# Supplementary Material: A mechanistic model of the neural entropy increase elicited by psychedelic drugs

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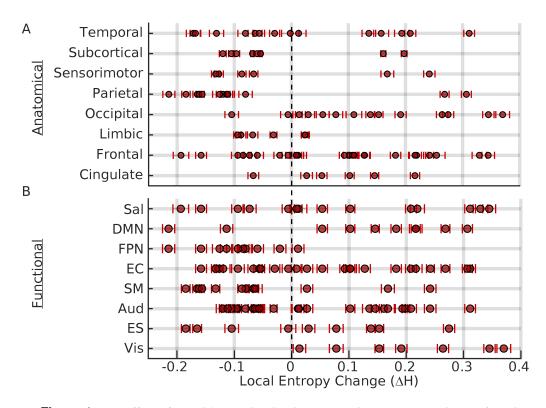
## ABSTRACT

Psychedelic drugs, including lysergic acid diethylamide (LSD) and other agonists of the serotonin 2A receptor (5HT2A-R), induce drastic changes in subjective experience, and provide a unique opportunity to study the neurobiological basis of consciousness. One of the most notable neurophysiological signatures of psychedelics, increased entropy in neural activity, is thought to be of crucial importance to the psychedelic experience, mediating both acute alterations in consciousness and long-term effects on well-being – yet, no mechanistic explanation of this phenomenon has been put forward so far. In this paper we undertake this task, and build upon a recent whole-brain model of serotonergic neuromodulation to study the entropic effects of 5HT2A-R activation. Our results reproduce the overall entropy increase observed in previous experiments *in vivo*, providing the first mechanistic account of this phenomenon. We also found that entropy changes were not uniform across the brain: entropy increased in some regions and decreased in others, suggesting a topographical reconfiguration mediated by 5HT2A-R activation. Interestingly, at the whole-brain level this reconfiguration was not explained by 5HT2A-R density, but by topological properties of the brain's anatomical connectivity. These results help us understand the mechanisms underlying the psychedelic state and, more generally, the pharmacological modulation of whole-brain activity.

#### Supplementary Subsection 1. Heterogeneous entropy changes induced by 5HT2A-R activation on anatomical and functional groupings of brain regions.

We asked whether the heterogeneous changes of entropy induced by 5HT2A-R activation could be explained by grouping the AAL brain regions according to anatomical and functional criteria. Regarding anatomical criteria brain regions can be spatially split into 8 major non-overlapping anatomical groups: Frontal, Temporal, Parietal, Occipital, Limbic, Sensorimotor, Cingulate and Subcortical.<sup>1</sup> Regarding the functional grouping, we used the Resting State Networks, a functional grouping of brain regions based on the observed spatio-temporal patterns of BOLD signals during resting state activity.<sup>2</sup> These groups are Salience (Sal), Fronto-Parietal (FPN), Default Mode (DMN), Primary Visual (Vis), Extrastiate Cortex (EC), Auditory (Aud), Sensorimotor (SM), and Executive Control (EC). The first one, Sal, was obtained from Lee*et al.*<sup>3</sup>, the second and third, FPN and DMN, were obtained from Oliver *et al.*<sup>4</sup>, and the rest from Beckmann *et al.*<sup>2</sup> Brain regions can potentially belong to different functional groups.

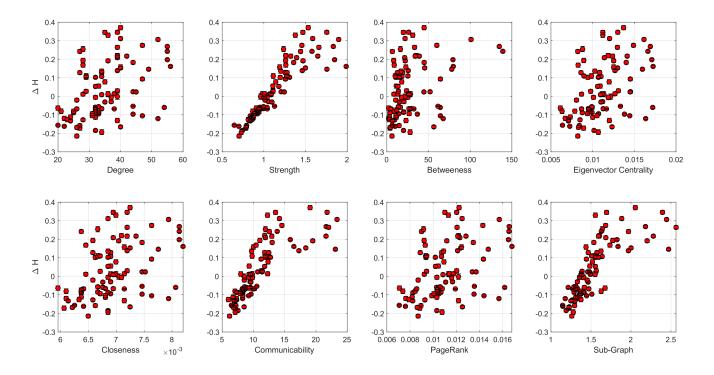
The effect of 5HT2A-R activation on entropy is heterogeneous also at the level of anatomical groups (Supplementary Figure 1A) – i.e. within all the groups there were both regions with increased and decreased entropy after the 5HT2A-R activation. However, Occipital and Cingulate regions show a strong tendency to increase their entropy, in agreement with entropy increases in these regions observed in human experiments with serotonergic psychedelics.<sup>5,6</sup> Regarding the functional grouping (Supplementary Figure 1B), we also found that the effect of 5HT2A-R activation on regional entropy (Fig. 3B) is heterogeneous within groups, with the exception of Vis and FPN, where almost all the regions increase their entropy, which resonates with the observed reduction of the DMN integrity on humans during psychedelic experiences.<sup>7</sup>



**Supplementary Figure 1.** The effect of 5HT2A-R activation is not explained by anatomical or functional groupings. (A) 5HT2A-R activation heterogeneously change entropy in regions belonging to the same anatomical group. (B) Entropy also changed in a heterogeneous way when functional grouping is considered. Note the special case of FPN and Vis networks, for which almost all regions decreased and increased their entropy, respectively (note that functional groups can be overlapping). Circles are averages and error bars 1 s.d. computed from 1000 simulations.

# Supplementary Subsection 2. Connectivity strength is the best predictor for entropy changes among local connectivity measures.

We control the role of local connectivity on the observed entropy changes ( $\Delta h_n$ ) induced by 5HT2A-R activation using as predictors for  $\Delta h_n$  other local connectivity measures as: degree,<sup>8</sup> eigenvector centrality,<sup>8</sup> communicability,<sup>9</sup> page-rank,<sup>8</sup> sub-graph centrality,<sup>8</sup> and closeness centrality.<sup>10</sup> We confirmed that local connectivity strength is the best linear predictor of entropy changes among other centrality measures.



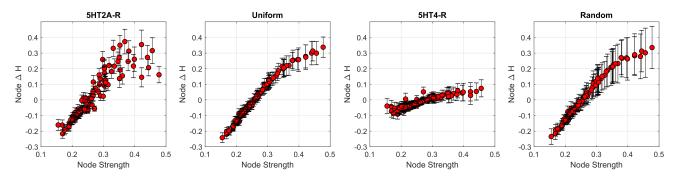
Supplementary Figure 2. Centrality measures as possible explanatory variables for  $\Delta h_n$ . Local connectivity strength is the best linear predictor of  $\Delta h_n$  among other centrality measures. Communicability and sub-graph centrality also show a good linear relationship with  $\Delta h_n$ , though with higher residual variance. Circles are averages and error bars 1 s.d. out of 1000 independent simulations.

#### Supplementary Subsection 3. Receptors controls.

We control the role of receptor density distribution on the observed entropy changes ( $\Delta h_n$ ) induced by 5HT2A-R activation by using alternative receptor distributions. To test the effect of the heterogeneous 5HT2A-R distribution on  $\Delta h_n$ , we used an uniform receptor distribution, where the receptor density for each region corresponds to the average 5HT2A-R density among all regions. To evaluate the role of the specific 5HT2A-R distribution, a randomised version of the 5HT2A-R was also used, where for each simulation the receptor expression is randomised. Finally, to evaluate the effect of activating other serotonin receptors, we used the 5HT4-R distribution, a receptor thought to play no role on the psychedelic state.

On the one hand, the Uniform and Random receptor distributions show almost the same behaviour on average, with  $\Delta h_n$  showing a linear relationship with the node strength that changed slope at node strength value ~ 0.35. The Random distribution shows more variability because the receptor distribution is randomised on each simulation. On the other hand, the 5HT4-R distribution changes entropy but in a subtler manner, yielding an average  $\Delta h_n \sim 0$ .

On summary, the heterogeneous 5HT2A-R distribution critically impacts the heterogeneity of  $\Delta h_n$  values and its relationship with the local connectivity strength. In addition, using other empirically-based distribution yields no significant change in average brain entropy, highlighting the key relationship between 5HT2A-R density and connectivity on the entropic effects induced by serotonergic psychedelic drugs.

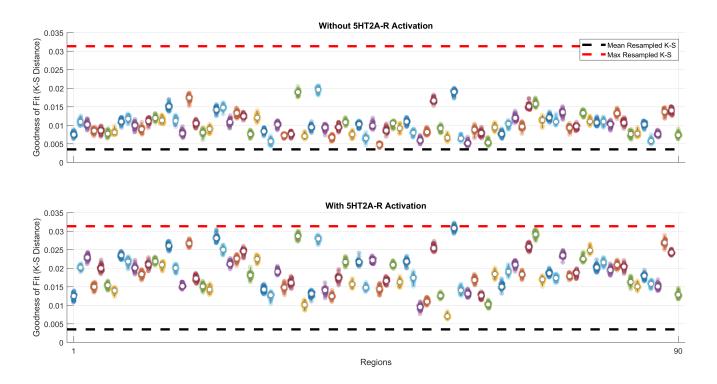


**Supplementary Figure 3.** Controls for receptor distribution vs  $\Delta h_n$ .  $\Delta h_n$  vs connectivity strength is plotted for 5HT2A-R, Uniform, 5HT4-R, and Random distribution of receptors (see text for details). The specific distribution of 5HT2A-R is critical both for the heterogeneity of  $\Delta h_n$  and for the average increase in local entropy. Circles are averages and error bars 1 s.d. out of 1000 independent simulations.

# Supplementary Subsection 4. The probability distribution of excitatory firing rates can be well fitted by a Gamma distribution.

To check the goodness of fit (GOF) of Gamma distribution to the simulated excitatory firing rates of each region, we generated 10<sup>6</sup> simulation points for each region under both PLA and 5HT2A condition, then, a Gamma distribution was fitted and the Kolmogorov-Smirnov (K-S) distance between the firing rate distribution and 1000 random samples (same size) of the respective fitted Gamma distribution was computed. We summarise the Gamma GOF as the average K-S for each region under both conditions. To assess the significance of average GOF values, we generated an acceptance interval computing the K-S distance between 100 independent samples (same size) sampled from exactly the same Gamma distribution (re-sampled K-S). This procedure was repeated for different set of Gamma distribution parameters. If the average K-S distance of a given region falls below the maximum re-sampled K-S distance, we consider this region to be well fitted by the Gamma distribution.

Despite the decreased GOF under 5HT2A condition (compared to PLA) all regions fall within the acceptance interval under both conditions, enabling us to use the Gamma distribution parameters to estimate each region's Shannon's differential entropy.



**Supplementary Figure 4.** Goodness of fit of Gamma distribution to firing rates distribution are within confidence intervals. Distribution of K-S distance values for PLA (top) and 5HT2A-R (bottom) condition for each region are represented by violins, where white circle denotes average K-S. Black (red) dashed line represent the average (maximum) re-sampled K-S distance (see the text for details).

## Supplementary Subsection 5. Brain Regions of the Automated Anatomical Labeling.

AAL Abbreviation	Brain Regions	
Precentral	Precental gyrus	
Front Sup	Superior frontal gyrus, dorsolateral	
Front Sup Orb	Superior frontal gyrus, orbital part	
Front Mid	Middle frontal gyrus	
Front Mid Orb	Middle frontal gyrus, orbital part	
Front Inf Oper	Inferior frontal gyrus, opercular part	
Front Inf Tri	Inferior frontal gyrus, triangular part	
Front Inf Orb	Inferior frontal gyrus, orbital part	
Rolandic Oper	Rolandic operculum	
Supp Motor Ar	Supplementary motor area	
Olfactory	Olfactory cortex	
Frontal Sup Med	Superior frontal gyrus, medial	
Frontal Mid Orb	Superior frontal gyrus, medial orbital	
Rectus	Gyrus rectus	
Insula	Insula	
Cingulum Ant	Anterior cingulate and paracingulate gyri	
Cingulum Mid	Median cingulate and paracingulate gyri	
Cingulum Post	Posterior cingulate gyrus	
Hippocampus	Hippocampus	
ParaHippocamp	Parahippocampal gyrus	
Amygdala	Amygdala	
Calcarine	Calcarine fissure and surrounding cortex	
Cuneus	Cuneus	
Lingual	Lingual gyrus	
Occipital Sup	Superior occipital gyrus	
Occipital Mid	Middle occipital gyrus	
Occipital Inf	Inferior occipital gyrus	
Fusiform	Fusiform gyrus	
Postcentral	Postcentral gyrus	
Parietal Sup	Superior parietal gyrus	
Parietal Inf	Inferior parietal, but supramarginal and angular g	
SupraMarginal	Supramarginal gyrus	
Angular	Angular gyrus	
Precuneus	Precuneus	
Paracentral Lobule	Paracentral lobule	
Caudate	Caudate nucleus	
Putamen	Lenticular nucleus, putamen	
Pallidum	Lenticular nucleus, pallidum	
Thalamus Heschl	Thalamus	
	Heschl gyrus	
Temporal Sup	Superior temporal gyrus	
Temporal Pol Sup	Temporal pole: superior temporal gyrus	
Temporal Mid Temporal Pol Mid	Middle temporal gyrus Temporal pole: middle temporal gyrus	
Temporal Inf		
Temporal Ini	Inferior temporal gyrus	

## Supplementary Table 1. AAL regions and abreviations

## Supplementary Subsection 6. Anatomical and Functional Grouping of Brain Regions.

Anatomical Group	AAL Regions
	Cingulum Ant
Cingulate	Cingulum Mid
Chigulate	Cingulum Post
	Frontal Sup
	Front Sup Orb
	Front Mid
	Front Mid Orb
Frontal	Front Inf Ope
	Front Inf Tri
	Front Inf Orb
	Supp Motor Ar
	Olfactory
	Front Sup Med
	Front Med Orb
	Rectus
	Hippocampus
Limbic	ParaHippocamp
	Amygdala
	Calcarine
	Cuneus
	Lingual
Occipital	Occipital Sup
<u>-</u>	Occipital Mid
	Occipital Inf
	Fusiform
	Parietal Sup
	Parietal Inf
Parietal	SupraMarginal Angular
	Precuneus
	Paracentr Lob
	Parietal Sup
	Parietal Inf
	SupraMarginal
Sensorimotor	Angular
	Precuneus
	Paracentr Lob
	L Caudate
Subcortical	Putamen
Subcortical	Pallidum
	Thalamus
	Insula
	Heschl
	Temporal Sup
Temporal	Tempr Pol Sup
1	Temporal Mid
	Tempr Pol Mid
	Temporal Inf

## Supplementary Table 2. Anatomical Grouping

**Supplementary Table 3.** Functional Grouping. If no hemisphere is specified, then regions from both left (L) and right (R) hemisphere are used.

Functional Group	AAL Regions
	Calcarine
$\mathbf{V}_{i}$ == -1 ( $\mathbf{V}_{i}$ =)	Cuneus
Visual (Vis)	Lingual
	Occipital Sup (L)
	Lingual (L)
	Occipital Sup
Extrastriate (ES)	Occipital Mid
Extrastriate (ES)	Occipital Inf
	1
	Parietal Sup
Auditory (Aud)	Front Inf Ope (L)
	Front Inf Tri (L)
	Rolandic Oper
	Insula
	Cingulum Ant
	Cingulum Mid
	Amygdala
	SupraMarginal
	Putamen
	Pallidum
	Thalamus
	Heschl
	Temporal Sup
	Temporal Mid (R)
	Tempr Pol Sup (R)
	Heschl
	Paracentr Lob
	Parietal Sup
Somatomotor (SM)	Postcentral
	Cingulum Mid
	Rolandic Oper
	Precentral (R)
	Precentral
	Frontal Sup
	Front Mid
	Supp Motor Ar
	Front Sup Med
	Front Med Orb
Excecutive Control (EC)	Insula
	Cingulum Ant
	Cingulum Mid
	SupraMarginal (L)
	Precuneus
	Tempr Pol Sup
	Caudate (R)
	Front Mid
	Front Inf Ope
Frontoparietal (FPN)	Front Inf Tri
	Parietal Inf
	Angular
	Front Sup Med
	Cingulum Ant
Default Mode (DMN)	Cingulum Post
	Angular
	Precuneus
	Front Sup Orb
	Front Mid
	Front Mid Orb
Salience (Sal)	
Salience (Sal)	Front Inf Orb
Salience (Sal)	Front Inf Orb Supp Motor Ar
Salience (Sal)	Front Inf Orb

#### Supplementary Subsection 7. Tractography.

For the sake of completeness, in the following we describe in detail the methods used by Ref.<sup>11</sup> to obtain the human connectome. We clarify that we did not produce these connectome data sets, instead, we used data kindly provided by Gustavo Deco.

The structural connectivity between the 90 AAL regions was obtained from averaging across 16 healthy young adults (5 females, mean SD age: 24.75 2.54). The linear registration tool from the FSL toolbox (www. fmrib.ox.ac.uk/fsl, FMRIB, Oxford) was used to coregister the EPI image to the T1-weighted structural image. The T1-weighted image was co-registered to the T1 template of ICBM152 in MNI space. The resulting transformations were concatenated and inversed and further applied to warp the AAL template from MNI space to the EPI native space, where interpolation using nearest-neighbor method ensured that the discrete labeling values were preserved. Thus the brain parcellations were conducted in each individual's native space. The structural connectivity (SC) maps were generated for each participant using the dMRI data acquired. The two data sets acquired have different phase encoding to optimize signal in difficult regions. The construction of these structural connectivity maps consisted of a three-step process. First, the regions of the whole-brain network were defined using the AAL template as used in the functional MRI data. Second, the connections between nodes in the whole-brain network (i.e., edges) were estimated using probabilistic tractography. Third, data was averaged across participants.

The FSL diffusion toolbox (Fdt) was used to carry out the various processing stages of the diffusion MRI data using the default parameters of this imaging pre-processing pipeline on all participants. Following this preprocessing, we estimated the local probability distribution of fiber direction at each voxel. The probtrackx tool in Fdt was used to provide automatic estimation of crossing fibers within each voxel.

The connectivity probability from a seed voxel *i* to another voxel *j* was defined by the proportion of fibers passing through voxel *i* that reach voxel *j* using a sampling of 5000 streamlines per voxel. This was extended from the voxel level to the region level, i.e., in an AAL parcel consisting of n voxels, 5000x n fibers were sampled. The connectivity probability  $P_{ij}$  from region *i* to region *j* is calculated as the number of sampled fibers in region *i* that connect the two regions divided by 5000 x n, where n is the number of voxels in region *i*. The SC matrix was thresholded at 0.1%, i.e., five streamlines.

For each brain region, the connectivity probability to each of the other 89 regions within the AAL was calculated. Due to the dependence of tractography on the seeding location, the probability from *i* to *j* is not necessarily equivalent to that from *j* to *i*. However, these two probabilities are highly correlated across the brain for all participants (the least Pearson r = 0.70,  $p < 10^{-50}$ ). As directionality of connections cannot be determined based on diffusion MRI, the unidirectional connectivity probability  $P_{ij}$  between regions *i* and *j* was defined by averaging these two connectivity probabilities. This unidirectional connectivity between the two areas, with  $C_{ij} = C_{ji}$ . The regional connectivity probability was calculated using in-house Perl scripts. For both phase encoding directions, 90x90 symmetric weighted networks were constructed based on the AAL90 parcellation, and normalized by the number of voxels in each AAL region; thus representing the structural connectivity network organization of the brain.

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