hb [g/dL] (n^a = 1140)	13 (12–14)	13 (11–14)	13 (11–14)	14 (12–14)	13 (12–14)	14 (12–15)	13 (12–15)	14 (13–15)	0.3044
Retired (n^a = 1312)	353 (26.9%)	136 (61.3%)	74 (33.6%)	23 (22.1%)	12 (5.9%)	13 (7.3%)	52 (28.1%)	43 (21.8%)	0.0644
Highest formal education (n^a = 1110)									0.4897
None	15 (1.4%)	3 (2.4%)	4 (2.1%)	2 (2.0%)	2 (1.1%)	2 (1.2%)	0 (0%)	2 (1.1%)	
In degree program	26 (2.3%)	0 (0%)	5 (2.6%)	0 (0%)	4 (2.1%)	7 (4.1%)	4 (2.5%)	6 (3.4%)	
Primary school	155 (14.0%)	31 (24.6%)	44 (23.3%)	14 (13.9%)	17 (8.9%)	16 (9.5%)	14 (8.8%)	19 (10.9%)	

Secondary school	458 (41.3%)	50 (39.7%)	63 (33.3%)	46 (45.5%)	80 (42.1%)	59 (34.9%)	75 (46.9%)	85 (48.6%)	
Technical certificate	235 (21.2%)	16 (12.7%)	38 (20.1%)	21 (20.8%)	57 (30.0%)	43 (25.4%)	32 (20.0%)	28 (16.0%)	
University degree	221 (19.9%)	26 (20.6%)	35 (18.5%)	18 (17.8%)	30 (15.8%)	42 (24.9%)	35 (21.9%)	35 (20.0%)	
GFAP [ng/mL] (n^a = 1247)	17 (6–46)	48 (15–96)	32 (11–61)	17 (6–43)	13 (5–30)	13 (5–30)	10 (3–23)	9 (3–22)	0.0005
T-tau [pg/mL] (n^a = 1248)	8 (4–19)	17 (7–38)	12 (6–23)	9 (5–19)	7 (3–14)	7 (3–13)	5 (3–12)	6 (3–11)	0.2568
S100B [ng/mL] (n^a = 1267)	0.3 (.2–.6)	0.6 (.3–1.3)	0.4 (.2–.6)	0.3 (.2–.6)	0.3 (.2–.4)	0.2 (.2–.4)	0.2 (.1–.5)	0.2 (.1–.3)	0.1929
NFL [pg/mL] (n^a = 1247)	55 (28–127)	121 (51–268)	85 (46–150)	61 (32–150)	48 (28–87)	41 (21–87)	30 (17–60)	35 (19–74)	0.3054
PTA (n^a = 1530)	187 (12.2%)	5 (1.6%)	15 (5.8%)	10 (8.5%)	43 (19.3%)	33 (16.8%)	50 (24.4%)	31 (14.4%)	0.0010
Worst head/neck, brain, or cervical spine AIS (n^a = 1523)									0.0001
(1) Minor	50 (3.2%)	6 (1.9%)	3 (1.1%)	5 (4.2%)	5 (2.2%)	4 (2.0%)	16 (7.8%)	11 (5.1%)	
(2) Moderate	31 (2.0%)	3 (0.9%)	3 (1.1%)	0 (0%)	5 (2.2%)	4 (2.0%)	8 (3.9%)	8 (3.7%)	
(3) Serious	112 (7.2%)	6 (1.9%)	6 (2.3%)	7 (5.8%)	21 (9.3%)	19 (9.5%)	25 (12.1%)	28 (12.9%)	
(4) Severe	484 (31.2%)	63 (19.8%)	54 (20.6%)	37 (30.8%)	71 (31.3%)	78 (39.0%)	87 (42.2%)	94 (43.3%)	
(5) Critical	846 (54.6%)	216 (67.9%)	195 (74.4%)	70 (58.3%)	125 (55.1%)	94 (47.0%)	70 (34.0%)	76 (35.0%)	
(6) Not survivable	27 (1.7%)	24 (7.5%)	1 (0.4%)	1 (0.8%)	0 (0%)	1 (0.5%)	0 (0%)	0 (0%)	

Data are median (IQR) for continuous characteristics and *n* (% of column group) for categorical characteristics. Units of characteristics are provided in square brackets. GCSm=motor component score of the Glasgow Coma Scale. Marshall CT=Marshall computerised tomography classification. tSAH=traumatic subarachnoid haemorrhage. EDH=extradural haematoma. Glu=glucose. Hb=haemoglobin. GFAP=glial fibrillary acidic protein. T-tau=total tau protein. S100B=S100 calcium-binding protein B. NFL=neurofilament light chain. PTA=incidence of post-traumatic amnesia. AIS=abbreviated injury scale.

[a]Limited sample size of non-missing values for characteristic.

[b]*p*-values are determined from proportional odds logistic regression analysis trained on all concise predictors concurrently [19] and are combined across 100 missing value imputations via *z*-transformation [29]. For categorical variables with $k > 2$ categories (e.g., GCSm), *p*-values were calculated with a likelihood ratio test (with k-1 degrees of freedom) on POLR.

S2 Table. Ordinal concise-predictor-based model (CPM) discrimination and calibration performance

Metric	Threshold	Model			
		CPM_{MNLR}	**CPM_{POLR}**	**CPM_{DeepMN}**	**CPM_{DeepOR}**
Ordinal *c*-index (ORC)		0.69 (0.67–0.70)	0.69 (0.68–0.70)	0.70 (0.68–0.71)	0.59 (0.58–0.61)
Somers' D_{xy}		0.43 (0.41–0.45)	0.43 (0.41–0.46)	0.44 (0.41–0.48)	0.23 (0.20–0.26)
Threshold-level dichotomous *c*-index[a]		0.77 (0.75–0.78)	0.77 (0.75–0.78)	0.76 (0.74–0.78)	0.76 (0.73–0.78)
	GOSE > 1	0.83 (0.81–0.85)	0.83 (0.81–0.84)	0.83 (0.80–0.86)	0.82 (0.79–0.85)
	GOSE > 3	0.81 (0.79–0.83)	0.81 (0.79–0.82)	0.80 (0.78–0.83)	0.80 (0.77–0.82)
	GOSE > 4	0.78 (0.76–0.80)	0.78 (0.76–0.79)	0.77 (0.74–0.80)	0.77 (0.74–0.79)
	GOSE > 5	0.76 (0.74–0.77)	0.76 (0.74–0.77)	0.75 (0.72–0.78)	0.74 (0.71–0.77)
	GOSE > 6	0.72 (0.70–0.74)	0.71 (0.69–0.73)	0.71 (0.68–0.74)	0.71 (0.67–0.74)
	GOSE > 7	0.72 (0.69–0.74)	0.73 (0.70–0.75)	0.71 (0.67–0.75)	0.71 (0.67–0.75)
Threshold-level calibration slope[a]		0.85 (0.78–0.91)	0.94 (0.88–1.01)	0.98 (0.81–1.12)	0.90 (0.79–1.02)
	GOSE > 1	0.92 (0.84–1.00)	1.13 (1.04–1.23)	0.95 (0.78–1.10)	1.01 (0.85–1.18)
	GOSE > 3	0.92 (0.85–1.00)	1.14 (1.05–1.23)	0.97 (0.80–1.12)	0.95 (0.83–1.09)
	GOSE > 4	0.91 (0.84–1.00)	0.99 (0.91–1.08)	1.06 (0.86–1.23)	0.93 (0.80–1.06)
	GOSE > 5	0.88 (0.80–0.97)	0.90 (0.82–0.99)	1.01 (0.78–1.21)	0.90 (0.76–1.06)
	GOSE > 6	0.81 (0.71–0.91)	0.71 (0.63–0.80)	0.98 (0.73–1.20)	0.86 (0.67–1.06)
	GOSE > 7	0.64 (0.50–0.80)	0.77 (0.67–0.88)	0.92 (0.69–1.18)	0.78 (0.57–1.02)

Data represent mean (95% confidence interval) for the CPM based on a given metric. Interpretations for each metric are provided in **Materials and methods**. Mean and confidence interval values were derived using bias-corrected bootstrapping (1,000 resamples) and represent the variation across repeated *k*-fold cross-validation folds (20 repeats of 5 folds) and 100 missing value imputations. GOSE=Glasgow Outcome Scale – Extended at 6 months post-injury. The CPM types (CPM_{MNLR}, CPM_{POLR}, CPM_{DeepMN}, and CPM_{DeepOR}) are decoded in the **Materials and methods** and described in **S1 Appendix**.

[a]Values in these rows correspond to the unweighted average across all GOSE thresholds.

S3 Table. Ordinal all-predictor-based model (APM) discrimination and calibration performance

Metric	Threshold	Model	
		APM_{MN}	**APM_{OR}**
Ordinal *c*-index (ORC)		0.76 (0.74–0.77)	0.66 (0.65–0.68)
Somers' D_{xy}		0.57 (0.54–0.60)	0.37 (0.33–0.40)
Threshold-level dichotomous *c*-index[a]		0.82 (0.80–0.83)	0.78 (0.76–0.80)
	GOSE > 1	0.90 (0.88–0.92)	0.83 (0.81–0.85)
	GOSE > 3	0.86 (0.84–0.88)	0.82 (0.80–0.84)
	GOSE > 4	0.83 (0.80–0.85)	0.80 (0.78–0.82)
	GOSE > 5	0.80 (0.78–0.83)	0.78 (0.75–0.80)
	GOSE > 6	0.76 (0.73–0.79)	0.74 (0.71–0.77)
	GOSE > 7	0.75 (0.72–0.79)	0.71 (0.68–0.75)
Threshold-level calibration slope[a]		0.84 (0.76–0.91)	0.13 (0.12–0.15)
	GOSE > 1	0.98 (0.86–1.10)	0.35 (0.31–0.38)
	GOSE > 3	0.90 (0.80–1.02)	0.18 (0.16–0.21)
	GOSE > 4	0.89 (0.79–1.00)	0.10 (0.09–0.12)
	GOSE > 5	0.82 (0.72–0.94)	0.07 (0.06–0.09)
	GOSE > 6	0.74 (0.62–0.87)	0.06 (0.05–0.07)
	GOSE > 7	0.68 (0.54–0.83)	0.05 (0.04–0.06)

Data represent mean (95% confidence interval) for the APM based on a given metric. Interpretations for each metric are provided in **Materials and methods**. Mean and confidence interval values were derived using bias-corrected bootstrapping (1,000 resamples) and represent the variation across repeated *k*-fold cross-validation folds (20 repeats of 5 folds). GOSE=Glasgow Outcome Scale – Extended at 6 months post-injury. The APM types (APM_{MN} and APM_{OR}) are decoded in the **Materials and methods** and described in **S2 Appendix**.

[a]Values in these rows correspond to the unweighted average across all GOSE thresholds.

S4 Table. Ordinal extended concise-predictor-based model (eCPM) discrimination and calibration performance

Metric	Threshold	Model			
		eCPM$_{MNLR}$	**eCPM$_{POLR}$**	**eCPM$_{DeepMN}$**	**eCPM$_{DeepOR}$**
Ordinal *c*-index (ORC)		0.72 (0.71–0.73)	0.71 (0.70–0.72)	0.73 (0.71–0.74)	0.67 (0.65–0.68)
Somers' D_{xy}		0.50 (0.48–0.52)	0.47 (0.45–0.49)	0.50 (0.46–0.54)	0.38 (0.35–0.41)
Threshold-level dichotomous *c*-index[a]		0.79 (0.78–0.80)	0.79 (0.78–0.80)	0.79 (0.77–0.81)	0.77 (0.76–0.79)
	GOSE > 1	0.86 (0.84–0.87)	0.85 (0.84–0.87)	0.86 (0.83–0.88)	0.85 (0.82–0.87)
	GOSE > 3	0.84 (0.83–0.86)	0.84 (0.83–0.85)	0.84 (0.82–0.86)	0.83 (0.81–0.85)
	GOSE > 4	0.82 (0.80–0.83)	0.81 (0.80–0.83)	0.81 (0.79–0.83)	0.80 (0.77–0.82)
	GOSE > 5	0.77 (0.75–0.79)	0.77 (0.76–0.79)	0.77 (0.74–0.80)	0.76 (0.73–0.78)
	GOSE > 6	0.75 (0.73–0.77)	0.73 (0.71–0.75)	0.74 (0.70–0.77)	0.72 (0.69–0.75)
	GOSE > 7	0.72 (0.70–0.75)	0.73 (0.70–0.75)	0.72 (0.68–0.76)	0.70 (0.66–0.74)
Threshold-level calibration slope[a]		0.75 (0.70–0.81)	0.89 (0.83–0.95)	1.00 (0.78–1.14)	0.59 (0.51–0.67)
	GOSE > 1	0.81 (0.75–0.89)	0.97 (0.87–1.10)	0.98 (0.78–1.14)	1.04 (0.90–1.20)
	GOSE > 3	0.83 (0.77–0.90)	1.12 (1.04–1.23)	1.05 (0.81–1.20)	0.79 (0.68–0.90)
	GOSE > 4	0.81 (0.75–0.89)	1.02 (0.94–1.11)	1.10 (0.85–1.27)	0.60 (0.52–0.69)
	GOSE > 5	0.75 (0.67–0.82)	0.86 (0.78–0.94)	1.01 (0.76–1.22)	0.47 (0.38–0.56)
	GOSE > 6	0.72 (0.63–0.81)	0.69 (0.62–0.77)	0.97 (0.70–1.20)	0.36 (0.27–0.46)
	GOSE > 7	0.58 (0.48–0.69)	0.68 (0.59–0.77)	0.89 (0.61–1.18)	0.28 (0.16–0.40)

Data represent mean (95% confidence interval) for the eCPM based on a given metric. Interpretations for each metric are provided in **Materials and methods**. Mean and confidence interval values were derived using bias-corrected bootstrapping (1,000 resamples) and represent the variation across repeated *k*-fold cross-validation folds (20 repeats of 5 folds) and 100 missing value imputations. GOSE=Glasgow Outcome Scale – Extended at 6 months post-injury. The eCPM types (eCPM$_{MNLR}$, eCPM$_{POLR}$, eCPM$_{DeepMN}$, and eCPM$_{DeepOR}$) are decoded in the **Materials and methods** and described in **S1 Appendix**.

[a]Values in these rows correspond to the unweighted average across all GOSE thresholds.